Previously, our group successfully characterized the effect of various lipids on the stalk formation in pure lipid multilayers by means of x-ray scattering. In this model system, the energy required for stalk formation was supplied by the osmotic pressure of the aqueous vapor. Despite its remarkable simplicity and efficiency, the sample environment of this method was distinct from the fusion sites in vivo. This work aims to extend the x-ray study of stalk formation to more physiological conditions. To this end, efforts on three levels have been devoted, namely the lipid level, the peptide level and the protein level. On the lipid level, PEG solutions rather than aqueous vapor were used as the stressor to promote stalk formation in pure lipid bilayers. On the peptide level, D-β-peptides were incorporated into model lipid multilayers to investigate its transmembrane behaviors. Lastly, on the protein level, a novel solvent-free protocol was developed, and SNAREs, a family of proteins which mediate vesicle fusion, were reconstituted into the multilayers via the micelle-vesicle-multilayer pathway.
Yihui Xu
Extending the X-ray Study of Membrane Fusion in Supported Multibilayers towards Physiological Conditions

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Yihui Xu

Extending the X-ray Study of Membrane Fusion in Supported Multibilayers towards Physiological Conditions

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Preface of the series editors

The Göttingen series in x-ray physics is intended as a collection of research monographs in x-ray science, carried out at the Institute for X-ray Physics at the Georg-August-Universität in Göttingen, and in the framework of its related research networks and collaborations.

It covers topics ranging from x-ray microscopy, nano-focusing, wave propagation, image reconstruction, tomography, short x-ray pulses to applications of nanoscale x-ray imaging and biomolecular structure analysis.

In most but not all cases, the contributions are based on Ph.D. dissertations. The individual monographs should be enhanced by putting them in the context of related work, often based on a common long term research strategy, and funded by the same research networks. We hope that the series will also help to enhance the visibility of the research carried out here and help others in the field to advance similar projects.

Prof. Dr. Tim Salditt
Prof. Dr. Sarah Köster
Editors
Göttingen June 2014

Preface to the present volume

Biomimetic lipid membranes are model systems for their more complex biological counterparts.
In a well controlled manner they allow us to study biomolecular structure, phase behavior and interactions of lipids, peptides and proteins the important self-assembled environment of fluid membranes. Interface sensitive x-ray scattering provides a powerful tool to analyze such systems with nanoscale resolution, preserving a clear distinction between lateral and vertical momentum transfer. That is, if the model membranes can be oriented on solid support. Unfortunately, there is a catch. The organic solvents required in spreading of the lipid films impede the incorporation of proteins, which would simply denature. Therefore, x-ray reflectivity and grazing incidence diffraction has been restricted to relatively simple multilamellar model systems consisting of lipids and small peptides, but excluding membrane proteins.

The present thesis, while addressing the important phenomenon of membrane fusion and teaching us about ‘magic lipid mixtures’ which promote membrane fusion, has made a surprising step forward: it shows how highly oriented protein-containing lipid multilamellar model systems can be prepared without solvent, simply from a vesicle suspension. This enables a new (x-ray) perspective of membrane protein assembly and interactions.

Prof. Dr. Tim Salditt
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Introduction

Many cellular and subcellular events such as virus infection [1], fertilization [2] and exocytosis [3] require two initially distinct bilayers to merge into one; this process is called membrane fusion [4, 5]. Lipid bilayers, however, do not fuse spontaneously with each other [3] due to the rather strong repulsive force between them. As a matter of fact, in *vivo* membrane fusion is predominantly mediated by fusion proteins [6]. For instance, soluble N-ethylmaleimide-sensitive factor attachment protein receptors (SNAREs) are known to mediate vesicle fusion [7]. The assembly of SNARE four-helix bundles overcomes the repulsive force to bring opposing bilayers into proximity, and merges them into one [8, 9].

Although planar bilayers can evolve into fusion pores via different fusion pathways [10], the hemifusion stalk seems to be an indispensable intermediate structure in this process [11]. As shown in Fig. 1, the proximal leaflets of stalks are connected with each other, while the distal leaflets stay separated [3]. Soon after the stalk model was proposed, it was supported by many theoretical calculations [11] and simulations [12]. Finally, in 2002, Yang and Huang [13] evidenced that stalk structures could be observed on model lipid bilayers under partial dehydration, which was the first direct experimental observation of the hemifusion stalk [14]. Moreover, 3d electron density maps were reconstructed from x-ray diffraction patterns, revealing the structure of stalks at the angstrom scale.

![Figure 1: Cartoon illustration of the membrane fusion pathway. (a) flat bilayers, (b) hemifusion stalk, (c) transmembrane contact/hemifusion diaphragm and (d) full fusion pore. The void space is colored gray. Reproduced from [3] with permission.](image)

Our group has long been devoted to the study of solid-supported lipid multibilayers under dehydration conditions, and many intrinsic physical properties
of lipid bilayers were investigated both experimentally [15, 16] and theoretically [17]. Our study has also been combined with molecular dynamic (MD) simulations which together offer a powerful toolkit for structural and energetical investigations of lipid bilayers [18]. With respect to stalk formation in particular, in the past the influence of some lipid species of great biological importance (e.g. cholesterol [19] and PIP$_2$ [20]) on stalk formation was carefully evaluated, taking advantage of our house-built vapor chamber where the relative humidity was precisely controlled. More recently, ÄFFNER et al. [21] systematically investigated the 3d structures of stalks of several common lipid compositions at increased spatial resolution, revealing that the favorable interbilayer distance of stalks is rather constant ($\sim 9$ Å) for all investigated compositions.

Fruitful results have been achieved with this simple humidity setup in pure lipid systems, and we now would like to extend this method to more complex systems closer to actual physiological conditions. To this end, two principle limitations of our current model system have to be overcome: (i) In our previous studies, the supported multibilayers were mounted in the vapor chamber where the desired osmotic pressure was facilitated by aqueous vapor. Despite the small amount of osmotic pressure induced by small molecules, biomembranes are normally not subject to such harsh dehydration. More importantly, in the vapor environment it is impossible to vary the physiological parameters such as ion strength and pH level. We thus would like to switch to aqueous solutions. For this purpose, we have to find an alternative route to facilitate osmotic pressure, and meanwhile search for a “magic lipid mixture” which is able to form stalks under mild dehydration of aqueous solutions. (ii) There are a wide variety of methods for the preparation of supported model lipid multibilayers. Previously, we were using the conventional spreading organic solution (sVS) method [15, 22] due to its high efficiency and convenience. In this protocol, lipids are first dissolved by organic solvents and then sprayed onto clean substrates. After solvent evaporation, highly oriented lipid stacks form on the substrates. However, organic solvent can lead to significant protein denaturation [23]. Consequently, the organic solvent method inhibits the reconstitution of fusion proteins into model multibilayers [24]. In order to study protein-mediated fusion in the multibilayer system, a new protocol has to be developed.

After this introduction, Chap. 1 presents the key principles of pure lipid bilayer fusion, the search for the “magic lipid mixture” which forms stalk under low osmotic pressure, and the first study of stalk formation in multibilayers of obtained candidate lipid mixtures in the aqueous environment.
Chap. 2 introduces the design and synthesis of heavy-atom labeled transmembrane $\beta$-peptides, the incorporation of such $\beta$-peptides into model lipid bilayers, and the x-ray characterizations of peptide conformations in the bilayers.

Chap. 3 presents the novel protein compatible protocol for supported multibilayers, namely the spreading vesicle suspension (sVS) method, which can be used to reconstitute membrane proteins such as SNAREs. The sVS preparation is composed of three stages: (i) the micelle stage, (ii) the vesicle stage and (iii) the multibilayer stage.

Chap. 4 takes advantage of the small-angle x-ray scattering (SAXS) technique and model fitting to investigate proteomicelles and proteoliposomes prepared by the novel sVS method. The influence of preparation methods, lipid compositions (only for vesicles) and SNARE reconstitution on micelle and vesicle structures are carefully evaluated.

Chap. 5 first presents the preliminary grazing-incidence small-angle x-ray scattering (GISAXS) study on on supported multibilayers reconstituted with SNAREs at only a few hydration conditions, followed by systematic in-house x-ray reflectivity and GISAXS characterizations performed at a large number of hydration conditions.

Chap. 6 summarizes the results within the framework of this thesis and discusses future improvements of the newly established model systems and methods in this work.
1 Stalk formation in pure lipid bilayers in aqueous solutions


The goal of this work is to achieve stalk formation in pure lipid multibilayers in aqueous solution. However, due to the lack of sufficient external energy to overcome the energy barrier between the lamellar phase and the rhombohedral (stalk) phase, pure lipid bilayers do not spontaneously form stalk structures in aqueous solutions. It is well known that water soluble polymers, e.g. polyethylene glycol (PEG) [26], introduces osmotic pressure to aqueous solution, and thus can mediate stalk formation [27] as well as full fusion [28] in pure lipid bilayers. Unfortunately, the osmotic pressure induced by PEG is rather weak [29, 30] compared with the requirements of fusion in supported multibilayers [21, 25]. In this chapter we first introduce basic principles of stalk formation in pure lipid bilayers, followed by the search for a “magic lipid mixture” which forms stalks at low osmotic pressure (high relative humidity), and finally the preliminary attempt to observe stalks in PEG solutions with the resulting “magic lipid mixture”.

1.1 Principles of stalk formation in pure lipid bilayers

Although in vivo fusion events are driven by fusion proteins, lipids which form fluid matrices for membrane proteins also have significant impact on fusion events [31]. In vitro we can make pure lipid membranes fuse by offering external energy such as heat [32], osmotic pressure [33], electric field [34], etc., so that the effect of lipids on fusion can be separately evaluated. This section introduces the basic principles of stalk formation in pure lipid bilayers under controlled osmotic pressure.
Stalk formation in pure lipid bilayers in aqueous solutions

6

Figure 1.1: Cartoon illustration of the average intrinsic curvature $C_0$ defined by $C_0 = 2(V/A_l - 1)/l$. $V$ is the volume of the entire lipid, $l$ is its full length and $A_l$ is the cross-section area of the headgroup. In the unrestrained state, $C_0 > 0$ leads to micelles, $C_0 \sim 0$ leads to planar bilayers and $C_0 < 0$ leads to inverted phases [36, 37]

1.1.1 The effect of lipid properties on the stalk energy

Chemical properties of the lipids such as their shape, charge, chain length, chain saturation, etc., can largely influence the overall phase behavior of lipid bilayers [35]. Here we briefly introduce a few lipid properties that may significantly lower the stalk energy (the energy barrier between the lamellar phase and the stalk phase).

**Lipid shape**

A lipid’s shape can be quantitatively described by the spontaneous curvature $C_0 = 2(V/A_l - 1)/l$ [37,38], where $V$ denotes the volume of the entire lipid, $l$ is its full length and $A_l$ is the cross-section area of the headgroup. As illustrated by Fig. 1.1, in the unstrained state lipids with positive $C_0$ tend to form micelles [36], lipids with $C_0$ close to zero tend to form planar bilayers, and lipids with negative $C_0$ tend to form inverted structures [39]. For mixed lipid monolayers, the average spontaneous curvature $C_{0,ave}$ is a molar average of $C_0$ of all lipids within the monolayers [40,41].

KOZLOVSKY and KOZLOV [42] have shown that lipid mixtures with smaller $C_{0,ave}$ (defined as spontaneous splay $J_s$ therein) leads to lower stalk energy. For example, the $C_0$ of pure 1,2-dioleoyl-$sn$-glycero-3-phosphocholine (DOPC) is -0.1 nm$^{-1}$ and the $C_0$ of 2-dioleoyl-$sn$-glycero-3-phosphoethanolamine (DOPE) is -0.35 nm$^{-1}$ [40], which result in the stalk energy of 45 $k_B T$ for DOPC and -30
1.1 Principles of stalk formation in pure lipid bilayers

$k_B T$ for DOPE [42]. Adding DOPE to DOPC can significantly reduce $C_{0,ave}$ [40], hence lower the stalk energy [42]. Therefore, we will incorporate lipids with lower $C_0$ such as DOPE, cholesterol (Chol) and 1-2-dioleoyl-\textit{sn}-glycerol (DOG) into the “magic mixture”, aiming at the lowest stalk energy by combining these lipids.

**Charges**

In nature, charged lipids such as phosphatidylinositol 4,5-bisphosphate (PIP\textsubscript{2}) help to mediate synaptic vesicle fusion by coupling with synaptotagmin [43]. In pure lipid systems, charged lipids are also found to promote fusion. For instance, oppositely charged lipids can together promote the fusion process of their host vesicles [44]. Vesicles containing phosphatidylserine (PS), a negatively charged lipid, can fuse with each other in the presence of a few mM Ca\textsuperscript{2+} [45, 46]. Besides the electrostatic interaction between bilayers, another possible reason for the fusion-promoting effect of charged lipids is that the surface charge density can alter the bending modulus $k$ and Gaussian curvature $k_G$ of the host membrane [46, 47], and thus reduce the stalk energy [42]. In this study we test the stalk-promoting effect of PIP\textsubscript{2} together with other lipids, based on the fact that at lower molar concentrations PIP\textsubscript{2} reduces the osmotic pressure needed to form stalks when mixed with DOPC [20].

**Alkyl chain saturation**

It is widely accepted that saturated lipids, such as sterols and glycosphingolipids, tend to form highly packed gel-phase lipid rafts which float in the membrane and achieve dedicated cellular functions [48]. In contrast, adding one C=C bond into the acyl chain region can dramatically lower the chain ordering and packing. Thus, monounsaturated lipids usually make up the majority of the liquid disordered phase ($L_d$) at physiological conditions [49]. By applying certain osmotic pressure, such membranes can transform from the $L$ phase to the $R$ (stalk) phase [13, 21].

Although most lipids in cell membranes are either saturated or monounsaturated, abundant polyunsaturated lipids which contain more than one C=C bond in the acyl chain region are found in many tissues [50]. It has been reported that polyunsaturated fatty acids are able to act like “oil” to activate the assembly of syntaxin 3 and SNAP-25, and thus promote synaptic vesicle fusion [51]. In pure lipid systems, similar promoting effect is also observed.
Teague et al. have found that in contrast to DOPE, for which certain osmotic pressure is required to form the $H_{II}$ phase, six-fold unsaturated 1-stearoyl-2-docosahexaenoic acid phosphatidylethanolamine (SDPE) can already form the $H_{II}$ phase at zero osmotic pressure. This finding can be explained by the fact that the polyunsaturated chains greatly increase the flexibility of the acyl chains and reduce the bending energy between lamellar and non-lamellar phases [52]. Therefore, we shall evaluate whether 1-stearoyl-2-docosahexaenoic acid phosphocholine (SDPC) and SDPE can effectively reduce the stalk energy in our model system as well, in comparison to their monounsaturated counter-lipids DOPC and DOPE.

1.1.2 Approaches to apply osmotic pressure to lipid bilayers

The vapor method

Osmotic pressure is one of the most common energy source for bilayer phase transitions [53, 54]. In our previous studies, osmotic pressure was mostly applied with aqueous vapor (the vapor method) [19, 20]. To briefly summarize, two $N_2$ flows, one wet one dry were pumped into a dedicated vapor chamber. By tuning the ratio of the wet and dry flows, the osmotic pressure, i.e. relative humidity (RH), could be precisely regulated on the time scale of a few minutes. The aqueous vapor can also be produced by equilibrating the chamber with aqueous solutions, typically aqueous solutions of salts [55, 56]. This method has high absolute precision but requires equilibrating time up to several hours or even days. Hence it is more often used as a calibration approach [55, 57].

The dispersion method

Another classic approach to apply osmotic pressure to lipid bilayers is to mix water and dry bilayers at desired ratios [58–60]. After full equilibration in a sealed environment, the re-dehydrated bilayers can be assumed to be subject to certain effective osmotic pressure [60].

The PEG method

Similar to salts, water soluble polymers such as polyethylene glycol (PEG) and polyvinylpyrrolidone (PVP) [61] can also apply osmotic pressure to lipid bilayers in an aqueous environment. As stated in the motivation of this chapter,
we intend to take advantage of the osmotic pressure facilitated by PEG [26] to replace the vapor method. In doing so, the sample environment switches from the gas to fluid state and therefore allows for the influence of physiological conditions, such as pH level and ion strength on stalk formation, to be evaluated in model lipid multibilayers [62]. The osmotic pressure resulting from PEG strongly depends on its molar fraction and molecular weight [30]. The investigation of the dependence of osmotic pressure on PEG concentrations will be presented later in this chapter.

1.2 Search for the “magic lipid mixture”

In the last section, we have pre-selected a series of stalk-promoting lipids from literature as well as our previous study, on the basis of lipid properties that can lower the stalk energy. In this section, we will investigate these lipids in a mixed fashion in order to find a “magic mixture” which requires the lowest stalk energy. We continue to use the conventional vapor method to bring in the osmotic pressure so that the stalk energy of various lipid mixtures can be efficiently analyzed and compared. The basic information of x-ray reflectivity measurements in this section is summarized in Appendix A.1.

1.2.1 Materials and methods

Preparation of supported multibilayers by spreading organic solution (sVS)

Eight lipids are investigated in this chapter, which are 1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC), 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), cholesterol (Chol), phosphatidylinositol 4,5-bisphosphate (PIP$_2$), 1,2-dioleoyl-sn-glycerol (DOG), docosahexaenoic acid phosphocholine (SDPC), docosahexaenoic acid phosphatidylethanolamine (SDPE) and porcine brain sphingomyelin (SM). Fig. 1.2 shows the structural formulas of these lipids. All lipids were purchased from Avanti Polar Lipids (Alabaster, AL, USA) and used without further purification. Solid-supported multibilayers which contain $\sim 1000$ lipid bilayers were prepared by spreading organic solution (sVS) [15, 22]. Prior to deposition, all lipids except PIP$_2$ were dissolved by the 1:1 (vol/vol) mixture of chloroform/2,2,2-trifluoroethanol (TFE) at 10 mg/ml lipid concentration. PIP$_2$ was dissolved by the 20:9:1 (vol/vol/vol) mixture of chloroform,
Figure 1.2: Structural formulas of lipids used in this chapter. DOPC is one of the most commonly used bilayer-forming lipid with its spontaneous curvature $C_0 \approx 0$, no net charge and monounsaturated acyl chains. Other lipids are added to DOPC based on their special properties such as negative $C_0$, charge and special chain saturation, in order to lower the stalk energy. All structures are drawn with ChemSketch freeware.

methanol and water also at 10 mg/ml lipid concentration. Meanwhile, silicon wafers with $\langle 100 \rangle$ orientation (Silchem, Freiberg, Germany) were first polished, cut to $15 \times 25$ mm$^2$ pieces and cleaned by ultrasonic bath with ultrapure water and methanol iteratively for $5 \times 15$ m in total. The resulting Si wafers were then surface treated in a plasma cleaner (Harrick PDC-002) for 5 min in order to fabricate hydrophilic SiO$_2$ layers on top of the wafers. 200 $\mu$l lipid organic solution containing the desired lipid mixture was gently pipetted onto each wafer. After $\sim 2$ h of in-air evaporation, the bulk solvent evaporated while a small amount remained inside. Hence samples were transferred into vacuum oven and stayed overnight to yield dry lipid multibilayers. For highly complex multibilayers which might contain a large number of defects, a slow annealing process was performed by heating the samples up to $40 \sim 50$ °C in a sealed vapor chamber. In the end, the resulting supported multibilayers were stored in the 4 °C refrigerator before measurements.

**X-ray reflectivity**

X-ray reflectivity experiments were performed with the laboratory x-ray 2-circle
diffractometer Wendi [19, 63], which is sketched in Fig. 1.3. The long fine focus x-ray tube (Dx-Cu 12×0.4-S GE-Seifert), operating at $U = 35kV$ and $I = 40mA$, generated a line-focus Cu K\textsubscript{α} ($\lambda = 1.54$ nm, $E = 8.048$ keV) beam at $6^\circ$ take-off angle. Here "long" refers to the length (12 mm) and "fine" refers to the width (0.4 mm) of the focal spot. A nickle window was mounted at the exit of the tube to attenuate the Cu K\textsubscript{β} emission. A macro-controlled, motorized filter wheel was mounted and controlled by macros to avoid over-exposure. The thickness and transmission of these filters are summarized in Appendix A.2. The resulting beam was collimated and further monochromated by a multilayer Göbel mirror (FOX 1D CU 12-INF, Xenocs). The beam size at the sample was defined to be $6\times1$ mm$^2$ by a set of beam-cleaning slits (S1 in Fig. 1.3). After all these optics the characteristic primary intensity was $\sim 2\times10^8$ cps with no filter in position. A monitor (GE-Seifert) was mounted between S1 and the sample position, allowing for the inspection of the intensity. Wafers carrying lipid multibilayers were placed in a self-built vapor chamber which was mounted on the 6-axis goniometer stage (Huber) with 3 translational axes (xs, ys and zs) and 3 rotational axes (th, phi and chi). Via iterative scans in these directions the wafer was accurately aligned with the beam. For reflectivity scans, the incident angle $\theta$ was coupled with the exit angle $\Theta$ so that $\Theta = 2\theta$. Downstream the sample position, the other two sets of slits (S2 and S3 in Fig. 1.3) were mounted to attenuate the scattering in non-specular directions. In the end the specular beam was collected by a fast scintillation counter (Cyberstar, Oxford-Danfysik) in each $\theta/2\theta$ position. For a typical reflectivity scan, the incident angle was scanned from 0-10$^\circ$ with 0.01$^\circ$ step size and 2 s exposure time per step. Both motor movements and beam collection were controlled by the software SPEC (Certified Scientific Software).
Humidity control

A dry nitrogen flow of constant pressure (5 bar) was equally divided into two branches. One was kept dry while the other was hydrated to RH $\sim 100\%$ by passing through pure water. A mass flow controller (Type 657C, MKS Instruments, Germany) mixed the two nitrogen flows at desired ratios and delivered them into the humidity chamber. Both the RH and temperature inside the humidity chamber were measured by a bifunctional sensor (Driesen+Kern GmbH, Germany). Humidity control was integrated into another SPEC console called SPEC-PID via a proportional-integral-derivative (PID) algorithm based macro. In order to reach higher RH, the tubing of the nitrogen flows was heated so that more $\text{H}_2\text{O}$ could be delivered into the humidity chamber. The highest achievable RH of this setup was $\sim 95\%$.

1.2.2 Data reduction and analysis

The data reduction and analysis process followed our previous studies [19, 20, 64] and has been introduced in great detail in Sebastian Äffner’s PhD thesis [65].

Data import

The original reflectivity data produced by the SPEC software was in .spec format, which was converted to plain .txt format by the Unspec software. Since the intensity $I(q_z)$ was recorded at specular conditions, the incident angle $\theta$ was converted to perpendicular momentum transfer $q_z$ with $q_z = 4\pi \sin \theta / \lambda$. The resulting $I(q_z) - q_z$ curves were imported into MATLAB (MathWorks Inc.) for further processing.

Background subtraction

The obtained intensity $I(q_z)$ is a superposition of the reflectivity from multiple lipid bilayers as well as the Si substrate. Either offset scans [66] or full $q_z$ range fitting [17, 67] could extract the contribution of the multibilayer from $I(q_z)$. Such a full $q_z$ range fitting was based on the master formula of reflectivity

$$R(q_z) = R_F(q_z) \left| \frac{1}{\rho_{12}} \int_{-\infty}^{\infty} d\rho(z) / dz e^{i q_z z} dz \right|^2,$$

(1.1)

where $R_F$ is the Fresnel reflectivity, $\rho_{12}$ is the electron density between the two
media and $\rho(z)$ is the electron density profile along the normal direction $z$. In our setup however, long counting time, low thermal fluctuation, large bilayer numbers, and high membrane orientation together gave raise to typically more than 8 sharp Bragg orders, which clearly separate from the weak scattering of the substrates (Fig. 1.4a). Therefore, only a simple background subtraction was performed to yield form factor modulus $|F_n|$ in the $n^{th}$ Bragg position [65].

![Figure 1.4](image)

**Figure 1.4:** (a) Reflectivity curves of pure DOPC multibilayer at RH 90-80%. The intensity is plotted in logarithmic scale and curves are shifted downwards for clarity.
(b) Form factor modulus $|F_n|$ in the $n^{th}$ Bragg position derived from the Bragg peak areas in (a).

**Intensity correction**

Prior to the derivation of form factor $F(q_z)$ from $I(q_z)$, a few corrections were applied to $I(q_z)$ using

$$I_{corr}(q_z) = KC_{abs}C_{pol}C_{Lor}C_{ill}C_{mul}I(q_z),$$

which have been introduced in [63, 65]. $K$ denotes the global scaling factor depending on the instrumentation.

$C_{abs}$ denotes the absorption factor resulting from radiation absorption of the membrane, with

$$C_{abs} = \frac{1 - \exp(-2\mu D/\sin\theta)}{2\mu D/\sin\theta},$$

where $\mu$ is the absorption coefficient and $D$ is the thickness of the membrane.
$C_{pol}$ is the polarization factor. Unlike synchrotron radiation, an x-ray beam generated by a sealed x-ray tube is not polarized, so that

$$C_{pol} = \frac{1}{2} [1 + \cos^2(2\theta)] . \quad (1.4)$$

$C_{Lor}$ is the Lorentz factor which is a decay factor depending on the experimental geometry and sample morphology. For reflectivity of oriented bilayers,

$$C_{Lor} = (\sin2\theta)^{-1} \propto q_z^{-1} . \quad (1.5)$$

$C_{ill}$ denotes the illumination factor caused by off-target illumination at small incident angle $\theta$. For $\theta < \arcsin(h/l)$,

$$C_{ill} = h/(l\sin \theta) ; \quad (1.6)$$

while for $\theta \geq \arcsin(h/l)$, $C_{ill} = 1$. Here $h$ and $l$ represent the beam sizes in the vertical and horizontal directions of the sample position.

$C_{mul}$ is the multiplicity factor resulting from a number of non-lamellar indices contributing to the same diffraction order. For the Bragg peaks in reflectivity experiments, $C_{mul} = 1$.

Finally, form factor modulus $|F_n|$ in the $n^{th}$ Bragg position was obtained with $|F_n| = \sqrt{I_{corr}(n)}$, where $I_{corr}(n)$ denotes the area of the $n^{th}$ Bragg peak.

**Electron density profile (EDP) reconstruction**

The electron density $\rho(z)$ along the membrane normal $z$ can be calculated with $F_n$ derived above [25, 68] with

$$\rho(z) = \sum_n v_n |F_n| \cos(q_n z) , \quad (1.7)$$

where $v_n$ denotes the phase of the $n^{th}$ Bragg order. The sVS method results in highly symmetric bilayers, and thus $v_n$ can only be +1 or −1. The swelling method [13, 33] was then applied in combination with the minus fluid model [69, 70]. The resulting minus-fluid form factor $F^{-1}(q_z)$ is a continuous function of $q_z$ and independent of the RH. The best phase combination was found when

$$\sum_{RH} \sum_n |v_n F_n - F^{-1}(q_n)|^2 = min . \quad (1.8)$$
1.2 Search for the “magic lipid mixture”

**Figure 1.5:** (a) Phased form factor $v_n F_n$ and continuous minus-fluid form factor $F^{-1}(q_z)$ as a function of $q_z$. $v_n F_n$ adopts different values at various RHs while $F^{-1}(q_z)$ is RH independent. The same data set as in Fig 1.4 is used. Here the best phase combination is shown. (b) Electron density profiles reconstructed with the phased form factor $v_n F_n$. The electron densities (EDPs) are in arbitrary units, and shifted for clarity. DOPC models are placed on top to illustrate the origin of the electron density.

Fig. 1.5a plots phased form factor $v_n F_n$ and minus-fluid form factor $F^{-1}(q_z)$ against $q_z$ with the best phase combination. It is clear that in this case $v_n F_n$ matches $F^{-1}(q_z)$ well for all investigated RHs.

Fig. 1.5b shows the corresponding EDPs reconstructed with $v_n F_n$ determined in Fig. 1.5a with the swelling method. The two maxima of the EDP stand for the headgroup region of the bilayer, while the minimum in the middle represents the bilayer mid-plane. The bilayer thickness $d_{hh}$ can be derived from the positions of the two maxima. Consequently, the water layer thickness $d_w = d - d_{hh}$. Both the phase retrieval and EDP reconstruction were performed with the MATLAB script `swelling_lamellar.m` [65].

**The determination of the RH**

In this study, the fusogenicity (the ability for stalk to form) of a certain lipid mixture is parameterized by the critical relative humidity RH*, where the $L$ phase transforms into the $R$ phase. Such a transition is usually determined by grazing-incidence small-angle x-ray scattering (GISAXS) technique (Fig. 1.6a) [19, 71], which can undoubtedly reveal the bilayer phases. However, GISAXS experiments take a rather long time especially when measured with in-house in-
Figure 1.6: (a) GISAXS determination of the critical RH (RH*) of the L – R transition of DOPC-DOPC 1:1 multibilayer. At RH 72% the typical R phase diffraction pattern is observed indicating L-R phase transition. Images were recorded with the in-house beamline Rosi (see Section 5.3.1) at 0.6° incident angle for 1800 s each. Images are shown in logarithmic scale and the white scale bar denotes 20 pixels. Dashed lines denote the positions of the primary beam (PB) and specular peak (SP). The lamellar indices are denoted in black and rhombohedral indices in red. The rectangular shadow in all images results from the beamstop.

(b) Reflectivity determination of the RH* of the same multibilayer as above. The 2nd Bragg peaks of the reflectivity curves measured at RH 74-70% are shown in logarithmic scale. At RH 72% the minimum intensity is found.

stuntments (a few hours per diffraction pattern) due to its relatively low flux. In previous reflectivity studies we found that when the L phase transforms into R phase, the intensity of higher order Bragg peaks (2nd, 3rd, 4th, etc.) first decreases and then increases again (Fig. 1.6b). Fig. 1.6b demonstrates that the 2nd Bragg intensity reaches the minimum at the RH* determined by GISAXS [25]. This way, we developed a more efficient approach to determine the RH* for L-R phase transition.

**Hydration repulsion potential**

For bilayers in the equilibrium state, the osmotic pressure $\Pi$ is balanced by the hydration pressure $P_{\text{hyd}}(d_\text{w})$ and van der Waals pressure $P_{\text{vdW}}(d_\text{w})$ with

$$\Pi + P_{\text{hyd}}(d_\text{w}) + P_{\text{vdW}}(d_\text{w}) = 0 . \quad (1.9)$$

Typical $d_\text{w}$ values (8-14 Å) [21] in our model system lead to negligible $P_{\text{vdW}}(d_\text{w})$ compared with the other terms [65]. We hence obtain

$$\Pi + P_{\text{hyd}}(d_\text{w}) = 0 . \quad (1.10)$$
In the vapor environment, the osmotic pressure $\Pi$ is a function of the relative humidity $RH$, with

$$\Pi(RH) = -\frac{k_B T}{v_w} \ln\left(\frac{RH}{100\%}\right), \quad (1.11)$$

where the volume per water molecule $v_w \approx 30$ Å$^3$ if we assume a constant water density of 1 g/ml. $P_{hyd}(d_w)$ can be empirically written as an exponential decay function with respect to $d_w [56, 72, 73]$

$$P_{hyd}(d_w) = P_0 \exp\left(-\frac{d_w}{\lambda_h}\right), \quad (1.12)$$

where $\lambda_h$ is the characteristic decay length and $P_0$ is the pre-exponential factor. Combining Eq. 1.10, Eq. 1.11 and Eq. 1.12, we finally arrive at

$$\frac{k_B T}{v_w} \ln\left(\frac{RH}{100\%}\right) = P_0 \exp\left(-\frac{d_w}{\lambda_h}\right). \quad (1.13)$$

With $d_w$ extracted from the EDPs and the experimental RH values, $P_0$ and $\lambda_h$ can be fitted to provide an insight into the dehydration behaviors of certain lipid mixtures. Lower $P_0$ and higher $\lambda_h$ indicate that it is easier to bring the bilayers into close contact [56].

### 1.2.3 Binary lipid mixtures

Stalk formation of natural lipids have been extensively studied with their RH* $\leq 43\%$ [21, 65]. The corresponding $\Pi$ is too high for PEG aqueous solutions to achieve [30]. We therefore mix different natural lipids in hope of a higher RH*, i.e. lower $\Pi$. One prerequisite of such a mixture is that lipid mixtures must adopt the $L$ phase (planar bilayers) at high hydration conditions. DOPC is one of the most commonly studied bilayer-forming lipids from nature which has a spontaneous curvature $C_0$ close to zero [38]. Moreover, the RH* of DOPC is slightly higher than other lipids of its kind [65]. Based on these reasons, we attempt to add one of the stalk-promoting lipids that we have introduced in the last section into DOPC in order to further increase the RH*. In this section, the phase diagrams and hydration repulsion results of DOPC-DOPE, DOPC-DOG, DOPC-Chol, DOPC-SDPC, DOPC-SDPE and DOPC-PIP$_2$ will be presented.

**DOPC-DOPE**

DOPE is regarded as the “gold standard” of non-lamellar lipids [42, 52, 74–76]. It has the same carbon chain as DOPC but a smaller headgroup (sketched in
Fig. 1.7b), hence negative spontaneous curvature. As a result, DOPC and DOPE are often studied in a mixed fashion to evaluate how spontaneous curvature influences bilayer properties [38, 60, 77]. DOPE is known to reduce the necessary temperature [39] and osmotic pressure [72] for the $L - H_{II}$ phase transition, and to cause lipid segregation at higher molar concentrations [60, 77]. However, the $R$ phase, i.e. the phase of the stalk intermediate was not well characterized in early studies of DOPC/DOPE mixtures. Following the pioneering work of Yang and Huang [13, 78], a few years ago our group has carefully investigated the formation of the $R$ phase of pure DOPC, DOPC/DOPE 3:1 and DOPC/DOPE 1:1 [21, 65]. Results show that less osmotic pressure is required to achieve the same dehydration level ($d_w$) in bilayers with higher DOPE concentration. Besides, neither of the DOPC-DOPE bilayers shows phase separation under all tested conditions.

In this work, DOPC and DOPE are investigated by x-ray reflectivity at more DOPC/DOPE molar ratios. Fig. 1.7a shows the phase diagram of DOPC-DOPE mixtures at RH 90-40% with the RH* determined by the reflectivity method. Similar to previous studies, increasing the DOPE concentration consistently leads to a higher RH*, from 42% to 72%, with no phase separation appearing. No higher DOPE molar fractions are studied to avoid phase separation, which leads to difficult phase identification. Fig. 1.7b shows the hydration repulsion
curves of the DOPC-DOPE mixtures at RH 90-76%. $d_w$ is derived from the EDPs reconstructed from the reflectivity data (not shown). Curves shift consistently towards the left when increasing DOPE fraction, indicating smaller $d_w$ at the same RH. Data is then fitted using Eq. 1.13, resulting in $P_0 = 1.19, 0.90, 0.89$ and $0.50 \times 10^9$ Pa, $\lambda_h = 2.89, 2.91, 2.84$ and $3.09$ Å for pure DOPC, DOPC-DOPE 9:1, 4:1 and 1:1 (mol/mol) respectively. The decrease of $P_0$ and the increase of $\lambda_h$ imply that it is easier to dehydrate the bilayers when more DOPE is added. Note that $P_0$ and $\lambda_h$ of the same lipid mixture can sometimes vary dramatically between different measurements [21,25], due to various experimental conditions and fitting ranges.

**DOPC-DOG mixtures**

![Figure 1.8](image.png)

Figure 1.8: (a) The phase diagram of DOPC-DOG mixtures at RH 90-40%. Each symbol represents one individual scan, with blue squares denoting the L phase and red diamonds denoting the R phase.

(b) Hydration repulsion results of DOPC-DOG mixtures plotted in natural logarithmic scale. Only the data of lamellar hydration conditions fitted. Circles denote the experimental data and the solid lines denote the fits, resulting in $P_0 = 1.19, 0.50, 1.42, 1.22$ and $1.28 \times 10^9$ Pa, $\lambda_h = 2.89, 3.88, 2.65, 2.76$ and $2.62$ Å for pure DOPC, DOPC-DOG 99:1, 98:2, 95:5 and 90:10 (mol/mol) respectively. The structural formula of DOG is sketched on the right side of the plot.

As sketched in Fig. 1.8b, DOG has a even smaller headgroup than DOPE and thus a more negative spontaneous curvature. We therefore incorporate DOG into DOPC in the hope of a higher RH* than DOPC-DOPE mixtures. Fig. 1.8a shows the phase diagram of DOPC-DOG mixtures at RH 90-40% with the RH* determined by the reflectivity method. The RH* increases consistently with the molar fraction of DOG, from 42% of pure DOPC to 58% of DOPC-DOG 9:1 (mol/mol). DOG leads to larger $\Delta$RH than DOPE at the same molar ratio. For
instance, the RH* for DOPC-DOG 9:1 is 58% while 56% for DOPC-DOPE 9:1. This result meets our expectation based on lipid shapes. Nonetheless, reflectivity curves of DOPC-DOG 9:1 (data not shown) already show phase separation at lower RHs, which prevents further addition of DOG into DOPC and further increase of the RH* by this means. Fig. 1.8b shows the hydration repulsion curves of the DOPC-DOG mixtures at RH 90-74%. Curves shift slightly towards the left as DOG amount increases, indicating a mild decrease of $d_w$ at the same RH due to DOG. Fitting results in $P_0 = 1.19, 0.50, 1.42, 1.22$ and $1.28 \times 10^9$ Pa, $\lambda_h = 2.89, 3.88, 2.65, 2.76$ and $2.62$ Å for pure DOPC, DOPC-DOG 99:1, 98:2, 95:5 and 90:10 (mol/mol) respectively. Both parameters of all samples except DOPC-DOG 99:1 fall into a narrow range, indicating similar dehydration behaviors.

**DOPC-Chol mixtures**

![Figure 1.9:](image)

(a) The phase diagram of DOPC-Chol mixtures at RH 90-40%. Each symbol represents one individual scan, with blue squares denoting the L phase and red diamonds denoting the R phase. (b) Hydration repulsion results of DOPC-Chol mixtures in natural logarithmic scale. Data kindly provided by Sebastian Äffner. Only lamellar hydration conditions are analyzed (RH 84-94% for DOPC-Chol 7:3 and 90-76% for others). Fitting (circles) yields $P_0 = 1.19, 1.15, 0.99$ and $0.29 \times 10^9$ Pa, $\lambda_h = 2.89, 2.76, 2.75$, and $3.53$ Å for pure DOPC, DOPC-Chol 9:1, 8:2 and 7:3 (mol/mol) respectively. The structural formula of Chol is sketched on the right side of the plot.

Another natural lipid with negative spontaneous curvature is Chol, whose structural formula is sketched in Fig. 1.9b. Fig. 1.9a shows the phase diagram DOPC-Chol mixtures at RH 90-40% which was previously determined by Sebastian Äffner with the GISAXS method [19]. The RH* increases almost linearly with 30% Chol bringing the RH* to 66%. When Chol concentration increases further, the cubic phase and $H_{III}$ phases appear beside the regular $L$ and $R$ phases [19]. Hence it is difficult to further increase the RH* by adding Chol. Fig. 1.11b shows...
the hydration repulsion curves of the DOPC-Chol mixtures at RH 90-76% (94-84% for DOPC-Chol 7:3). Generally the plots shift to the left when more Chol is added, indicating smaller $d_w$ at the same RH due to Chol. The fit results in $P_0 = 1.19, 1.15, 0.99$ and $0.29 \times 10^9$ Pa, $\lambda_h = 2.89, 2.76, 2.75,$ and $3.53$ Å for pure DOPC, DOPC-Chol 9:1, 8:2 and 7:3 (mol/mol) respectively. These results demonstrate that Chol leads to lower $P_0$ and higher $\lambda_h$, i.e. easier dehydration.

**DOPC-SDPC and DOPC-SDPE mixtures**

Figure 1.10: (a) The phase diagram of DOPC-SDPC mixtures at RH 90-30%. Each symbol represents one individual scan, with blue squares denoting the L phase and red diamonds denoting the R phase.

(b) Hydration repulsion results of DOPC-SDPC mixtures plotted in natural logarithmic scale. Only the data of lamellar hydration conditions are used in fitting. Circles denote the experimental data and the solid lines denote the fits, resulting in $P_0 = 1.19, 0.73, 0.90$ and $1.61 \times 10^9$ Pa, $\lambda_h = 2.89, 3.23, 3.02$ and $2.62$ Å for pure DOPC, DOPC-SDPC 9:1, 4:1 and 1:1 (mol/mol) respectively. The structural formula of SDPC is sketched on the right side of the plot.

Now we take a look at the lipids with polyunsaturated carbon chains. As sketched in Fig. 1.10b, SDPC has the same phosphatidylcholine headgroup as DOPC but a six-fold unsaturated docosahexaenoic acid carbon chain. Figure 1.10a shows the phase diagram of DOPC-SDPC mixtures at RH 90-30% with the RH* determined by the reflectivity method. Surprisingly the RH* goes down from 42% to 34%, indicating a stalk-inhibiting effect of SDPC in our model system. Fig. 1.10b shows the hydration repulsion curves of the DOPC-SDPC mixtures at RH 90-76%. The plots are very close to each other meaning that the hydration behaviors are not dramatically changed by the addition of SDPC. Fitting results in $P_0 = 1.19, 0.73, 0.90$ and $1.61 \times 10^9$ Pa, $\lambda_h = 2.89, 3.23, 3.02$ and
Figure 1.11: (a) The phase diagram of DOPC-SDPE mixtures at RH 90-30\%. Each symbol represents one individual scan, with blue squares denoting the L phase and red diamonds denoting the R phase.

(b) Hydration repulsion results of DOPC-SDPE mixtures plotted in natural logarithmic scale. Only the data of lamellar hydration conditions are used in fitting. Circles denote the experimental data and the solid lines denote the fits, resulting in $P_0 = 1.19, 1.13, 9.10$ and $0.77 \times 10^9$ Pa, $\lambda_h = 2.89, 2.71, 1.91$ and $2.48$ Å for pure DOPC, DOPC-SDPE 9:1, 4:1 and 1:1 (mol/mol) respectively. The structural formula of SDPE is sketched on the right side of the plot.

As sketched in Fig. 1.11b, SDPE has the same phosphatidylethanolamine headgroup as DOPE and the same docosahexaenoic acid carbon chain as SDPC. Fig. 1.11a shows the phase diagram of DOPC-SDPE mixtures at RH 90-30\% with the RH* determined by the reflectivity method. The RH* increases from 42\% to 62\% upon the addition of SDPE, indicating a similar stalk-promoting effect as reported in [51, 52]. However, such a promoting effect is much weaker if we compare it with DOPE, which has increased the RH* from 42\% to 72\% at the same molar ratio. Fig. 1.11b shows the hydration repulsion curves of the DOPC-SDPE mixtures at RH 90-76\%. All plots shift towards the left side with the increase of SDPE molar fraction except for DOPC-SDPE 4:1 (mol/mol), indicating smaller $d_w$ at the same RH for bilayers containing more SDPE. Fitting results in $P_0 = 1.19, 1.13, 9.10$ and $0.77 \times 10^9$ Pa, $\lambda_h = 2.89, 2.71, 1.91$ and $2.48$ Å for pure DOPC, DOPC-SDPE 9:1, 4:1 and 1:1 (mol/mol) respectively. The fitting results of DOPC-SDPE 4:1 seem to be out of order either due to experimental error or a special coupling effect of DOPC and SDPE.

In summary, the addition of SDPC actually lowers the RH*, indicative of an unexpected stalk-inhibiting effect of SDPC when mixed with DOPC, whereas the
addition of SDPE does increase the RH* but probably due to the PE headgroup rather than the polyunsaturated acyl chain, because the $\Delta RH*$ resulted from SDPE is smaller than from DOPE at equal molar ratios. These results demonstrate that in our model system, in particular when mixed with DOPC, the polyunsaturated chains do not provide desired stalk-promoting effect. Therefore, we no longer take them into consideration in the following study.

**DOPC-PIP$_2$ mixtures**

![Phase diagram of DOPC-PIP$_2$ mixtures](image)

Figure 1.12: *The phase diagram of DOPC-PIP$_2$ mixtures at RH 90-10%, redrawn with permission [20].* Results at higher PIP$_2$ molar concentration are not shown. Each symbol represents one individual scan, with blue squares denoting the L phase, red diamonds denoting the R phase and black circles denoting the $H_{11}$ phase. The structural formula of PIP$_2$ is sketched on the right side of the plot.

As sketched in Fig. 1.12, PIP$_2$ is a negatively charged lipid which should also be able to reduce the RH* of DOPC. Previously in our group, Ghosh et al. have systematically studied the phase behavior of DOPC-PIP$_2$ mixtures at low PIP$_2$ molar concentrations (1-10%) by the GISAXS method [20]. It is found that on the one hand PIP$_2$ is able to increase the RH* from 38 to 44% at molar concentrations of 1-4%, and on the other hand it leads to an additional $H_{11}$ phase at molar concentrations $\geq$ 4% but no further increase of the RH*. 
Conclusion

By incorporating other natural stalk-promoting lipids into DOPC, we find that lipids such as DOPE, DOG, Chol and PIP$_2$ are able to increase the RH*, whereas the polyunsaturated lipids SDPC and SDPE do not manifest the expected stalk-promoting effect. Among the lipids with significant stalk-promoting effect, DOPE gives rise to the highest ΔRH with 50% DOPE leading to a RH* $\sim 72\%$. Moreover, at investigated molar ratios, DOPC-DOPE mixtures do not show any signs of phase separation. Although compared with RH* $= 43\%$ for pure DOPC, RH* $= 72\%$ is already a great leap forward, its corresponding osmotic pressure is still difficult for the PEG method [30]. Therefore, we choose DOPC-DOPE 1:1 (mol/mol) as the base mixture, and add other stalk-promoting lipids to further raise the RH*. In the next section, we will investigate the RH* and dehydration behaviors of ternary lipid mixtures, aiming at a even higher RH* in the absence of phase separation.

1.2.4 Ternary lipid mixtures

Seeing that binary lipid mixtures are unable to yield a sufficiently high RH*, we now proceed to ternary lipid mixtures. DOPC-DOPE 1:1 (mol/mol, hereafter referred to as PC-PE 1:1) is used as the base mixture because it has the highest RH* among all tested binary mixtures that exhibit single phase; other stalk-promoting lipids that we have verified above, namely DOG, Chol and PIP$_2$, are added in to it. In this section, phase diagrams and hydration repulsion results of PC-PE-DOG, PC-PE-Chol and PC-PE-PIP$_2$ at various molar concentrations of the third lipid component will be presented. This part of data is published in [25], with the PC-PE-Chol data being re-measured.

PC-PE-DOG

Fig. 1.13a shows the phase diagram of PC-PE-DOG mixtures at RH 93-70%. PC-PE molar ratio is kept at 1:1, and 1, 5 and 10% DOG is added into it. On the one hand similar to DOPC-DOG mixtures, DOG slightly increases the RH*, from 72% to 79%. On the other 10% DOG here results in a phase coexistence throughout the entire measured RH range, in contrast to DOPC-DOG 9:1 where the phase coexistence occurs only at lower RHs (for reflectivity curves see Appendix A.3. This is probably because DOG and DOPE together bring about an extremely negative spontaneous curvature, so that energetically bilayers can not maintain single phase even at high RHs. Fig. 1.13b shows the hydration re-
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Figure 1.13: (a) The phase diagram of PC-PE-DOG at RH 93-70%. Each symbol represents one individual scan, with blue squares denoting the L phase, red diamonds denoting the R phase. (b) Hydration repulsion results of PC-PE-DOG mixtures at RH 93-83% plotted in natural logarithmic scale. Circles denote the experimental data and the solid lines denote the fits, resulting in \( P_0 = 1.99, 0.82, 0.65, \) and \( 0.28 \times 10^9 \) Pa, \( \lambda_\text{h} = 1.95, 2.35, 2.57 \) and \( 3.32 \) Å for pure PC-PE 1:1, PC-PE-DOG 49.5:49.5:1, 47.5:47.5:5 and 45:45:10 (molar ratio) respectively. The structural formula of DOG is sketched on the right side of the plot.

Hydration repulsion curves of the PC-PE-DOG mixtures at RH 93-83%. All plots stay close to each other but tilts upon the addition of DOG, indicating an easier dehydration resulted from DOG. Fitting yields \( P_0 = 1.99, 0.82, 0.65, \) and \( 0.28 \times 10^9 \) Pa, \( \lambda_\text{h} = 1.95, 2.35, 2.57 \) and \( 3.32 \) Å for pure PC-PE 1:1, PC-PE-DOG 49.5:49.5:1, 47.5:47.5:5 and 45:45:10 (molar ratio) respectively. \( P_0 \) decreases and \( \lambda_\text{h} \) increases consistently upon DOG addition.

**PC-PE-Chol**

In the binary section, Chol brings about the second highest \( \Delta \text{RH}^* \) following DOPE, but leads to the appearance of an additional cubic phase at Chol > 30%. Here we incorporate Chol into PC-PE 1:1 mixture to see if the stalk-promoting effect of PE and Chol is cumulative. Fig. 1.14a shows the phase diagram of PC-PE-Chol mixtures at RH 93-70%. It is exciting to see that Chol brings the RH* to a much higher level: 5% of Chol is already able to increase the RH* from 72% to 82%. Subsequently 10% Chol brings the RH* to 85% and 20% Chol further brings it to 87%, which is the highest RH* we have ever achieved. However, phases coexistence begins to occur at Chol 20%, as shown by the double Bragg peaks in its reflectivity curves (Appendix A.4). 10% Chol on the other hand, yields a RH* of 85% which is slightly lower, but mono-phase bilayers at
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Figure 1.14: (a) The phase diagram of PC-PE-Chol at RH 93-70%. Each symbol represents one individual scan, with blue squares denoting the L phase, red diamonds denoting the R phase. (b) Hydration repulsion results of PC-PE-Chol mixtures at RH 93-83% plotted in natural logarithmic scale. Circles denote the experimental data and the solid lines denote the fits, resulting in $P_0 = 1.99, 0.90, 0.35,$ and $0.45 \times 10^9$ Pa, $\lambda_h = 1.95, 2.43, 2.62$ and $2.90 \text{Å}$ for pure PC-PE 1:1, PC-PE-Chol at molar ratios of 49.5:49.5:1, 47.5:47.5:5, 45:45:10 and 40:40:20 respectively. The structural formula of Chol is sketched on the right side of the plot.

all investigated RHs. Fig. 1.14b shows the hydration repulsion curves of the PC-PE-Chol mixtures at RH 93-83%. The hydration repulsion plot of PC-PE-Chol 45:45:10 lies far away from the other three, exhibiting a distinct dehydration behavior. Although PC-PE-Chol 40:40:20 has a higher RH*, the accompanying cubic phase probably affects its dehydration behavior. Fitting results in $P_0 = 1.99, 0.90, 0.35,$ and $0.45 \times 10^9$ Pa, $\lambda_h = 1.95, 2.43, 2.62$ and $2.90 \text{Å}$ for pure PC-PE 1:1, PC-PE-Chol at molar ratios of 49.5:49.5:1, 47.5:47.5:5, 45:45:10 and 40:40:20 respectively. The lowest $P_0 (0.35 \times 10^9$ Pa) can be found from the PC-PE-Chol 45:45:10 mixture whereas the highest $\lambda_h (2.90 \text{Å})$ is obtained from the PC-PE-Chol 40:40:20 sample.

$\textbf{PC-PE-PIP}_2$

When mixed with DOPC, PIP$_2$ greatly increases the RH* but introduces an additional $H_{II}$ phase at PIP$_2$ molar concentrations greater than 5% [20]. In contrast, when mixed with PC-PE 1:1 no clear phase coexistence occurs, even at 30% PIP$_2$ (for reflectivity curves see Appendix A.5). Figure 1.15a shows the phase diagram of PC-PE-PIP$_2$ mixtures at mono-phase molar concentrations (0-20%). Interestingly, 5%, 10% and 20% PIP$_2$ yields the same RH* (80%), slightly higher than the RH* of PC-PE 1:1 (72%) but lower than the RH* of PC-PE-Chol 45:45:10 (85%).
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Figure 1.15: (a) The phase diagram of PC-PE-PIP\(_2\) at RH 93-70%. Each symbol represents one individual scan, with blue squares denoting the L phase, red diamonds denoting the R phase. 
(b) Hydration repulsion results of PC-PE-Chol mixtures at RH 93-83% plotted in natural logarithmic scale. Circles denote the experimental data and the solid lines denote the fits, resulting in \(P_0 = 1.99, 0.65, 0.43, \) and \(0.34 \times 10^9\) Pa, \(\lambda_h = 1.95, 2.43, 2.82\) and \(2.83\) Å for pure PC-PE 1:1, PC-PE-PIP\(_2\) at molar ratios of 49.5:49.5:1, 47.5:47.5:5, 45:45:10 and 40:40:20 respectively. The structural formula of PIP\(_2\) is sketched on the right side of the plot.

seems that the RH* of PC-PE-PIP\(_2\) mixtures quickly reaches saturation at PIP\(_2\) molar concentration as low as 5%. Fig. 1.15b shows the hydration repulsion curves of PC-PE-PIP\(_2\) mixtures. The curves shift towards the left when more PIP\(_2\) is added, indicating smaller \(d_w\) at the same RH for bilayers containing more PIP\(_2\). Fitting yields \(P_0 = 1.99, 0.65, 0.43, \) and \(0.34 \times 10^9\) Pa, \(\lambda_h = 1.95, 2.43, 2.82\) and \(2.83\) Å for pure PC-PE 1:1, PC-PE-PIP\(_2\) at molar ratios of 49.5:49.5:1, 47.5:47.5:5, 45:45:10 and 40:40:20 respectively. \(P_0\) decreases while \(\lambda_h\) increases consistently as more PIP\(_2\) is added, meaning that bilayers dehydrate more easily in the presence of PIP\(_2\), which agrees with the DOPC-PIP\(_2\) results.

Summary

In this section, three stalk-promoting lipids, DOG, Chol and PIP\(_2\) are added into PC-PE 1:1, the “best” binary mixture that we have determined in the last section. Results show that the stalk promoting effect is indeed cumulative as indicated by the further increased RH*. Such an increase is significant at lower molar concentrations of the third component, but saturates as soon as higher amount is added. Meanwhile, higher amount of the third component also leads to noticeable phase separation. PC-PE-Chol 40:40:20 for example, yields the highest RH* (87%) among all ternary mixtures, but exhibits strong phase separation. In con-
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Contrast PC-PE-Chol 45:45:10 yields a slightly lower RH* (85%) but without phase separation. Moreover, RH* = 85% of PC-PE-Chol 45:45:10 is still much higher than the RH* of PC-PE-DOG and PC-PE-PIP$_2$ mixtures, and is already achievable by the PEG method [30]. Considering that we will introduce PEG and other physiological conditions in the following study, PC-PE-Chol 45:45:10 with clean mono-phase is certainly more favorable.

1.2.5 Quaternary lipid mixtures

In the last section we have determined that PC-PE-Chol 45:45:10 facilitates a high RH* (85%) as well as clean mono-phase. Additionally, PIP$_2$ and DOG are also able to increase the RH* of PC-PE but less effective than Chol. We now add either 1% DOG or 5% PIP$_2$ to PC-PE-Chol 45:45:10 in hopes of a even higher RH* without introducing new phases.

Another quaternary mixture studied in this section is PC-PE-Chol-SM 35:30:15:20. It is regarded as the “Nature’s own fusiogenic mixture” [79] because of its similar lipid composition as synaptic vesicle membranes. HAQUE et al. [79] have revealed that this mixture is able to promote fusion and reduce vesicle rupture. It is thus interesting to evaluate its stalk-promoting effect in the supported multibilayer system.

**PC-PE-Chol-DOG**

Fig. 1.16 shows the reflectivity curves of PC-PE-Chol-DOG at molar ratio of 44.5:44.5:10:1 at RH 92-75%. Phase coexistence occurs at almost all investigated RHs. It is an unexpected result since PC-PE-Chol 45:45:10 exhibits clean singles phase and here only 1% DOG is added. Moreover, at lower hydration conditions (e.g. RH 75%), less Bragg orders can be observed with some showing 3-fold peaks, indicating a even stronger phase separation and reduced lamellar ordering. Similar to PC-PE-DOG mixtures, DOG’s highly negative spontaneous curvature again seems to be unfavorable among the majority of the lipids and thus leads to phase separation. As a result of the severe phase separation, it difficult to undoubtedly identify the RH* with the reflectivity determination.

**PC-PE-Chol-PIP$_2$**

Fig. 1.17 shows the reflectivity curves of PC-PE-Chol-PIP$_2$ at molar ratio of 42.5:42.5:10:5 at RH 94-80%. At higher hydration conditions (RH 94-91%), only
1.2 Search for the “magic lipid mixture”

Figure 1.16: Reflectivity curves of PC-PE-Chol-DOG 44.5:44.5:10:1 at RH 92-75% from top to bottom. Data plotted in logarithmic scale and scaled for clarity. Inset: Zoom of the 2nd Bragg peak at RH 87%.

Figure 1.17: Reflectivity curves of PC-PE-Chol-PIP2 42.5:42.5:10:5 at RH 94-80% from top to bottom. Data plotted in logarithmic scale and scaled for clarity. Inset: Zoom of the 3rd Bragg peak at RH 87%.
one phase appears; whereas at lower hydration conditions a new phase with smaller bilayer periodicity emerges, which is perhaps the $H_{II}$ phase [20]. This observation is not in line with the results of PC-PE-Chol 45-45-10 and PC-PE-PIP$_2$ 47.5-47.5-5 where single phase persists. We hence assume that the coexistence of Chol and PIP$_2$ leads to large packing stress [80], and the membrane reacts to it by forming an additional $H_{II}$ phase. Consequently, we can not undoubtedly identify the RH$^*$ of PC-PE-Chol-PIP$_2$ 42.5:42.5:10:5 with the reflectivity determination.

**PC-PE-Chol-SM**

![Reflectivity curves of PC-PE-Chol-SM](image)

Figure 1.18: Reflectivity curves of PC-PE-Chol-SM 35:30:15:20 at RH 93-81% from top to bottom. Data plotted in logarithmic scale and scaled for clarity. The dashed circle shows the minimum of the 3rd Bragg peaks at RH 89%. Inset: Zoom of the 2nd Bragg peak at RH 83%.

Fig. 1.18 shows the reflectivity curves of the “nature’s own fusiogenic mixture”, PC-PE-CH-SM 35:30:15:20 at RH 95-83%. There is only one phase at higher hydration conditions (RH 93-91%); whereas the second phase start to appear at RH $\sim$ 90% and persists until RH 83%. Despite the phase coexistence at lower RHs, we are still able to clearly figure out the intensity minimum of the Bragg peaks, as denoted by the blue circle in Fig. 1.18 at RH 89%. Indeed, the “nature’s own fusiogenic mixture” is able to deliver a even higher RH$^*$ than solely PC-PE-CH, but at the cost of phase separation.
1.3 Investigation of selected mixtures in PEG aqueous solutions

Summary

In this section reflectivity scans at various RHs are performed on three quaternary lipid mixtures, namely PC-PE-Chol-DOG 44.5:44.5:10:1, PC-PE-Chol-PIP$_2$ 42.5:42.5:10:5 and PC-PE-Chol-SM 35:30:15:20. All mixtures show certain degrees of phase separation, either throughout all test RHs or at lower RHs. It certainly disturbs our determination of the RH* and more importantly limits the possible extension of this model system towards physiological conditions. Consequently, the ternary mixture PC-PE-Chol 45:45:10 with a RH* of 85% and clean mono-phase that we have find in the last section is still the best candidate “magic mixture”.

1.3 Investigation of selected mixtures in PEG aqueous solutions

According to the van’t Hoff equation, a solution of volume $V$ containing $n$ moles of solute will have an osmotic pressure $\Pi = nRT/V$, where $R$ is the gas constant and $T$ is the temperature [81]. Polymers such as low-molecular-weight PEG are highly soluble in H$_2$O and thus can be used as a stresser to bring osmotic pressure into aqueous solutions [26,82]. Moreover, PEG has also been widely used to achieve membrane phase transition [83] as well as membrane fusion [62,84]. In this section we use PEG-400 instead of the previously used aqueous vapor to apply the osmotic pressure and to promote $L$-$R$ phase transition.

1.3.1 Osmotic pressure induced by PEG

First of all the effective RH of PEG-400 at various mass concentrations was measured and then converted to $\Pi$ with

$$\Pi(RH) = -\frac{k_B T}{v_w} \ln \left( \frac{RH}{100\%} \right). \quad (1.14)$$

Results were compared with literature results to check its validity.

Petri dishes containing PEG aqueous solutions at 30, 40, 50, 60, 70 and 80% mass concentrations were placed in the same vapor chamber as in the vapor method. The chamber was entirely sealed so that an equilibrium state could be slowly reached at room temperature. For lower PEG concentrations (30, 40 and 50 wt%) $\sim 24$ h was needed for the equilibrium state, while for higher PEG
concentrations (60, 70 and 80 wt%) \( \sim \) 12 h was needed. Three humidity sensors (Driesen+Kern GmbH, Germany) were installed in parallel to yield more accurate RH results. Fig. 1.19a shows the RH-time plots of lower PEG concentrations, resulting in equilibrium RHs of 97.51%, 94.45% and 91.52% for PEG 30, 40 and 50 wt% respectively. Fig. 1.19b shows the RH-time plots of higher PEG concentrations, resulting in equilibrium RHs of 86.36%, 75.87% and 66.25% for PEG 60, 70 and 80 wt% respectively.

Fig. 1.20 displays in-house experimental data (black) that we have obtained from Fig. 1.19, as well as three sets of literature data [29, 30, 85]. Our data is fitted via a third-degree polynomial, resulting in

\[
RH[\%] = -7.95 \cdot 10^{-5} C_{PEG}^3 + 1.95 \cdot 10^{-3} C_{PEG}^2 - 7.42 \cdot 10^{-2} C_{PEG} + 99.99, \tag{1.15}
\]

where \( C_{PEG} \) is the mass fraction of PEG-400 in %. The RH is converted to \( \Pi \) with Eq. 1.14 and shown by the right Y axis. At lower PEG concentrations, the RH decreases slightly, staying above 90%. When PEG-400 concentration exceeds 50% on the other hand, the RH decreases rapidly: 80 wt% PEG-400 brings about a surprisingly low RH \( = 66.25\% \). It can be found that all literature data shows a similar tendency as our own measurements. Furthermore, different measuring techniques yield results with large variation, especially in the non-measured concentration range (> 50 wt%). Our results show median values, which are the closest to RAND’S data [85]. We have determined in the last section that the best candidate “magic mixture” PC-PE-Chol 45:45:10 forms clean stalk phase at RH lower than 85%. From fig. 1.20 we can anticipate that the necessary RH
1.3 Investigation of selected mixtures in PEG aqueous solutions

for stalk formation can be accomplished by PEG-400 aqueous solution of PEG mass concentration ~ 58%.

1.3.2 DOPC in PEG aqueous solutions

Since the bilayer structure and phase behaviors of DOPC is well known, we thus use it as the standard sample to yield an insight of the interactions between PEG-400 and lipid bilayers. Additionally, due to its small size, we shall also inspect whether PEG-400 enters the lipid bilayers. Therefore, before we evaluate the candidate “magic mixture”, we first evaluate how DOPC multibilayer responds to various PEG-400 aqueous solutions.

X-ray reflectivity results

X-ray reflectivity experiments were performed with the commercially available D8 Advance x-ray diffractometer (Bruker-AXS, Germany). The beam generated by a Mo source at 40 mA and 40 kV first passed through a 65 µm thick Zr filter to remove the Kβ emission. The resulting Mo Kα beam had a much higher energy ($E = 17.48$ keV, $\lambda = 0.071$ nm) compared with Cu Kα ($E = 8.02$ keV, $\lambda = 1.54$ nm).
that we used in the vapor method. Thus it could penetrate the aqueous solution with much less absorption. After being collimated by a Göbel mirror the beam was further defined by a set of horizontally wide open slits with $65 \, \mu m$ slit size in the vertical direction. The beam then entered the self-built fluid chamber (Fig. 1.21), where the Si wafer carrying the multibilayer was mounted in the wafer slot on the bottom of the inner chamber [86]. After passing through another set of slits, the exit beam was finally detected by a scintillation counter. Scans were recorded from $\theta = 0$ to $2.5^\circ$ at intervals of $0.001^\circ$ for 2 s per step.

Figure 1.21: Sketch of the self-built fluid chamber [86] designed for x-ray characterizations of lipid multibilayers in solutions. The chamber interior is sealed by two polypropylene films (30 $\mu m$) on both sides. The inlet and outlet in the upper part the chamber can be used for dynamic flow, while in this work they are kept sealed to achieve equilibrated osmotic pressure.

Figure 1.22: Reflectivity curves of DOPC in PEG-400 aqueous solutions at several PEG mass fractions. Curves are plotted in logarithmic scale and shifted downwards for clarity.
1.3 Investigation of selected mixtures in PEG aqueous solutions

Fig. 1.22 shows the reflectivity curves of DOPC in PEG-400 aqueous solutions of PEG mass fractions of 30, 40, 50, 60, 70 and 80 wt%. The curves exhibit relatively high experimental errors compared with the reflectivity curves measured in vapor chamber, as indicated by the rough baseline. For almost all PEG concentrations 5 sharp Bragg peaks can be clearly observed. When PEG concentration increases, the Bragg peaks shift towards lower $q_z$ due to the osmotic pressure induced by PEG.

Figure 1.23: (a) EDPs reconstructed with the reflectivity curves in Fig. 1.22, using the phase combination of $-1, +1, -1, +1, -1$. Curves are normalized by the electron density of the methyl dip. (b) Bilayer parameters derived from the EDPs and a function of PEG mass fraction (the lower X-axis). PEG mass fraction is converted to the RH and denoted in the higher X-axis. Standard deviations are too small to be shown.

Fig. 1.23a shows the EDPs reconstructed with the reflectivity curves above, using the phase combination of $-1, +1, -1, +1, -1$. Firstly, all EDPs display the typical cross-bilayer lineshape, implying no significant PEG-400 penetration into the bilayers. Secondly, the electron densities between the water layer and the headgroup region tend to smear out when more PEG is added. This might originate from the PEG molecules that enter the water layer, lead to a higher electron density of the water layer. Lastly, the EDPs of the acyl chains largely overlap with each other, demonstrating a unaltered cross-bilayer structure in the presence of PEG-400, which again proves that no PEG penetrates the bilayers.

Fig. 1.23b shows the bilayer parameters extracted from the EDPs on the left, including the bilayer periodicity $d$, bilayer thickness $d_{hh}$ and water layer thickness $d_w$. PEG-400 drastically reduces both $d$ and $d_w$ but barely changes $d_{hh}$, which is analogous to bilayers’ reaction to aqueous vapor [25, 65]. This is an
encouraging result because it validates the method of using PEG to induce osmotic pressure and to promote bilayer phase transition in our model system. Furthermore at lower PEG concentrations, both $d$ and $d_w$ values are comparable to literature values under the same dehydration conditions [65,87], whereas at higher PEG concentrations, slightly lower $d$ and $d_w$ are obtained. For example in our measurement $d \approx 46 \, \text{Å}$ at PEG 80 wt% (RH = 66.25%), while $d \approx 49 \, \text{Å}$ in [65, 87] at RH 66%. It is possibly because that there might be a larger error in the estimated osmotic pressure at higher PEG concentrations (see Fig. 1.20), where the osmotic pressure increase rapidly with the PEG concentration.

### 1.3.3 PC-PE-Chol in PEG aqueous solutions

Having proved that PEG-400 yields desired osmotic pressure without penetrating the lipid bilayers, we now set the candidate “magic mixture”, PC-PE-Chol 45:45:10 into the same series of PEG-400 solutions. Unlike the vapor method where dehydration conditions can be efficiently tuned by software-controlled pumps, in the PEG method one has to manually prepare PEG solutions and mount the samples for each hydration condition. Although automated strategies like continuous pumping can be developed to mix PEG and H$_2$O with higher efficiency, currently we can not identify the $L$-$R$ phase transition in PEG solutions using the reflectivity determination, as it usually requires a large number of reflectivity curves at various conditions. We therefore turn to the GISAXS method. Considering the high Cu-K$\alpha$ absorption coefficient of PEG solutions, high-energy synchrotron radiation is used.

GISAXS experiments were performed at the undulator beamline ID01 of the European Synchrotron Radiation Facility (ESRF) in Grenoble, France. The photon energy was set to 17.91 keV by the Si (111) double crystal monochromator. A series of beamline optics yielded a beam size of $160 \times 20 \, \mu\text{m}^2$ on the sample, which was set in the fluid chamber (Fig. 1.21). A 6-circle sample tower carried the chamber and enabled sample alignment in 3 translational and 3 rotational directions. A 4-unit 2D pixel detector (Medipix TAA22PC) with $516 \times 516$ pixels and $55 \, \mu\text{m} \times 55 \, \mu\text{m}$ pixel size was mounted 178.59 mm behind the sample position. A rectangular-shape beamstop was attached to the detector to attenuate the primary beam (PB), the specular peaks (SP) and the 1$^{st}$ Bragg peaks (BP). Each exposure was recorded for 10 s using a 200 $\mu$m thick Mo attenuator. PEG-400 aqueous solutions of various PEG mass fractions was successively added into the fluid chamber where the multibilayer sat. Preceding exposures, the whole system was let stand for a few minutes to reach equilibrium.
1.3 Investigation of selected mixtures in PEG aqueous solutions

Figure 1.24: (a) GISAXS patterns of PC-PE-Chol 45:45:10 immersed in PEG-400 solutions of various mass fractions, with only ROI being displayed. The shadow results from the beamstop which attenuates the primary beam (PB), specular peaks (SP) and the 1<sup>st</sup> Bragg peaks (BP). Intensity is plotted in logarithmic scale. (b) Zoom of the GISAXS pattern at PEG 65 wt%. R-<i>H</i><sub>11</sub> phase coexistence is observed. The in-plane Bragg peaks are denoted in black while the off-plane peaks are denoted by red (R) and blue (<i>H</i><sub>11</sub>) dashed circles.
Fig. 1.24a shows the GISAXS patterns of PC-PE-Chol 45:45:10 immersed in 40-80 wt% PEG-400 aqueous solutions. At lower PEG concentrations (40-60 wt%), only a single L phase shows up. At PEG concentrations higher than 65 wt%, phase coexistence of the R and HII phase can be observed, which is more clearly shown by Fig. 1.24b. The in-plane Bragg peaks (denoted in black) split into two, and meanwhile the characteristic out-plane peaks of both phases appear on both sides of the mid-plane. At even higher PEG concentrations (70-80 wt%) the R-HII phase coexistence persists, while the Bragg peaks become blurry and less visible probably due to radiation damage. Changing the sample after every exposure can eliminate this possibility, but certainly will take more preparation time.

First of all, it is exciting to see the appearance of the R phase in PEG solution, which is the result we have perused in this whole chapter. It opens up a new window for the x-ray characterization of model lipid bilayers. But in the mean time, a unexpected HII phase also appears. Such a phase separation has occurred in the last section, but at 20% Chol rather than at 10%. This is also the reason why we chose PC-PE-Chol 45:45:10 over 40:40:20. This issue of unexpected phase separation is possibly PEG-related, but more investigations have to be performed before we come to an conclusion. Lastly, 65 wt% PEG is in line with our anticipation that the R phase starts to appear at 58 wt% based on the PEG-II dependence determined in the beginning of this section.

1.4 Summary and outlook

The beginning of this chapter introduces the search of candidate “magic lipid mixtures”. After systematic investigations of various binary, ternary and quaternary lipid mixtures, PC-PE-Chol 45:45:10 mixture was determined to require the lowest osmotic pressure (RH* = 85%), among mixtures that exhibit clean single-phase at all applied hydration conditions. In the last section of this chapter this candidate mixture was preliminarily investigated in PEG-400 solutions by GISAXS. Excitingly, the desired R phase appears in solutions of PEG concentrations higher than 65 wt%. This finding validates the new model system where stalk structures can form in aqueous solutions in the absence of fusion proteins, and enables upcoming characterization of the influence of physiological conditions such as pH level and ion strength on stalk formation. However, prior to the introduction of these conditions, we first have to optimize the model system by solving the problem of R-H phase coexistence.
2 X-ray studies of transmembrane \( \beta \)-peptides


Integral membrane proteins anchor themselves into the membrane via transmembrane domains (TMDs) [89], which play a critical role in many membrane functions [90, 91] including membrane fusion [92–94]. Most transmembrane proteins are large and complex, and interact strongly with their surrounding lipids in multiple ways [95]. Many model transmembrane peptides [96,97] have been developed in order to separately investigate the TMDs. For this purpose, \( \beta \)-peptides are well-suited candidates as they are conformationally stable [98], exhibit significant helical propensities in short sequences [99], and offer the possibilities to customize the dipole moment and helical width [100].

This chapter first presents the design and synthesis of heavy-atom labeled 14-helical transmembrane \( \beta \)-peptides, and the preparation of \( \beta \)-peptide/DOPC bilayers. Following previous characterizations of model transmembrane \( \alpha \)-peptides [101–103], the resulting \( \beta \)-peptide/DOPC bilayers were investigated by CD spectroscopy, x-ray reflectivity and grazing-incidence small-angle x-ray scattering (GISAXS). Results reveal a successful incorporation of model \( \beta \)-peptides into DOPC bilayers in a slightly tilted transmembrane fashion. Starting from such a success, our collaborators [104] introduced recognition units (\( \beta \)-glutamine) into the current peptide sequence, enabling helix-helix assembly in a sequence-controlled manner. In the future, these results can be further utilized to design and synthesize the TMDs of SNARE analogs, in association with various fusion recognition motifs [105–107] and linkers [108, 109].

\(^{1}\) These authors contributed equally.
2.1 Fundamentals of β-peptides

α- and β-peptides

Two decades ago, Seebach et al. [99] and Gellman et al. [112] showed that synthetic β-peptides which consist of β-amino acids (Fig. 2.1b) were also able to form stable helical structures. Compared with α-amino acids, the additional Cβ atoms and side chains result in profound differences in the helical architecture [111], as shown by Fig. 2.1c and 2.1d. One turn of α-helices consists of ~3.6 residues with its pitch \( p \approx 5.4 \text{ Å} \). In contrast one turn of β-helices consists of ~3 residues with its pitch \( p \approx 5 \text{ Å} \) [110].

Advantages of using β-peptides as TMDs

The helical structures of β-peptides result in several advantages over α-
2.1 Fundamentals of β-peptides

peptides in TMD design, synthesis and characterization [88]: (i) β-peptides are more stable against both solvents [113] and enzymes [114]. Thus their helical structures are presumably well preserved in most experimental conditions. (ii) Less amino acids are required for stable β-helices. CD results show that at least 14-15 amino acids are needed to facilitate significant α-helix propensity, whereas as few as 6 residues can already form stable β-peptides [99, 110]. Shorter TMDs can thus be synthesized to better evaluate how TMD length affects TMD behaviors. (iii) The helical width and the helical dipole moment of β-peptides can be varied [97, 99]. In other words, β-peptides can be tailored with higher degree of freedom compared to α-peptides, allowing for a larger variety of resulting TMD structures.

**Different types of β-peptides**

![β-peptide structures](image)

Figure 2.2: Upper: Major Ca/Cβ substitution patterns of β-peptides, including (a) β², (b) β³ and (c) β²/β³ [110]. O, N, C and H atoms are denoted by red, blue and gray spheres respectively. Rⁿ denotes the side chains.

Lower: Major hydrogen-bonding patterns of β-peptides, including (e) 8- (f) 10- (g) 12- (h) 14- and (i) 10/12-helices. Side chains are not shown for clarity. Adapted from [113].

One of the many approaches to classify β-peptides is by means of Ca/Cβ substitution patterns of the amino acids, resulting in β²-peptides, β³-peptides, β²/β³-peptides, etc. [110]. As shown in the upper part of Fig. 2.2, β²-peptides are ex-
clusively substituted at Cα, β3-peptides are exclusively substituted at Cβ, and β2/β3-peptides are alternatingly substituted at Cα and Cβ.

Another approach to classify β-peptides is based on the hydrogen-bonding patterns, i.e. the number of the atoms that form the hydrogen-bonded rings [111]. This is also one of the conventional nomenclature in literature [113]. Common hydrogen-bonding patterns of β-peptides include 8-, 10-, 12-, 14-, and 10/12-helices [112, 115, 116], which are illustrated in the lower part of Fig. 2.2. Among them, the 14-helix is the most common hydrogen-bonding pattern for β2- and β3-peptides [117]. Its side chain of every third amino acid (i and i+3) aligns on the same side of the helix [97], which enables stronger medium-range interactions (i and i+3 association), hence the helix is more stable [113].

2.2 Sample preparation

In this section, we first introduce the design and synthesis of two families of 314 transmembrane β-peptides. Each peptide family consists of three β-peptides with different labeling conditions, i.e. non-labeled, I-labeled in the tail region and I-labeled in the center region (see Fig. 2.4 below). I-labels can give rise to stronger x-ray scattering intensity in labeled moieties and thus reveal peptide conformations in the membrane. The only difference between these two families is that the second contains additional htryptophan (hTrp) anchors, which are known to locate at the polar/nonpolar interface of phosphatidylcholine bilayers [118], and thus enhance the anchoring effect. After synthesis they were integrated either into DOPC vesicles for CD spectroscopy, or into DOPC multibilayers for x-ray characterizations.

2.2.1 Synthesis of I-labeled β-amino acids

I-labeled β-peptides were obtained by modifying commercially available β-amino acids [119], following previously published protocol for α-peptides [101]. Only one of the two side chains was labeled, yielding building blocks compatible with the following Fmoc-based solid-phase peptide synthesis (SPPS) [120].

Fig. 2.3 shows the synthesis pathway of doubly iodinated Fmoc-protected D-β3-amino acid. The starting product Boc-D-β3-Asp-OBzl (1) was obtained from Boc-l-Asp(OBzl)-OH. 1 was converted to Weinreb amide (5) with N-ethylmorpholine, N,O-dimethylhydroxylamine hydrochloride and propylphos-
Figure 2.3: Synthesis pathway of Fmoc-D-β3-6,6-diiodoallylhomoglycine (8). Boc-d-β3-Asp-OBzl (1) was converted to Weinreb amide (5), and reduced with DIBAL to yield aldehyde (6). Finally deprotection/protection steps were performed under Wittig conditions, yielding tFmoc-D-β3-6,6-diiodoallylhomoglycine (8). Adapted from [88].

2.2.2 Design of transmembrane β-peptides

This section presents the synthesis of the two families of I-labeled transmembrane β-peptides by means of manual microwave-assisted SPPS [119, 123]. Figure 2.4 shows their structural formulas.

These two families of β-peptide share a similar peptide sequence. 19 D-β3-valines (hVal) were incorporated in the center of the peptide sequence to span the whole acyl-chain region of lipid bilayers, as hVal is hydrophobic and forms stable 314-helical structures [124]. In addition, each side of the peptide was flanked by two D-β3-lysines (hLys) to effectively anchor both ends of transmembrane β-peptides at the water/headgroup interface of the bilayers [125]. We thus obtained the first peptide family (9, 10 and 11) which consisted of only hLys and hVal. Moreover, it is known that the aromatic indole moieties of D-β3-tryptophan (hTrp) tend to reside at the polar/apolar interface of phosphocholine bilayers [126]. In order to further enhance their anchoring effect,
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Figure 2.4: Structural formulas of synthesized transmembrane $\beta$-peptides. 9-11: $\beta$-peptides do not contain $^h$Trp, and 12-14: $\beta$-peptides contain $^h$Trp. 9 and 12 are non-labeled, 10 and 13 are labeled at the tail, while 11 and 14 are labeled in the center. I-labels are denoted in orange. Adapted from [88].

$\beta^3$-tryptophans were inserted into the existing peptide sequences, yielding the second peptide family (12, 13 and 14) which consisted of $^h$Lys, $^h$Trp and $^h$Val. Within each peptide family, three labeling strategies were employed: 9 and 12 were not labeled to serve as control peptides. 10 and 13 were labeled in the tail region, whereas 11 and 14 were labeled in the center region. As a result, each peptide family consisted of 3 peptides with different I-labeling conditions. With x-ray reflectivity we will be able to reveal the positions of the labeled moieties in the $z$ direction with respect to the bilayers, and thus determine peptide conformations [101].

2.2.3 Peptide incorporation into model bilayers

The resulting transmembrane $\beta$-peptides were incorporated into large unilamellar vesicles (LUVs) for CD-spectroscopy and into supported multibilayers for x-ray reflectivity and GISAXS characterizations. Pure DOPC was used as the lipid component for both model bilayers.

Peptide incorporation into LUVs

$\beta$-peptide/DOPC LUVs were prepared by combined vortex and extrusion [127]. First the synthesized transmembrane $\beta$-peptides were dissolved by MeOH,
whereas DOPC was dissolved by chloroform. Two solutions were mixed to yield a mixed solution of chloroform/MeOH (1:1, \textit{vol/vol}) at peptide/lipid (P/L) molar ratio of 1:20 and \(\beta\)-peptide concentration of 38 mM. A mild nitrogen stream then slowly removed the organic solvents and resulted in dry \(\beta\)-peptide/lipid films, which was re-dissolved by pure tetrafluoroethylene (TFE) to form helical structures \cite{128}. Afterwards, TFE was again removed by the nitrogen stream which resulted in \(\beta\)-peptide/lipid films containing desired helical structures. The films were stored in vacuum at 40 \(^\circ\)C for overnight to thoroughly remove solvents. The resulting \(\beta\)-peptide/lipid films were incubated with ultrapure water for 2 h at 25 \(^\circ\)C to gain multilamellar vesicles. Subsequently, the multilamellar vesicle suspensions were vortexed (30 s) and incubated (5 min) iteratively for 5 rounds in total. In the end, vesicle suspensions were extruded through a polycarbonate membrane with 100 nm nominal pore size 31 times using an extruder (Avestin Liposofast, Ottawa, Canada) to yield unilamellar vesicles in pure water for CD spectroscopy.

\textbf{Peptide incorporation into supported multibilayers}

Peptides were incorporated into supported DOPC multibilayers by the conventional sVS method \cite{15,22} introduced in Chap. 1. In brief, DOPC and \(\beta\)-peptides were first separately dissolved by 1:1 (\textit{vol/vol}) mixture of chloroform/TFE with lipid concentration of 10 mg/ml. The two solutions were then mixed at P/L ratios of 1:50, 1:20 and 1:10. 200 \(\mu\)l of each stock solution was pipetted onto pre-cleaned, highly oriented Si wafers (10 × 15 mm\(^2\)), and kept still for 2 h so that the lipids self-assembled into bilayer stacks. Subsequently, the wafers carrying mixed multibilayers were transferred into vacuum and stayed for over night to thoroughly remove the organic solvents. In the end, annealing the samples in sealed vapor chamber yielded highly oriented bilayer stacks containing various transmembrane \(\beta\)-peptides. Samples were stored in 4 \(^\circ\)refrigerator prior to x-ray characterizations.

\section*{2.3 Sample characterization}

In the last section, we prepared two families of transmembrane \(\beta\)-peptides, with the second family containing additional \(^h\)Trp anchors. Each peptide family consists of three peptides with different labeling conditions, namely non-labeled, tail-labeled and center-labeled. The resulting \(\beta\)-peptides were then incorporated into DOPC LUVs and supported DOPC multibilayers, which were
characterized by CD-spectroscopy to inspect whether the β-helical structures can be preserved in the membrane environment, and by x-ray reflectivity and GISAXS to reveal peptide conformations with respect to the bilayers. In this section, experiments and results of these investigations will be presented and discussed.

### 2.3.1 CD spectroscopy

![Circular dichroism spectra](image)

Figure 2.5: Circular dichroism (CD) spectra of (a) transmembrane β-peptides without (9-11) and (b) transmembrane β-peptides with additional $^h$Trp anchors (12-14) in LUVs of 1:20 peptide/-DOPC in pure water. I-labels are sketched in the legends. Adapted from [88].

Circular dichroism (CD) spectroscopy is powerful tool to characterize the helical structures of peptides and proteins [129]. Fig. 2.5a and 2.5b show the CD spectra of transmembrane β-peptides without (9-11) and with (12-14) additional $^h$Trp anchors in LUVs in pure water. The CD spectra of all 6 β-peptides show typical patterns of $\alpha$-helices, as indicated by a minimum at 189 nm, a zero crossing at 198 nm, and a maximum at 205 nm. These values are comparable to the literature [116] where a maximum at 200 nm, a zero crossing at 207 nm, and a minimum at 215 nm are found in the CD spectra. Therefore, the β-helical structures were well preserved in the membrane environment, for both the peptides with and without additional $^h$Trp anchors. Moreover, the positions of these signals do not vary within the same peptide family, indicating that I-labels barely affect the helical structures of these transmembrane β-peptides. Lastly, when comparing the CD spectra of 9-11 (Fig. 2.5a) with the spectra of 12-14 (Fig. 2.5b), a weak maximum can be found at 230 nm in the spectra of 12-14. It might be attributed to the additional $^h$Trp anchors in 12-14, as aromatic side chains of $^h$Trp can result in a characteristic CD band at ~ 225 nm [130].
2.3.2 X-ray reflectivity

Instrumentation

X-ray reflectivity experiments of $\beta$-peptides/DOPC multibilayers at 0, 1:50, 1:20 and 1:10 P/L ratios were performed with the same self-built in-house x-ray diffractometer Wendi as introduced in Chap. 1. Briefly, a sealed x-ray tube (Dx-Cu 12$\times$0.4-S GE-Seifert) operating at $U = 35kV$ and $I = 40mA$ generated a Cu K$_\alpha$ ($\lambda = 1.54$ nm, $E = 8.048$ keV) beam, which was monochromated and collimated by a series of x-ray optics, yielding a beam size of $1\times5$ mm$^2$ in the sample position. Samples were mounted in a seal humidity chamber on the 6-axis goniometer stage (Huber). The final specular scattering intensity was detected by a fast scintillation counter (Cyberstar, Oxford-Danfysik). Reflectivity scans were performed at coupled $\theta/2\theta$ with a resolution of $\Delta \theta = 0.01^\circ$ and 1 s counting time at each angle. The relative humidity (RH) inside the humidity chamber was kept at $\sim 95\%$. The intensity $I$ was plotted against vertical momentum transfer $q_z = 4\pi \sin \theta / \lambda$, yielding one $I$-$q_z$ plot for each sample.

X-ray reflectivity curves

![Figure 2.6](image)

Figure 2.6: The reflectivity curves of $\beta$-peptide/DOPC mixed multibilayers (a) without $^h$Trp anchors and (b) with $^h$Trp anchors. The reflectivity curves are shifted downwards for clarity. The labeling conditions are sketched in the legends.

Fig. 2.6 shows the reflectivity curves of $\beta$-peptides/DOPC mixed multibilayers at 1:10 P/L ratio. 4 Bragg peaks occur in the reflectivity curves of multibilayers without additional $^h$Trp anchors (Fig. 2.6a), and 5 can be detected from the ones
with $^h$Trp (Fig. 2.6b), with the 5th peak being hardly visible. This is in sharp contrast to more than eight orders observed for pure DOPC multilayers (see Fig. 1.4), indicating a drastic decrease of lamellar ordering. This seems to be a common phenomenon for peptide/lipid mixed multilayers, which has been observed for many other membrane peptides [131, 132]. Moreover, the lineshapes of multilayers containing β-peptides differ dramatically from the one of pure DOPC multilayer, indicating a possible change of the structure factor induced by peptide incorporation. The difference in reflectivity curves are thus likely to be associated with changes in the inter-bilayer interaction and possibly strain fields around defects rather than with changes within the bilayers. Otherwise a change of the form factor rather than the structure factor [133] should occur. In this respect, the transmembrane β-peptides in this work completely follow previously observed scenarios.

**Reconstructed electron density profiles (EDPs)**

EDPs of the β-peptide/lipid bilayers were reconstructed from the intensities in the Bragg positions $I_n$ in a similar way as introduced in Section 1.2.2, except that the best phase combinations were not determined by the swelling method. The reason is that this method requires a series of reflectivity curves for one single sample, while for β-peptide/lipid multilayers only one hydration condition (RH ≈ 95%) was conducted. Thus the phases were manually set to $-1, +1, -1, +1$ for 4-peak curves and to $-1, +1, -1, +1, -1$ for 5-peak curves, on the basis of our previous experience that these phase combinations can result in reasonable EDPs [25,65]. The electron density $\rho(z)$ was calculated by

$$\rho(z) = \sum_n v_n \sqrt{I_n} \cos(q_n \cdot z)$$

(2.1)

where $n$ denotes the number of Bragg orders and $v_n$ denotes the phase of the $n^{th}$ Bragg order.

Figure 2.7 shows the EDPs of β-peptide/DOPC multilayers at a P/L ratio of 1:10, reconstructed from the reflectivity curves in Fig. 2.6. All resulting EDPs exhibit the typical bilayer lineshape of pure DOPC (see Fig. 1.5), with the two maxima corresponding to lipid headgroups, the minima on both sides corresponding to the water layer and the minimum in the center corresponding to the methyl dip. First of all, it is rather surprising to see well-preserved bilayer structures even at such high peptide concentrations (P/L = 1:10). This indicates that the peptides do not alter the basic structural motif of the DOPC bilayer. However, the peptide insertion results in observable changes of the bilayer structure.
2.3 Sample characterization

Figure 2.7: The EDPs of 1:10 β-peptide/DOPC multibilayers (a) without \(^h\)Trp anchors and (b) with \(^h\)Trp anchors, reconstructed from the reflectivity curves in Fig. 2.6. The electron density distribution is illustrated by drawing 3d sphere models of DOPC underneath (a). The electron contrasts between bilayers containing I-labeled and non-labeled peptides are plotted in the center. Possible peptide orientations are illustrated by placing the molecular drawing underneath both (a) and (b). The labeling conditions are sketched in the legends.

parameters in the electron density and the bilayer thickness, as we discuss further below. These changes might result from both the elastic response of the lipid bilayer to peptide insertion, as well as the direct contribution of the peptides to the electron density.

To disentangle these two effects, we subtract the EDPs of bilayers containing I-labeled peptides by the ones without I-labels. Subtraction curves are plotted in the center of Fig. 2.7. As shown in the legends, 10 and 13 are labeled in the center region, whereas 11 and 14 are labeled in the tail region. Unfortunately, in the absence of a full \(q\)-range fit of the reflectivity curve as in [133], the absolute electron densities are not available. Instead, we only obtain relative shape functions, as the Bragg peak intensities (i.e. the Fourier coefficients) are normalized by the intensity of the first Bragg peak, separately for each curve. Nonetheless it is still meaningful to compare the EDPs in arbitrary units, since all the samples were prepared and measured under the same conditions.

For center-labeled peptides (11 and 14), a strong contrast is clearly visible in the center region of the EDP. This confirms the full insertion of the TMD, which is not affected by peptide tilting in the bilayers. Hence, the peptides always center themselves in the bilayer mid-plane, as desired. The tail-labeled peptides, 10 and 13 do not exhibit a similar contrast: 10 - 9 provides a small peak at the hydrophobic/hydrophilic interface, which may be associated with the iodine
label in the tail region of 10. While such a contribution is not visible for 13 - 12, possibly because it is too widely distributed and hence ‘shielded’ by the head-group density. Assuming that the mentioned small peak really represents the I-label, the peptides must adopt a strongly tilted conformation, as illustrated by the peptides models underneath Fig. 2.7. The I-labels exhibit a much clearer labeling effect in the center region than in the tail region, possibly because the original electron density of the headgroup region is much higher than the methyl dip, while I-labels bring the same absolute amount of extra density in both regions. Another reason is that the original electron density the I-labels in the tail region have to be distributed to both bilayer surfaces since only one of the two tails is labeled. In addition, an unexpectedly large contrast around the headgroup region occurs in all subtraction curves, which is closer to the water layer for 11 - 9 and 10 - 9 whereas closer to acyl chains for 14 - 12 and 13 - 12. This could indicate either an unintended effect of iodine labeling on the host membrane surface, or a fraction of peptides oriented parallel to the bilayer (the S state) [134, 135].

Bilayer parameters derived from the EDPs

Fig. 2.8 presents the water layer thickness $d_w$ and the bilayer thickness $d_{hh}$ of the $\beta$-peptide/DOPC mixed multibilayers at P/L ratios of 0, 1:50, 1:20 and 1:10, derived from EDPs in Fig. 2.8. $\beta$-peptides, both with and without $^6$Trp anchors show a decrease of $d_{hh}$ with P/L ratios, also known as the membrane thinning effect which has been observed for many other membrane peptides [133, 136]. When the peptides adopt an inserted trans-membrane helical conformation (the $I_s$ state [135]), this thinning could be induced by a hydrophobic mismatch, forcing both the lipids and peptides to adjust their hydrophobic moieties to achieve a match [137]. With the acyl chain length of DOPC ($d_c \approx 30 \text{ Å}$, [87]) slightly shorter than the hydrophobic length of the peptides ($d_c \approx 31.17 \text{ Å}, 5.0 \text{ Å per pitch}$), a match can be achieved either by peptide tilting or by shrinking. In the latter case, a membrane thickening effect instead of a thinning effect is expected. Therefore it seems that the mismatch is relieved solely by a chain tilt, with an estimated tilt angle of 16°. In this case, one may expect that the tilted $\beta$-peptides also induces according acyl chains tilts in its neighborhood. The increase of chains tilts would then explain the thinning effect.

This thinning effect is obviously more significant for 9, 10 and 11, compared to 12, 13 and 14. In other words, additional $^6$Trp anchors may reduce the ability to minimize mismatch by increased peptide tilting. This tentative explanation is also in line with the vanishing contrast of the tail-labeled peptides, since
2.3 Sample characterization

Figure 2.8: (a) the water layer thickness \(d_w\) and (b) the bilayer thickness \(d_{hh}\) of peptide/DOPC bilayers without \(^h\)Trp anchors (9, 10 and 11) at various P/L ratios; (c) \(d_w\) and (d) \(d_{hh}\) of peptide/-DOPC bilayers with \(^h\)Trp anchors (12, 13 and 14) at various P/L ratios. The error bars denote the standard deviations. The labeling conditions are sketched in the legends.

Moreover one may be concerned to which extent the labels may change the structural properties of the transmembrane \(\beta\)-peptides. Here we see by comparison of labeled and non-labeled peptides that their \(d_{hh}\) and \(d_w\) are fairly similar, indicating that the I-label does not cause significant structural changes in the bilayer, in line with the CD results above.

2.3.3 Grazing-incidence small-angle x-ray scattering

Having determined the bilayer structural changes of the \(\beta\)-peptide/DOPC mixed multibilayer with respect to P/L ratios, we now take advantage of grazing-
incidence small-angle x-ray scattering (GISAXS) technique to investigate their chain-chain correlations, as well as the β-helical structures which offer a direct insight of the peptide conformation within lipid bilayers. To this end, multibilayers containing the first peptide family, i.e. β-peptides without \( \text{Trp} \) anchors were characterized.

**Instrumentation and data reduction**

Chain-correlation characterization was performed at ID01, ESRF with similar beamline settings as introduced in Chap. 1, except that the sample-detector distance and position of the detector arm were specially chosen to cover the \( q \) range of chain correlation peaks as well as helical peaks. Samples were placed in a similar humidity chamber as used in the reflectivity section where the RH was kept at \( \sim 95\% \). Each image was recorded with 10 s exposure time. The data reduction followed previous work \[64, 139\]. The diffraction data was first converted from pixel units to scattering vector components \( q_z \) and \( q_\parallel \), where

\[
q_x = \frac{2\pi}{\lambda} (\cos \alpha_f \cos \psi - \cos \alpha_i), \quad (2.2)
\]
\[
q_y = \frac{2\pi}{\lambda} (\cos \alpha_f \sin \psi), \quad (2.3)
\]
\[
q_z = \frac{2\pi}{\lambda} (\sin \alpha_f + \sin \alpha_i), \quad (2.4)
\]
\[
q_\parallel = \sqrt{q_x^2 + q_y^2}, \quad (2.5)
\]

as shown in Fig. 2.9a. 1d intensity profiles at different \( \phi \) angles were extracted from the 2d patterns, and then fitted with a Lorentzian above a linear background

\[
f(q) = I_0 \frac{\omega^2}{(q - q_0)^2 + \omega^2} + mq + b, \quad (2.6)
\]

where \( \omega \) is the half width maximum, \( q_0 \) the peak center, \( I_0 \) the maximum of the Lorentzian, \( m \) the slope of the linear background, and \( b \) the constant offset. The average chain-chain distance \( a \) is then obtained from \[139\]

\[
a \simeq \frac{9\pi}{4q_0} - \frac{3\omega}{2q_0^2}, \quad (2.7)
\]

and the correlation length \( \xi \) of the acyl chains by

\[
\xi = \frac{1}{\omega}. \quad (2.8)
\]
The experimental and fitted $I-q$ curves of pure DOPC multibilayer is plotted in Fig. 2.9b as an example of the fitting process. In Fig. 2.9c, the resulting parameters $I_0$, the chain-chain distance $a$ and chain correlation length $\xi$ are plotted against $\phi$, representing the parameters for the fraction of chain segments tilted at $\phi$. For a detailed explanation please see [64].

**Results and discussion**

![Figure 2.9](image-url)

Figure 2.9: (a) GISAXS patterns of DOPC multibilayers containing 10% $\beta$-peptide without $^b$Trp (9, 10 and 11) measured in the chain-correlation $q$ regime. The dashed lines denote $I_0$. Each colored line represents the intensity profile at the according $\phi$ angle. All images were recorded with 10 s exposure time. The false color scale corresponds to the logarithmic scattering intensity and the dark blue bar results from the beamstop.

(b) Experimental (stars) and fitted (solid lines) $I-q$ plots of pure DOPC, shown as an example of the fitting process.

(c) Lateral ordering parameters of the multibilayers derived from the fitting. The maximum of the Lorentzian $I_0$, chain-chain distance $a$, correlation length $\xi$ and their standard deviations are plotted as a function of $\phi$. 
First of all, by visual inspection alone, the 2d patterns suggest that the intensity of chain correlation peaks is dramatically decreased by \(\beta\)-peptide incorporation, indicating a lower lateral ordering which is expected for transmembrane peptides [140] and can thus be considered a further evidence for the transmembrane orientation. Secondly, the intensity decreases with \(\phi\) for DOPC but not in the presence of \(\beta\)-peptides, indicating a broader distribution function for the chain tilt probability due to \(\beta\)-peptide incorporation. This is exactly in line with the interpretation of the observed membrane thinning above. As a word of caution to the previous argument based exclusively on the lipid chain signal, however, we must also consider the fact that the structural peak of the \(\beta\)-helix itself gives rise to a maximum centered around \(q_z \sim 1.35 \text{ Å}^{-1}\), resulting in a helical pitch of \(p = 4.7 \text{ Å}\), which is in the same order of the literature value \(p = 5.0 \text{ Å}\) [110]. For further analysis of helical peaks please see previous work on helical form factors of \(\alpha\)-helices [140]. For tilted peptides, however, this signal may also be smeared out on an arc and merge into the chain correlation peak without clear separation. Therefore, the ring-shaped signal at high \(q_z\) may be a superposition of the chain-tilting signal and helical signal. Of course, this would then also confirm successful incorporation of the \(\beta\)-peptides into DOPC host bilayers, as already deduced from reflectivity.

Fig. 2.9c shows the parameters \((I_0, a \text{ and } \xi)\) deduced from the least-square fits as a function of \(\phi\). Again, the analysis is based on a decomposition of chain populations as a function of \(\phi\) [64, 140]. (i) The maximum intensity \(I_0\) of DOPC decays rapidly with \(\phi\), with main chain-tilting angle \(\leq 10^\circ\), similar as observed before for DOPC [64]. This reflects that the dominating fraction of lipids in the pure DOPC multibilayer are untitled. Contrarily, \(I_0-\phi\) curves of peptide-containing samples increase slightly with \(\phi\), indicating a broader distribution of chain tilt induced by tilted TMDs as well as a transmembrane conformation of the incorporated peptides. (ii) The average chain-chain distance \(a\) remains approximately constant \((4.82 \sim 5.38 \text{ Å})\), with respect to \(\phi\) and also between peptide-free and peptide-containing membranes. The width of all 3 \(\beta\)-peptides appear to be similar to DOPC so that the average chain-chain distance is not affected by peptide incorporation. (iii) For the peptide-free multibilayer, the correlation length \(\xi\) decreases with \(\phi\), in agreement with the fact that untitled lipids have a stronger chain-chain correlation than tilted ones [64]. In contrast for peptide-containing multibilayers, \(\xi\) is almost \(\phi\) independent. We thus assume that the helical signal should have largely attributed to \(\xi\) at high \(\phi\) angles.
2.4 Summary and outlook

In this chapter, we designed and synthesized two families of D-3\textsuperscript{14}-\(\beta\)-peptides, one with and one without additional \(h\text{Trp}\) anchors. In each peptide family, two of the three peptides were labeled with iodine to yield electron density contrast in either the tail region or the center region. These \(\beta\)-peptides were then incorporated into DOPC bilayers and characterized by CD spectroscopy, x-ray reflectivity and GISAXS. The CD spectra demonstrate the anticipated \(\beta\)-helical structures for all synthesized peptides including the ones with I-labels. X-ray reflectivity and GISAXS investigations together give rise to the following consistent picture: The \(\beta\)-peptides are successfully inserted into the model membrane stacks and form \(\beta\)-helical TMDs. The positive hydrophobic mismatch is relieved by a minor helical tilt, which also induces an increase in the number of chains with corresponding tilt angles. This in turn leads to membrane thinning and to a perturbation of the acyl chain packing. Additional \(h\text{Trp}\) anchors can effectively diminish the peptide tilt, hence less membrane thinning.

Having obtained the desired transmembrane 3\textsuperscript{14}-\(\beta\)-peptides in DOPC bilayers, in the future we can proceed with the design and synthesis of SNARE analogs containing \(\beta\)-helical TMDs, in association with various types of recognition motifs like DNA [108] and PNA [105], and linkers with different lengths [109].
3 Preparation of SNARE-reconstituted proteolomicelles, proteoliposomes and multibilayers

Part of this chapter is based on the manuscript: Y. Xu, J. Kuhlmann, M. Brennich, K. Komorowski, R. Jahn, C. Steinem and T. Salditt. Reconstitution of SNARE proteins into solid-supported lipid bilayer stacks and x-ray structure analysis. BBA – Biomembranes (submitted)

Soluble N-ethylmaleimide-sensitive factor attachment protein receptors (SNAREs) are a family of proteins which promote vesicle fusion [7]. Reconstituting SNAREs into supported multilayers can provide an ideal model system for high-resolution characterizations of SNARE-induced fusion in vitro. However, the use of organic solvent in the conventional multibilayer preparation [15,22] inhibits the reconstitution of membrane proteins. Therefore, in this work a novel vesicle-based protein-compatible protocol was developed, which was then employed to reconstitute SNAREs into supported multilayers via the micelle-vesicle-multibilayer pathway. This chapter is composed of (i) a brief introduction of SNAREs, (ii) basics of supported multibilayers, (iii) protein expression and purification, and the most importantly (iv) the preparation of SNARE-reconstituted proteolomicelles, proteoliposomes and multibilayers.

3.1 Fundamentals of SNAREs

After the discovery in the late 1980s [141], SNAREs immediately captured a lot of attention and were extensively studied due to their great significance for neuron transmission or more generally for membrane trafficking [142]. In the early stage it was believed that complementary assemble of SNAREs was a “universal mechanism” for imparting specificity to both regulated and constitutive vesicular membrane fusion (the SNARE hypothesis [143, 144]). In this hypothesis, the SNAREs couple with each other in an anti-parallel fashion whereas the energy needed for vesicle fusion is supplied by ATP hydrolysis from NSF [145]. However, later research has shown that SNAREs self-assemble into a 4-helix bundle from the N-terminal to the C-terminal in a zipper like fashion (Fig. 3.1 [142]).
Preparation of SNARE-reconstituted proteolmicelles, proteoliposomes and multibilayers

It is now commonly believed that this self-assembly supplies enough energy to overcome the repulsion between opposing membranes, pulls them into close contact and thus facilitates fusion [142, 146].

Various SNAREs are already found in Saccharomyces cerevisiae, in humans and in Arabidopsis thaliana [8]. They can be categorized into two groups, namely v-SNAREs (e.g. synaptobrevin and synaptotagmin) which anchor themselves in the synaptic vesicle membrane and t-SNAREs (e.g. syntaxin and SNAP25) which locate on the presynaptic plasma membrane. Despite the wide variety of SNAREs, they all contain SNARE motifs, which are recognized as “the minimal machinery” of membrane fusion [149]. The SNARE motifs are generally soft and flexible preceding the assembly of SNARE complexes [150]. Once formed, the coiled-coil structure is highly helical and stable, thanks to the ionic layer in the center of the coiled-coil (0 position in Fig. 3.2) and the 16 hydrophobic layers on both sides. Another important segment of SNAREs is the α-helical transmembrane domain (TMD) which can be found in both synaptobrevin and syntaxin, while SNAP25 anchors into the membrane via its palmitoyl side chain. Additionally, N-terminal domains can also be found at the distal end of many SNAREs.
3.2 Advantages of supported lipid multibilayers

In order to simplify the study of complex biological membranes, many model lipid bilayer systems have been developed, including black lipid membranes (BLMs) [152], vesicles [153], nanodiscs [154], supported lipid bilayers [155,156], etc. These model bilayer systems are depicted in Fig. 3.3.

All these model bilayers above are commonly used in membrane research and have their own advantage over others [157]. Supported lipid bilayers, either
solid-supported, polymer-supported or tethered (see Fig. 3.3d), offer a model bilayer system with remarkable membrane orientation and long-term stability, which enable high-resolution surface-sensitive characterizations such as Fourier transform infrared spectroscopy (FTIR), nuclear magnetic resonance spectroscopy (NMR), atomic-force microscopy (AFM), x-ray and neutron scattering, etc, [158]. For x-ray and neutron scattering in particular, the supports used for supported bilayers not only greatly suppress thermal fluctuations of free-standing bilayers (e.g. BLMs and vesicles) which diminish the bilayer lamellar ordering [17]; They also overcome the "powder averaging" problem of some model bilayers (e.g. vesicles) and hence give rise to stronger signal for x-ray and neutron scattering [159], due to the fact the all lipid molecules align themselves along the membrane normal.

Supported lipid multibilayers are composed of tens of up to thousands of lipid bilayers on a certain support, with thin water layers isolating different bilayers. Such multibilayers have several advantages over supported single bilayers. First of all, the constraints from the solid-support are reduced. Adding a spacer layer such as polymer or tether (Fig. 3.3d) could also achieve it, [160], but at the cost of additional preparation steps and system complexity. Most bilayers within a multibilayer are distant from the substrates and thus barely affected by them [161]. Secondly, single bilayers especially the ones prepared by spreading vesicle suspensions suffer from low covering rate, while multibilayers could almost cover 100% of the substrate surfaces.

For x-ray characterization of SNAREs in model bilayers in particular, the multibilayer structure brings several advantages: (i) The multibilayers structure could tremendously amplify the diffraction signal thanks to the increased bilayer number $N$, especially regarding the weak signal of the incorporated proteins. In multibilayers, both the readily existing helices and the helical structure of the four-helix bundle of SNAREs [150] may be effectively detected by e.g. GISAXS, which have been performed on mixed multibilayers of lipid/peptide before [140]. (ii) The opposing bilayers within a multibilayer stack can be easily directed into close contact by means of e.g. partial dehydration, which is a prerequisite for the functioning of many membrane proteins including SNAREs [162]. (iii) Finally and most importantly, our long-term goal is to reconstruct the 3-dimensional structure of the stalk in the presence of SNAREs, based on our previous experience from pure lipid multibilayers [21].
3.3 Existing preparation methods of supported lipid multibilayers

Several preparation methods have been developed to prepare supported lipid multibilayers, including Langmuir-Blodgett monolayer transfer, spreading organic solution (sOS) and spreading vesicle suspensions (sVS) (see Fig. 3.4).

Figure 3.4: Cartoon illustration of three different preparation techniques for multibilayers: (a) Langmuir-Blodgett monolayer transfer, (b) spreading organic solution (sOS) and (c) spreading vesicle suspension (sVS). The defect in the sVS multibilayer is caused by incomplete rupture of vesicles. The lipid organic solution is painted in yellow and the aqueous suspension in blue.
3.3.1 Langmuir-Blodgett monolayer transfer

Langmuir-Blodgett (LB) monolayers can be formed by self-assembly of amphiphilic molecules (e.g. detergents and lipids) at the air-water interface, with hydrophilic headgroups immersed in water and hydrophobic acyl chains heading upwards in the air [163]. These monolayers can be transferred onto substrates by vertically dipping and lifting the substrates in and out of the fluid (Fig. 3.4a). A monolayer is then deposited onto the substrate at each withdraw. By varying the number of withdraws either a supported single monolayer, a supported single bilayer or a supported multibilayer can be fabricated [24].

One strong advantage of the LB monolayer transfer is the precise manipulation of each monolayer [158]. Moreover, transmembrane proteins could be incorporated into LB monolayers [164], and could potentially be further introduced into multibilayers with integrity. On the other hand, it takes a lot of time and efforts to prepare multibilayers with this technique, since the monolayers have to be deposited one after another. In addition, the multibilayers prepared by LB monolayer transfer can not be well reproduced because of a variety of accompanying uncertainties such as complex thermal-dynamic and kinetic behavior, monolayer compression and the transfer process itself [22]. Another shortcoming of the LB method is that the higher monolayers do not transfer so well as the lower ones. Thus one could achieve up to merely \( \sim 50 \) bilayers [165], which fails to provide sufficient sample volume to x-ray characterizations.

3.3.2 Spreading organic solution (sOS)

Spreading organic solution (sOS) (Fig. 3.4b) is the most commonly used method for supported lipid multibilayers thanks to its ease of use and high efficiency. This protocol was first systematically investigated by Seul and Sammon [22] over 20 years ago on dipalmitoylphosphatidylcholine (DPPC) films using x-ray diffraction and electron microscopy. They found out that a variety of membrane defects could be observed on sOS films, in contrast to the rather defect-free surfaces of LB films. Nevertheless, the sOS films are still highly oriented and able to yield up to 12 Bragg peaks for x-ray reflectivity experiment on dry films. The sOS method thus offers a rapid preparation of lipid multibilayers highly suitable for x-ray study, as long as the proper solvent mixture, lipid concentration and substrate are chosen. In this initial study, about only 50 bilayers could be fabricated. Later on, by optimizing preparation conditions, lipid multibilayers of up to several hundred or thousand bilayers could be achieved [15, 166],
yielding even higher effective sample volume for x-ray studies. It is considered as the most adequate preparation method for pure lipid [167] and lipid/peptide systems [132, 168]. However, the use of organic solvent inhibits the preparation of complex multibilayers containing membrane proteins by this method, as it may lead to protein denaturation.

### 3.3.3 Spreading vesicle suspension (sVS)

One of the less common preparation methods for lipid multibilayers is the spreading vesicle suspension (sVS) method (Fig. 3.4c), which can be performed both with and without proteins [169, 170]. The preparation process is composed of two main steps: (i) Lipid vesicles are first prepared, resized and refined with various techniques such as vortex, sonication, size-exclusion, extrusion, dialysis, etc.; (ii) Vesicle suspensions are then spread onto substrates so that vesicles rupture into planar bilayer upon evacuation. This approach is developed from the classic vesicle-based deposition of single lipid bilayers [155, 171]. The major difference between these two methods is that for single bilayer preparation only a single layer of vesicles adsorb onto the solid-supports and slowly rupture into single bilayers in the presence of buffer solutions; while for bilayer stacks bulk vesicle suspensions are forced to dry and deposit on the substrate surface to form multibilayers during water evaporation.

Results have shown that such vesicle-based multibilayers could be well characterized by x-ray reflectivity [169]. This method should be able to achieve the reconstitution of SNAREs into supported multibilayers which are suitable for x-ray characterizations. However, the orientation and lamellar ordering of such multibilayers are not yet determined and the reconstitution rate of the desired protein remains also unclear [24]. In order to properly take advantage of this method, special attention has to be paid to these two issues during the development of the novel protocol.

### 3.4 Expression and purification of SNAREs

#### 3.4.1 Protein constructs

Both the SNARE expression and purification procedures follow the protocol described in detail elsewhere [172]. The SNAREs including syntaxin-1A
Preparation of SNARE-reconstituted proteolmicelles, proteoliposomes and multibilayers

(Syx1A), SNAP-25B (SN25B) and synaptobrevin 2 (Syb2) from Rattus norvegicus were used in this study, with all expression constructs performed in *Escherichia coli* cells with the pET28a vector. More specifically, the full length Syb2 (aa 1-116), one of the natural vesicular SNARE components, was directly used as the v-SNARE for this study, while the soluble C-terminal segment of Syb2 (aa 49-96) was assembled together with the C-terminally truncated Syx1A (aa 183-288, including its SNARE motif and TMD) and SN25B (aa 1-206, with all its cysteine replaced by serine) to form a the ΔN acceptor complex (hereinafter referred to in short as ΔN complex or simply ΔN), which was used as the t-SNARE complex for this study. They assembly process of ΔN was carried out at 4°C for overnight with an excess of SN25B (1:1:1.5) in the presence of 1% CHAPS. All SNARE components used in this work are sketched in Fig. 3.5.

3.4.2 ΔN acceptor complex

Most of the fusion experiments of SNAREs are performed with Syb2 and the 2:1 complex of Syx1A/SN25, where the binding site of Syb2 is occupied by an extra syntaxin with its TMD being truncated (Fig. 3.5 [150, 173]). In this mechanism, the rate of full SNARE complex assembly is predominately determined by the competitive displacement between Syb2 and the extra Syx1A. Unfortunately, this rate is considerably slow (hour-scale) in contrast to the millisecond-scale fusion processes in *vivo*. Pobbat et al. [148] thus developed a novel t-SNARE complex denoted as ΔN acceptor complex, which is composed of a 1:1 Syx1A/SN25 complex stabilized by the C-terminal soluble segment of Syb2 (Fig. 3.5). They found that Syb2 could bind to ΔN rapidly, similar to the unstabilized 1:1 complex of Syx1A/SN25. The reason is that the 4-helix assembly initiates from the N-termini which is not occupied in ΔN. Later research has confirmed that this novel complex does promote rapid fusion and thus enables more comprehensive monitoring of the whole fusion process [174, 175].

3.4.3 Protein purification

H-tags were first cleaved by thrombin digest overnight. A Ni2+-nitrilotriacetic acid affinity chromatography was then performed followed by an ion exchange chromatography. MonoQ ion-exchange column (GE Healthcare) was used for Syx1A and SN25B while MonoS (GE Healthcare) for both full length and the soluble segment Syb2. After assembly, the ΔN complex was further purified by ion
exchange chromatography with MonoQ. The SNAREs with TMD were always handled in the presence of 1% CHAPS. Stocks containing SNAREs were snap-frozen with liquid nitrogen and stored at -80 °C for further use.

### 3.5 SNARE reconstitution into supported multibilayers by sVS

The whole spreading vesicle suspension (sVS) protocol is illustrated by Fig. 3.6 where it is divided into three stages according to the morphology of the aggregates, namely the proteomicelle stage, the proteoliposome stage and the multibilayer stage.
Figure 3.6: Cartoon illustration of the sVS protocol (i.e. the micelle-vesicle-multibilayer pathway). Stage 1: The SNAREs are incorporated into the detergent/lipid mixed micelles to form proteomicelles. Stage 2: After going through the Sephadex columns for 2 times, proteoliposomes transform into proteoliposomes since n-OG is removed by size-exclusion chromatography. Stage 3: Resulting proteoliposome suspension is spread onto the substrate so that supported multibilayers form upon water evaporation. Syb2 is used as an example of reconstituted SNAREs. A certain number of vesicles underwent incomplete ruptures, hence membrane defects.

3.5.1 Stage 1: proteomicelles

The proteomicelles containing SNARE were prepared by the co-micellization method following [148, 176]. All lipids were purchased from Avanti Polar Lipids (Alabaster, AL, USA) and used without further purification. Primarily two lipid mixtures were used for this thesis, the quaternary mixture of PC-PE-PS-Chol and the binary mixture of PC-PE. Among them, PC-PE-PS-Chol is close to the lipid composition of synaptic vesicle membrane (SM not included). It is thus considered highly suitable for the preparation of unilamellar vesicles and for SNARE fusion [177]. On the other hand, PC-PE mixture has been extensively reported to be able to form highly aligned supported multibilayers [21, 25, 78]. As a result, PC-PE acts as the main multibilayer-forming mixture in this study.

First of all, 1 mg of lipid mixtures with/without 0.67 wt% Texas Red (TR, Eugene, Oregon, USA) was separately dissolved by the mixed solvent of chloroform/TFE (1:1 vol/vol) and dried under mild nitrogen flow for 1 h. Especially, PS was dissolved by isopropanol due to its poor solubility in chloroform/TFE. The lipid
films were then dried in vacuum for 2 h to fully remove the organic solvents. 1.8 mg n-octyl-β-D-glucoside (n-OG) was added to 50 µL buffer solution containing 20 mM 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid (HEPES), 100 mM KCl and 1 mM dithiothreitol (DTT). Due to the fact that the n-OG concentration (~120 mM) was much higher than its CMC (25 mM), detergent/lipid mixed micelles formed spontaneously (Fig. 3.4a [178]). The dry lipid films were re-dissolved by the resulting n-OG micelle suspension. Subsequently, the n-OG/lipid mixed suspension was vortexed every 5 min for 3 times to homogeneously mix them. ΔN and Syb suspensions were taken out of the -80 °C freezer and thawed under room temperature. 2 aliquots (~8 µM) of either ΔN or Syb suspension containing 1% CHAPS were pipetted into the n-OG/lipid mixed micelle suspension at the protein/lipid ratio of 1:500 [176]. After incubation on ice for 30 min, SNAREs anchored into the readily formed n-OG/lipid mixed micelles, hence proteomicelles containing SNAREs. Resulting suspensions contained rather high amount of n-OG which was to be removed by the later size-exclusion chromatography.

### 3.5.2 Stage 2: proteoliposomes

The first Sephadex G-25 size-exclusion column (Illustra NAP-25, GE Healthcare) was equilibrated with buffer by eluting 5 ml reconstitution buffer through the column for 3 times. The proteoliposome suspensions then passed through the first column so that the n-OG could be removed. As the n-OG got washed away, proteoliposomes transformed into proteoliposomes (Fig. 3.4b) due to the decrease of the overall packing parameter. The second G-25 column was equilibrated with ultrapure water by eluting 5 ml MilliQ water through the column for 3 times as well. After eluting the vesicle suspension with the second column, the remaining salt from the buffer was also removed. After being concentrated to 10 mg/ml (Concentrator plus, Eppendorf), proteoliposome suspensions were stored in refrigerator at 4 °C for later deposition of supported multibilayers. In addition, two pure-lipid vesicle suspensions were prepared either by the same method only without SNAREs, or by sonicking 1 mg lipid film together with 2 ml ultrapure water.

### 3.5.3 Stage 3: supported multibilayers

Similar to the wafer processing in the last two chapters, silicon wafers (Silchem, Freiberg, Germany) were first polished, cut to 10 × 15 mm² pieces and cleaned
by 15 m ultrasonic bath with ultrapure water and methanol iteratively for 5 times in total. Since the vesicle suspensions can not spread out so well as organic solutions on hydrophobic surfaces, here the Si wafers were especially plasma treated (PDC-002, Harrick) under constant O\textsubscript{2} flow for 10 m. A highly hydrophilic SiO\textsubscript{2} layer was then fabricated on top of each Si wafer so that the vesicle suspensions spread out once deposited. Note that the wafers should be directly used after plasma-cleaning, otherwise adsorption of dust from the air could re-hydrophobize the wafer surface.

In order to prepare multibilayers containing both ΔN and Syb, 50 μl ΔN and 50 μl Syb proteoliposome suspensions were first gently mixed and co-incubated at room temperature. Afterwards, the suspension containing both ΔN and Syb was spread onto a Si wafer which was then transported into a vacuum desiccator. Over-night evacuation was performed so that H\textsubscript{2}0 was thoroughly removed (Fig. 3.4c). As water evaporated, the vesicles began to rupture and formed planar bilayers on top of each other [179]. Noticeably, incomplete ruptures could lead to a large number of membrane defects whose effect should be carefully investigated by the x-ray characterizations below. A series of control multibilayers were prepared in parallel: (i) pure lipid multibilayer by sOS, (ii) pure lipid multibilayer by sVS, (iii) the multibilayer containing only ΔN and (iv) the multibilayer containing only Syb.
4 SAXS studies of SNARE-reconstituted proteomicelles and proteoliposomes

Part of this chapter is based on the manuscript: Y. Xu, J. Kuhlmann, M. Brennich, K. Komorowski, R. Jahn, C. Steinem and T. Salditt. Reconstitution of SNARE proteins into solid-supported lipid bilayer stacks and x-ray structure analysis. BBA-Biomembranes (submitted)

In the last chapter, I have presented the newly established sVS protocol for the reconstitution of SNAREs into supported multibilayers. This protocol is composed of three stages including the proteomicelle stage, and proteoliposome stage and the multibilayer stage. For both the proteomicelle and the proteoliposome stages, the SNARE containing aggregates exist in the suspension phase, which can be properly characterized by SAXS as well as dynamic light scattering (DLS). In this chapter, I first present the experimental setup and physical theory of solution SAXS, then seek to reveal the structural information of both micelles and vesicles with the help of appropriate fitting models, and finally evaluate the influence of preparation techniques, lipid compositions and SNARE reconstitution on micelle and vesicle structures.

4.1 Beamline BM29

The BM29 beamline (BioSAXS) is a newly upgraded beamline at ESRF particularly designed for SAXS experiments on biological macromolecules in solution [180]. It features tunable beam energy (7-15 keV, 12.5 keV by default), higher flux (up to $2 \times 10^{13}$ photons/s) and smaller beamsize ($\leq 500 \times 500 \mu$m) compared to the previous ID14-3 beamline. These upgrades enable high-resolution SAXS detection in relatively short time scale.

The BM29 beamline (Fig. 4.1) is located on the bending-magnet dipole with a 0.85 T magnetic field and a 20.35 keV critical energy. After passing through the white beam slits and the water-cooled mask, the x-ray beam is monochromated by a water-cooled double multilayer monochromator, whose exit beam shifts slightly (5 $\mu$m) when the beam energy varies. A set of metal filters are installed right behind the monochromator. They are made of Fe, Cu and Pt re-
Figure 4.1: BM29 beamline layout adapted from [180], re-drawn with permission. The distances between key components are noted under the layout. The toroidal mirror converts the divergent beam to convergent, which is not shown in the layout. The detector can be moved accordingly to provide the proper q range.

spectively, whose adsorptions edges fall right in the energy range of the beam. Further downstream a 1.1 m Rh coated cylindrical toroidal mirror is installed to focus the monochromated beam. Finally the beam is defined by a set of beam cleaning slits, which deliver a 0.7×0.7 mm² size beam on the sample with 130 µrad divergence. A flight tube, a beamstop (located in the flight tube), a diode (integrated into the beamstop) and a Pilatus 1M detector (DECTRIS) are placed downstream the sample position. Pilatus 1M is a pixel detector composed of 10 units and 981 × 1043 pixels in total (172 × 172 µm² each pixel). The sample-detector distance can be adjusted accordingly with respect to the desired q range. The BM29 beamline is aimed at high throughput as well as the ease of use. To this end, the entire beamline is highly automated on both the hardware and software sides as shown below.

4.1.1 Automatic sample changer

The sample changer is equipped with a robot system of multiple functions: automatic sample loading and unloading, sample chamber cleaning and drying, which are controlled by a simple software installed right next to the sample changer (Fig. 4.2 [183]). Three types of sample plates can be used for sample storage: (i) metal plate with 4×8 sample positions for standard PCR tubes (0.2 ml, Eppendorf, Germany) and 4×8 buffer positions for microcentrifuge tubes (1.5 or 2.0 ml, Eppendorf, Germany), (ii) 96 well plate with shallow wells and (iii) 96 well plate with deep wells. The internal temperature can be set between 2-60 °C. More importantly, after the samples are loaded and the experimental hutch closed, all sample/buffer delivery as well as x-ray exposures are controlled by the beamline operating software BsxCuBE [183].
Figure 4.2: The automatic sample changer system of BM29 beamline [181, 182]. All three types of samples plates are mounted in the loading position of the sample changer in the photo. Functions like sample loading/unloading, chamber cleaning/drying and temperature control are achieved using the sample loading interface shown in the upper right corner.

4.1.2 BsxCuBE operating software, EDNA pipeline and ISPyB database

The BsxCuBE (Biosaxs Customized Beamline Environment) operating software is installed on the main computer in the control hutch. After mounting the sample solutions into one or more of the three sample plates and loading them, users can edit the sample information and choose experimental parameters using the BsxCuBE software before starting a measurement. Sample information could be input by editing the excel-like interface as shown in Fig. 4.3 [182, 183]. Essential information that users have to constantly modify includes type (buffer or sample), row (A-D for the metal plate), concentration (mg/ml), well (1-11 for the metal plate), name of the macromolecule, name of the buffer and volume (20-120 µl, ideally 50 µl). Note that this table should be saved as a new file prior to exposures. Later a couple of other parameters shall be carefully chosen for the entire measurement. They include directory, prefix, run, frame (10 by default), time per frame (1 s by default) and radiation damage. With all these being set, the users can finally open the shutter (the “open” button) and start the measurement (the “collect” button). BsxCuBE will automatically run the measurement according to the given sample sequence. Immediately after
recording, 2d exposures are azimuthally integrated to yield a series of 1d intensity profiles.

The EDNA-driven [184] online data-processing pipeline first disposes the exposures with radiation damage, averages the chosen 1d intensity profiles and subtracts the SAXS data of buffer solution from the SAXS curves of the suspensions. Later on, it also performs “routine” data analysis including Kratky analysis, Guinier approximation and Porod approximation [180]. In the end, the sample information table, data processing and routine data analysis are uploaded to the ISPyB (Information System for Protein crystallography Beamlines) database (Fig. 4.4 [185]). Users are able to view, edit and download them after logging in to the ISPyB website with their user account.

4.1.3 Experimental settings

All suspensions prepared in the last chapter were characterized at BM29 BioSAXS beamline with identical beamline settings. Briefly, the photon energy was set to 12.5 keV and the beam size was set to $700 \times 700 \mu m^2$ at the exposure capillary by the beam-cleaning slits. The Pilatus 1M detector was mounted
2.867 m away from the capillary, resulting in a $q$ range between 0.003-0.495 Å$^{-1}$. Sample suspensions and pure buffer solutions (HEPES buffer for micelles and MillQ water for vesicles) were first pipetted into the automatic sample changer before measurements. For micelles, the original suspensions (∼ 1 mg/ml) were used. For vesicles, both the original suspensions and concentrated suspensions (∼ 5-10 mg/ml) were measured. After properly setting the sample information and measurement parameters, BsxCuBE then automatically delivered the sample suspensions and buffer solutions into the exposure capillary and recorded 10 frames of 1 s for each suspension/solution. The EDNA-driven pipeline automatically performed routine analysis, which failed to provide structural information of the micelles and vesicles as it is designed for solution SAXS of macromolecules. We thus performed specific structural analysis with proper models as shown below.
4.2 General SAXS theories

Small-angle x-ray scattering is a powerful technique to probe a wide variety of macromolecules and particles from the nm up to µm scale, which is relatively large compared to the short wavelength of x-ray (e.g. 1.54 Å for Cu-Kα emission) [186]. Therefore, the corresponding x-ray scattering signal of such macromolecules and particles fall into the small angle range, in contrast to the wide angle of atomic structures.

Fig. 4.5 sketches the typical data collection process of SAXS experiments. A monochromatic x-ray beam is first defined by a series of x-ray optics such as pinholes. Considering the fact that small-angle x-ray signal can be easily affected by misalignment of the beam or the scattering from the optics [187], special attention has to be paid to delivering clean beam onto the sample. The well-aligned x-ray beam then hits the sample and is scattered by the macromolecules inside the sample-holding capillary, with the scattering signal interfering with each other. The scattered wave projects onto a pixel detector to yield a 2-dimensional (2d) diffraction pattern. The pixel detector is usually mounted far away from the sample so that more information in the small-angle regime can be detected. Finally, the 2d diffraction pattern is azimuthally averaged, resulting in 1-dimensional (1d) intensity profiles against the incident angle θ or scattering vector modulus $q$, with $q = 4\pi \sin \theta / \lambda$ [188].

Figure 4.5: Schematic illustration of typical SAXS data collection. A monochromatic beam first passes through a set of pinholes, strikes the sample and scatters onto a 2d pixel detector. After being azimuthally integrated the intensity $I$ is plotted against the scattering vector modulus $q$ to yield 1d $I$-$q$ plot. Both 2d and 1d results are plotted in logarithmic scale.
The scattering intensity of an ideal single particle $I_{sp}$ in vacuum is proportional to the square of its form factor $F_{sp}$:

$$I_{sp} \sim |F_{sp}(q)|^2 = \left| \int_{V_{sp}} \rho_{sp}(r) \cdot \exp(iq \cdot r) dr \right|^2. \quad (4.1)$$

$q$ is the scattering vector in reciprocal space and $r$ is the position vector in real space. Since particles do not exist on their own, we should consider the scattering from the environment (e.g. aqueous solution for lipidic aggregates) so that

$$I_{sp} \sim |F_{sp}(q)|^2 = \left| \int_{V_{sp}} \Delta \rho(r) \cdot \exp(iq \cdot r) dr \right|^2. \quad (4.2)$$

Here $\Delta \rho$ is the electron density contrast between a particle and its environment. When bulk particles coexist in one environment and are distant from each other (i.e. weak inter-particle correlation), the total scattering intensity is simply a summary of intensities of all particles [188]. For anisotropic particles, an averaging over all directions has to be performed [189], yielding

$$I_{av} \sim \langle |F_{av}(q)|^2 \rangle = \int_0^{2\pi} d\Phi \int_0^{\pi} |F_{sp}(q)|^2 \sin \theta d\theta. \quad (4.3)$$

Here $\Phi_r$ and $\theta_r$ are the polar and azimuthal angles in the spherical coordinate system, respectively. For particles of different shapes, the form factors can be further derived with proper models. In particular, the modeling of micelles and vesicles will be presented below. Here the scattering intensity is denoted in kDa based on the molecular weight derived from the forward scattering intensity $I_0$ [183, 190, 191].

### 4.3 SAXS modeling and fitting of proteomicelles

Micelles are aggregates of surfactants mostly formed in aqueous solutions, with a hydrophilic headgroup shell separating the solution and inner hydrocarbon core [192]. Micelles can adopt several different shapes such as sphere, ellipsoid (globular shape) and cylinder [193]. For each of these shapes, a specific model can be applied to calculate its form factor $F$. 
4.3.1 The form factor of cylindrical micelles

For a uniform (the electron density $\rho$ is a constant) cylindrical particle with radius $R$ and height $2H$, its form factor can be written as [194]:

$$F_c(q) = 2V_c \Delta \rho \frac{\sin(u_H)}{u_H} \times \frac{J_1(u_R)}{u_R}, \quad (4.4)$$

where $u_H = qH \cos \theta$, $u_R = qR \sin \theta$ and the cylinder volume $V_c = 2\pi HR^2$. $J_1$ is the first order spherical Bessel function. As we have introduced above, each surfactant micelle consists of a hydrophilic shell and a hydrophobic carbon core. Hence we can treat them as two-component cylinders with inner radius $R_1$, inner electron density $\rho_1$, outer radius $R_2$ and outer density $\rho_2$. By adding up the form factor of the shell and the core, we obtain

$$F_c(q) = 2V_1(\rho_1 - \rho_2) \frac{\sin(u_H)}{u_H} \times \frac{J_1(u_R_1)}{u_{R_1}} + 2V_2(\rho_2 - \rho_s) \frac{\sin(u_H)}{u_H} \times \frac{J_1(u_R_2)}{u_{R_2}}. \quad (4.5)$$

With Eq. 4.3 we then perform the orientational averaging [189, 195], yielding

$$\langle F_c(q)^2 \rangle = \int_0^\pi \left[ 2V_1(\rho_1 - \rho_2) \frac{\sin^2(u_H)}{u_H^2} \times \frac{J_1^2(u_R_1)}{u_{R_1}^2} + 2V_2(\rho_2 - \rho_s) \frac{\sin^2(u_H)}{u_H^2} \times \frac{J_1^2(u_R_2)}{u_{R_2}^2} \right] \sin \theta d\theta. \quad (4.6)$$

4.3.2 The form factor of spherical and ellipsoidal micelles

The form factor of a uniform sphere can be written as [196]

$$F_s(q) = 3V_s \Delta \rho \frac{\sin(qr) - qr \cos(qr)}{(qr)^3} = 3V_s(\rho - \rho_s) \frac{J_1(qr)}{qr}, \quad (4.7)$$

in which $V_s$ is the volume of the sphere, and $J_1$ is the first order spherical Bessel function. For an ellipsoid with one axis of length $a$ and two axes of length $b$ (spheroid) as illustrate in Fig 4.6, the $qr$ term can be replaced by $u = q(a^2 \cos^2 \theta + b^2 \sin^2 \theta)^{1/2}$. $\theta$ is again the polar angle in spherical coordinate system. The form factor of an ellipsoid $F_e$ can be written as

$$F_e(q) = 3V_s(\rho - \rho_s) \frac{J_1(u)}{u}. \quad (4.8)$$
4.3 SAXS modeling and fitting of proteomicelles

![Diagram of the 2-component ellipsoid model](image)

Figure 4.6: Left: Sketch of the 2-component ellipsoid model, which is composed of 1 semi-axis of length a and 2 semi-axis of length b, with t_a and t_b being the corresponding thickness of the outer shell. Right: Molecular illustration of possible arrangement of the detergents and lipids in our mixed micelles.

Similar to the two-component cylinders, here we introduce two-component ellipsoids with two discrete electron densities: \( \rho_1 \) for the core and \( \rho_2 \) for the shell. The total form factor is obtained by adding up the form factor of the inner core and outer shell, yielding

\[
F_e(q) = (3V_1(\rho_1 - \rho_2)\frac{J_1(u_1)}{u_1} + 3(V_1 + V_2)(\rho_2 - \rho_s)\frac{J_1(u_2)}{u_2}),
\]

in which \( \rho_s \) is the electron density of the solution, \( u_1 = q(a^2 x^2 + b^2 \sin^2 \theta)^{1/2} \),

\[
u_2 = q((a + t_a)^2 \cos^2 \theta + (b + t_b)^2 \sin^2 \theta)^{1/2},
\]

the inner volume \( V_1 = 4/3\pi ab^2 \), and the total volume \( V_1 + V_2 = 4/3\pi(a + t_a)(b + t_b)^2 \), with \( a \) and \( b \) being the axis length of the inner core and \( t_a \) and \( t_b \) being the thickness of the outer shell (see Fig. 4.6). Micelles are oblate if \( a < b \), spherical if \( a = b \) and prolate if \( a > b \).

Finally performing orientational averaging with Eq. 4.3 results in [195, 196]

\[
\langle F_e(q)^2 \rangle = \int_0^\pi [(3V_1(\rho_1 - \rho_2)\frac{J_1(u_1)}{u_1} + 3(V_1 + V_2)(\rho_2 - \rho_s)\frac{J_1(u_2)}{u_2})^2 \sin \theta d\theta. \quad (4.10)
\]

### 4.3.3 SAXS fitting of n-OG/PC-PE-PS-Chol micelles with the ellipsoid model

LIPFERT et al. have successfully fitted the n-OG micelles with the 2-component ellipsoid model [196, 197]. We apply this model to fit the SAXS data of our OG/lipid mixed micelles and n-OG/lipid/SNARE proteomicelles. Additionally, a scaling factor \( s \) and a constant background \( f \) are introduced to yield the final intensity, with

\[
I_e = s\langle F_e(q)^2 \rangle + f. \quad (4.11)
\]
The \textit{lsqnonlin} function from the Optimization Toolbox in MATLAB (MathWorks Inc.) is used to perform the fitting. The goodness of fit is evaluated by the the reduced $\chi^2$ \cite{198, 199}:

\[
\chi^2_{\text{red}} = \frac{\sum_{n=1}^{N} (I_{\text{exp},n} - I_{\text{fit},n})^2}{\sigma_n^2} \frac{1}{N - p - 1}.
\] (4.12)

$I_{\text{exp},n}$ and $I_{\text{fit},n}$ are the experimental and fitted intensities of the $n^{th}$ data point, respectively. $\sigma_n$ is the Poisson error of the $n^{th}$ data point. $p$ is the number of free model parameters to $N$ data points. Appendix B.2 shows the MATLAB script to calculate the scattering intensity. In total 9 free parameters are fitted, including $a$, $b$, $t_a$, $t_b$, $\rho_1$, $\rho_2$, $s$ and $f$.

First of all, we use n-OG/PC-PE-PS-Chol 5:2:2:1 mixed micelles as an example to figure out the proper fitting strategy for our micelle data. The SAXS curve of the n-OG/PC-PE-PS-Chol 5:2:2:1 micelle suspension is subtracted by the data of buffer. Both prolate and oblate fitting are performed within the $q$ range of 0.050-0.495 Å$^{-1}$. Fitting curves are compared with the experimental curves in Fig. 4.7, and the fitting results are summarized in Tab. 4.1.

Fig. 4.7 shows the experimental and fitting curves of the (a) oblate and (b) prolate ellipsoid model. Generally both models are able to roughly describe the SAXS data, with only minor residuals being observed. However, systematic discrepancies appear in both cases, indicative of an oversimplified model. In particular, the present mixed micelles cannot be fully characterized by a uniform headgroup, as they incorporate both lipids and detergents in the highly mixed regions. The two-component ellipsoid model may therefore fail to properly fit the data, accentuating the usual deficiencies of the model in the high $q$ range \cite{196, 200}. For the prolate shape, a more significant 1\textsuperscript{st} minimum ($q = 0.09-0.11$ Å$^{-1}$) can be observed on the experimental curve rather than on the fit. This is unlikely to happen in SAXS curve fitting as many experimental conditions tend to smear out low-intensity SAXS signal. Next we inspect the structural parameters obtained from fitting.

Tab. 4.1 tabulates the fitting results of Fig. 4.7. The geometrical parameters, namely $a$, $b$, $t_a$, $t_b$. Both shapes result in reasonable inner core thickness $a$ and $b$, which are comparable to the literature values \cite{49, 196}. The outer shell thickness $t_a$ and $t_b$ however, vary dramatically with the shapes. The oblate shape leads to unequal $t_a$ and $t_b$, i.e. heterogeneous lipid and n-OG distribution. In contrast, $t_a$ and $t_b$ of the prolate model are almost equal, indicating homogeneously mixed micelles. As discussed above, such a homogeneous molecular
distribution in the mixed micelles should not result in systematic discrepancies between SAXS curves and their fits. We then take a look at the electron densities \(\rho_1\) and \(\rho_2\). Compared with literature values [76, 196], the oblate model provides reasonable results for both \(\rho_1\) and \(\rho_2\), whereas the electron densities of the prolate model are significantly lower than the values therein. Lastly, the reduced \(\chi^2\) of the oblate model is profoundly lower, also indicating that the oblate shape is more suited to our micelle data. Based on reasons above, we deduce that the mixed micelles in this study adopt the oblate ellipsoid shape. This result is well in line with previous observations that n-OG/PC micelles are “flattened” [201, 202]. As all the mixed micelles in this study share the same main composition (n-OG/PC-PE-PS-Chol), the oblate ellipsoid model is hence also used to fit the SAXS data of proteomicelles below.
4.3.4 SAXS fitting of n-OG/PC-PE-PS-Chol/SNARE proteomicelles with the oblate ellipsoid model

Having determined the proper fitting model, we now use it to fit the SAXS data of SNARE-reconstituted proteomicelles. Three types of micelles exist in our preparation, namely (i) n-OG/PC-PE-PS-Chol 5:2:2:1 micelles, (ii) n-OG/PC-PE-PS-Chol/ΔN proteomicelles and (iii) n-OG/PC-PE-PS-Chol/Syb proteomicelles. Their SAXS data are fitted with the 2-component oblate ellipsoid model introduced above.

![SAXS curves](image)

Figure 4.8: (a) SAXS curves (colored circles) and their fits (black lines) of (i) n-OG/PC-PE-PS-Chol, (ii) n-OG/PC-PE-PS-Chol/ΔN, and (iii) n-OG/PC-PE-PS-Chol/Syb micelles, plotted on a logarithmic scale. The micelle mass concentration (total surfactant and lipid) is ∼ 36 mg/ml. Data in the q range of 0.050-0.495 Å⁻¹ is fitted, as indicated by the vertical dashed line. The intensities at q → 0 are marked by arrows. By virtue of the instrument’s calibration in absolute units, the scattering intensity can be expressed in terms of (effective) molar mass of an equivalent protein solution. The experimental errors of the first and last fitted data points are plotted in cyan. (b) Residuals of the two-component ellipsoid fits corresponding to the fits shown in (a). (c) 2d sketch of the possible molecular arrangement of the n-OG/PC-PE-PS-Chol/Syb proteomicelle, using the micelle size determined by fitting (Tab. 4.2) and PDB molecular structures. The sketch is assembled “by hand” using PyMOL.

Fig. 4.8a shows the SAXS curves (colored circles) of (i) n-OG/PC-PE-PS-Chol, (ii) n-OG/PC-PE-PS-Chol/ΔN, and (iii) n-OG/PC-PE-PS-Chol/Syb micelles. All
4.3 SAXS modeling and fitting of proteomicelles

Table 4.2: Fitting results of the SAXS data of n-OG/PC-PE-PS-Chol (5:2:2:1), n-OG/PC-PE-PS-Chol/ΔN and n-OG/PC-PE-PS-Chol/Syb micelles. Only data in the q range of 0.050-0.495 Å⁻¹ is fitted, using the two-component oblate ellipsoid model.

<table>
<thead>
<tr>
<th>Samples</th>
<th>a [Å]</th>
<th>b [Å]</th>
<th>ρ₁ [e/Å³]</th>
<th>ρ₂ [e/Å³]</th>
<th>qₐ [Å]</th>
<th>qₐ [Å]</th>
<th>s</th>
<th>f</th>
<th>χ²_red</th>
</tr>
</thead>
<tbody>
<tr>
<td>n-OG/PC-PE-PS-Chol</td>
<td>11.66±0.22</td>
<td>28.65±0.34</td>
<td>0.24±0.00</td>
<td>0.46±0.01</td>
<td>11.09±0.41</td>
<td>3.38±0.17</td>
<td>1.44×10⁻⁵</td>
<td>4.19</td>
<td>22.22</td>
</tr>
<tr>
<td>n-OG/PC-PE-PS-Chol/ΔN</td>
<td>11.97±0.11</td>
<td>36.82±1.29</td>
<td>0.24±0.00</td>
<td>0.47±0.01</td>
<td>12.64±0.26</td>
<td>5.00±0.40</td>
<td>0.67×10⁻⁵</td>
<td>4.44</td>
<td>8.56</td>
</tr>
<tr>
<td>n-OG/PC-PE-PS-Chol/Syb</td>
<td>11.87±0.13</td>
<td>31.40±0.43</td>
<td>0.25±0.00</td>
<td>0.47±0.01</td>
<td>12.59±0.27</td>
<td>2.71±0.22</td>
<td>1.10×10⁻⁵</td>
<td>4.42</td>
<td>12.80</td>
</tr>
</tbody>
</table>

Curves exhibit the typical functional form of micelles [203], with only small systematic changes except for \( I(q \to 0) \), where the curve corresponding to the ΔN-containing micelles exceeds the value of the Syb-containing micelles by a factor of about 7 and that of the protein-free micelles by a factor of 9. This change is indicative of a certain degree of protein aggregation, as we discuss further below. As a model-free parameter, the dominant head group to head group length \( L \) can be derived from the 2nd peak positions without any model fit [197]. All mixed micelles showed similar \( L \) (36.61-40.02 Å), with the SNARE-containing micelles being slightly larger (40.02 Å for ΔN and 37.85 Å for Syb) than the pure n-OG/lipid micelles (36.61 Å). These parameters are verified by model fitting using the two-component oblate ellipsoid model that we have determined above, which introduces more micelle structural parameters. The fits are plotted in Fig. 4.8a (black lines) and the fitting parameters are summarized in Tab. 4.2. For all micelles, the model fits describe the experimental data sufficiently well in the fitted region \((q = 0.050-0.495 \text{ Å}^{-1})\), as indicated by the low fitting residuals plotted in Fig. 4.8b.

Parameters in Tab. 4.2 show that the geometrical parameters, namely the core thickness \( a \) and \( b \), the shell thickness \( t_a \) and \( t_b \), increase only slightly for the SNARE-containing suspensions, in good agreement with the model-free parameter \( L \) above. In order to interpret these structural results, we must keep in mind that the SAXS corresponds to an ensemble, i.e. an average over SNARE-containing and SNARE-free micelles within the illuminated volume. According to the stoichiometric estimation in Appendix C.1 we expect only \( \sim 9\% \) of the micelles to contain a SNARE protein. The SAXS signal is thus dominated by the protein-free micelles, which explains the observation that all curves give very similar micelle parameters. However, larger aggregations must be present in the ΔN-containing solution. To see this, we first compute an upper bound for the total mass of a SNARE-containing micelle. From the fitted geometrical form factors of the micelles and the known composition and stoichiometry of
surfactants and lipids, we obtain values in the range of 70-80 kDa. We add it to the molecular masses of the protein $M_{\Delta N} = 40.993$ kDa, or $M_{Syb} = 12.69$ kDa, respectively, and compare this sum to the molecular mass extracted from $I(q \to 0)$ of the calibrated scattering intensity. Note that the molecular masses of the instrument apply to protein solutions, assuming a protein mass density of $\rho_P = 1.35 \text{ g/cm}^3$ [191]. Therefore, $I(q \to 0) = 2263 \text{ kDa/(mg/ml)}$ of the $\Delta N$ curve must be scaled with the corresponding contrast ratio (micelle-to-water/protein-to-water). Taking this into account along with the concentration $c \approx 36 \text{ mg/ml}$, we get values well in excess of 120 kDa, which we consider evidence of aggregation. At the same time, we presume that not all $\Delta N$-containing micelles aggregate based on the clarity of the solution. Finally, we note that in view of problems associated with aggregation and averaging over inhomogeneous scatterers, the systematic discrepancies are not surprising, but since the residuals are comparable for all curves, we still conclude that the main limitation of this model is the over-simplistic description of the micellar structure [196, 200]. Nonetheless, the small averaged expansion of the micelles does indicate a measurable response of the system to SNARE reconstitution into the n-OG/lipid micelles, so that the SNARE reconstitution into vesicles can be subsequently performed.

### 4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

Several models can be used to calculate the vesicle form factor $F$. Among them, the two most common are the sphere model and the flat bilayer model. They are both able to properly model a large variety of vesicles [204]. In this section, the form factors of these two models are derived from literature [189,204], while only the flat bilayer model is applied to actual vesicle fitting due to its simplicity. Fitting results of both pure lipid vesicles and SNARE-reconstituted proteoliposomes are presented. For pure lipid vesicles in particular, not only the commonly used vesicle-forming mixture PC-PE-PS-Chol [172] but also other lipid mixtures including PC-PE, PC-PE-Chol, PC-PE-PIP$_2$, etc. are investigated, in order to shed light on the effect of lipid composition on vesicle structures.
4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

4.4.1 Gaussian electron density profiles

Unlike micelles, for which the 2-component model is used, vesicle bilayers are modeled by \( n \) Gaussian shells, with each of them representing a certain moiety of the bilayer [189, 205]. Hence the overall electron density profile is a summation of \( n \) Gaussian functions:

\[
\rho(r) = \sum_{k=1}^{n} \rho_k \exp\left[ -\frac{(r - \delta_k)^2}{2\sigma_k^2} \right],
\]

(4.13)

where \( \delta_k \) is the distance between the Gaussian shell and the vesicle center, and \( \sigma_k \) is the width (standard deviation) of the Gaussian shell. With the EDP in hand, we now introduce the derivation of the form factor \( F(q) \) for both the sphere model and flat bilayer model [204].

4.4.2 The form factor of spherical vesicles

The form factor of sphere structures can be derived from the radically-symmetric Fourier transform of Eq. 4.13 [204]:

\[
F_s(q) = 2q^{-1} \sum_{k=1}^{n} \rho_k \sigma_k \exp(-q^2 \sigma_k^2/2) \left[ \delta_k \sin(q \delta_k) + \sigma_k^2 q \cos(q \delta_k) \right].
\]

(4.14)

The term \( \sigma_k^2 q \cos(q \delta_k) \) is relatively small and can thus be ignored. We then obtain

\[
F_s(q) = 2q^{-1} \sum_{k=1}^{n} \rho_k \sigma_k \delta_k \exp(-q^2 \sigma_k^2/2) \sin(q \delta_k).
\]

(4.15)

No orientational averaging is needed thanks to the spherical shape. Instead, we have to average \( F_s(q) \) over vesicle radii \( R \) for a population of non-uniform vesicles. A Gaussian function with average radius \( R_0 \) and standard deviation \( \sigma_R \) can be introduced to describe the vesicle size distribution [204]. After a normalized ensemble average we finally obtain:

\[
\langle F_s(q)^2 \rangle = q^{-2} \sum_{k,k'} (R_0 + \epsilon_k)(R_0 + \epsilon_{k'}) \rho_k \rho_{k'} \sigma_k \sigma_{k'} \exp\left[ -\frac{q^2(\sigma_k^2 + \sigma_{k'}^2)}{2} \right] \times \cos\left[ q(\epsilon_k - \epsilon_{k'}) \right].
\]

(4.16)

Here \( \delta \) is replaced by \( R + \epsilon \) where \( \epsilon \) is the relative position of the Gaussian shell with respect to the bilayer center.
4.4.3 The form factor of bilayer-like vesicles

Vesicles that are large enough \((R > 25 \text{ nm})\) can be considered as flat bilayers when performing x-ray characterization. A simple 1d Fourier Transform of the EDP in Eq. 4.13 results in

\[
F_f(q) = q^{-1} \sum_{k=i}^{n} \rho_k \sigma_k \exp(-q^2 \sigma_k^2/2) \exp(i q \delta_k). \tag{4.17}
\]

No orientational averaging is needed if we assume that the vesicles are a “perfect powder”, i.e. bilayers have random orientation \([204]\). \(\langle F_f(q)^2 \rangle\) can be directly calculated with \(\langle F_f(q)^2 \rangle = F_f(q) F_f(q)^*\) and therefore,

\[
\langle F_f(q)^2 \rangle = q^{-2} \sum_{k,k'} \rho_k \rho_{k'} \sigma_k \sigma_{k'} \exp[-q^2(\sigma_k^2 + \sigma_{k'}^2)/2] \times \cos[q(\epsilon_k - \epsilon_{k'})]. \tag{4.18}
\]

Here \(\delta\) is again replaced by \(\epsilon\), so that \(d_{hh} = |\epsilon_1 - \epsilon_3|\).

From previous \([172]\) and our own dynamic light scattering data (shown below in Fig. 4.17) we gain the knowledge that our vesicles are large enough \((R > 25 \text{ nm})\) so that the curvature effect can be ignored. As a result, both the sphere model and the flat bilayer model are well suited. As the sphere form factor \(F_s\) contains a lot more fitting parameters, we choose the simpler flat bilayer model to fit the scattering intensity \(I_f\). A scaling factor \(s\) and a constant background \(f\) is added in the calculation, yielding

\[
I_f = s \langle F_f(q)^2 \rangle + f. \tag{4.19}
\]

Fitting is performed with the \texttt{lsqnonlin} function from the Optimization Toolbox in MATLAB (MathWorks Inc.). The goodness of fit is again evaluated by the the reduced \(\chi^2\) as introduced in Section 4.3.3. Appendix B.1 summaries the preparation and fitting conditions of all vesicles investigated in this work, and Appendix B.3 shows the MATLAB script to calculate the scattering intensity.

4.4.4 SAXS fitting of pure lipid vesicles with the bilayer model

As we have discussed in great detail in Chap. 1, lipid compositions can largely influence bilayer properties. In this subsection, vesicles of various pure lipids are carefully investigated by SAXS. Some of them are lipid mixtures commonly used for vesicle preparation such as PC-PE-PS-Chol \([172]\) and PC-PE-Chol-SM \([79]\),
4.4 SAXS modeling and fitting of pure lipid vesicles and
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while the others are the “magic mixtures” candidates that we have characterized in Chap. 1. These include PC-PE, PC-PE-Chol and PC-PE-PIP₂, which are more suitable for multibilayer preparation. Although in this study only PC-PE 4:1 vesicles are utilized for multibilayer deposition, in the future others could also be potentially used to yield multibilayers with higher orientation and fusigenicity.

**PC-PE-Chol**

Fig. 4.9 shows the SAXS curves of PC-PE-Chol vesicles prepared by (a) the column method, i.e. the co-micellization/size-exclusion routine and (b) the sonication method (See Chap. 3). The first impression we could obtain from the SAXS curves is that all vesicles possess a multibilayer structure, as indicated by the characteristic Bragg peaks [205]. This property might result from the lack of charged lipid in the current vesicle composition, such as PS, PG and PIP₂ [207]. Charged lipids are able to prevent bilayers from stacking onto each other due to the electrostatic effect.

<table>
<thead>
<tr>
<th>Samples</th>
<th>$d$ [Å] (column)</th>
<th>$d$ [Å] (sonication)</th>
</tr>
</thead>
<tbody>
<tr>
<td>PC-PE 1:1</td>
<td>54.87 ± 2.10</td>
<td>60.88 ± 1.90</td>
</tr>
<tr>
<td>PC-PE + 5% Chol</td>
<td>55.36 ± 1.11</td>
<td>61.18 ± 2.13</td>
</tr>
<tr>
<td>PC-PE + 10% Chol</td>
<td>57.96 ± 1.96</td>
<td>61.72 ± 1.44</td>
</tr>
<tr>
<td>PC-PE + 20% Chol</td>
<td>60.36 ± 2.30</td>
<td>63.21 ± 2.15</td>
</tr>
<tr>
<td>PC-PE-Chol-SM (Nat.’s Own)</td>
<td>-</td>
<td>66.03 ± 2.55</td>
</tr>
</tbody>
</table>

Table 4.3: Bilayer periodicity $d$ of PC-PE-Chol vesicles prepared by (left) column and (right) sonication. Additionally the $d$ of the “nature’s own fusogenic mixture” [79] vesicles prepared by sonication is also included. The standard deviations are shown after ±.

We first compare the SAXS curves within each preparation. The SAXS curves appear similar to each other for vesicles prepared by the same method, despite the difference in Chol concentration. Chol might be able to incorporate themselves into the PC-PE 1:1 vesicles without leading to significant bilayer-vesicle modification. When we compare the SAXS curves between the two methods, distinct lineshapes can be observed. The PC-PE and PC-PE-Chol vesicles prepared by the column method seem to be highly multibilayer, with 2 Bragg orders appearing in the SAXS curves. In contrast, PC-PE and PC-PE-Chol vesicles prepared by the sonication method are close to unilamellar, with the Bragg peaks being considerably weak and hardly observable. The sonication process seems to supply external energy to destabilize the multibilayer structure [207].

The fitting of multibilayer vesicles involves rather complicated modeling and
Figure 4.9: SAXS curves of PC-PE-Chol vesicle suspensions prepared by (a) the column method and (b) the sonication method. Curves are shifted for clarity and the lipid concentrations in the two series are ~4 and 5 mg/ml respectively. PC-PE molar ratio is kept at 1:1 with Chol concentration increasing from top to bottom. Pure H$_2$O is used for both samples (no buffer). Bragg peaks due to the multilamellar structure are observed for all vesicles suspensions.

requires relatively high data quality [205]. Therefore, we simply take a look at the bilayer periodicity $d$ Tab. 4.3 instead, which can be easily calculated with the positions of the Bragg peaks without any model fitting. When Chol is added to PC-PE 1:1 vesicles, $d$ increases continuously with Chol concentration, from 54.87 up to 60.34 Å for the column method, and from 60.88 up to 66.03 Å for the sonication method. Assuming that the bilayer thickness $d_{hh}$ increases linearly with $d$ under the same hydration condition [20], this result is well in line with the fact that Chol leads to an increase in $d_{hh}$ [208]. Interestingly, PC-PE-Chol vesicles prepared by the sonication method have generally thicker bilayers compared by the column method. Since their lipid compositions and the sample environment (ultrapure H$_2$O) are the same, we assume that there is some n-OG remaining in the vesicles prepared by the column method. n-OG has a much short chain length and hence can largely reduce the bilayer thickness of long-chain lipids [209]. In our case the column method is capable of efficiently remove most n-OG during the fast preparation process, but fails to thoroughly remove it.
4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

“Nature's own fusiogenic mixture” (PC-PE-Chol-SM)

![SAXS curves of “Nature's own fusiogenic mixture”](image)

Figure 4.10: SAXS curves of “Nature's own fusiogenic mixture” (PC-PE-Chol-SM 35:30:15:20) and “Nature's own fusiogenic mixture” doped with 10% PS (PC-PE-Chol-SM-PS), prepared by sonication. For both samples only pure H₂O is used (no buffer). The lipid concentrations is 5 mg/ml and curves are vertically shifted for clarity.

As introduced in Chap. 1, the “nature's own fusiogenic mixture” (PC-PE-Chol-SM 35:30:15:20) has a lipid composition close to synaptic vesicle membrane and forms high fusiogenic vesicles with low rupture rate [79]. In this section, firstly PC-PE-Chol-SM vesicles prepared by sonication were investigated by SAXS whose curve is shown in Fig. 4.10 (blue). The SAXS curve exhibits two clear Bragg peaks, in contrast to the only 1 Bragg order from PC-PE-Chol vesicles by sonication (Fig. 4.9b). We already know that Chol barely changes the vesicle structure of PC-PE 1:1, while it seems that SM largely strengthens the multibilayer structure possibly due to the coupling effect of SM and Chol. Tab. 4.3 shows that the \(d\) of PC-PE-Chol-SM is 66.03 Å, much larger than the PC-PE-Chol vesicles prepared by the same method (60.88-63.21 Å). This result is in good agreement with other experiments where SM strongly increased the bilayer thickness due to its high chain-ordering [210].

Along with PC, PE, Chol and SM, PS is also an essential lipid type in synaptic vesicles. Therefore, it would be meaningful to add PS into the “Nature's own fusiogenic mixture” to make it complete. In this study, 10% PS was thus mixed with PC-PE-Chol-SM to form vesicles with a lipid composition even closer to the synaptic vesicle membrane.
Fig. 4.10 shows the SAXS curve (red) of PC-PE-Chol-SM-PS vesicle suspension, which demonstrates a typical unilamellar SAXS lineshape. When comparing it with the SAXS curve of PC-PE-Chol-PS (blue), the most significant difference is the disappearance of the Bragg peaks. It is interesting to gain the knowledge that 10% PS could already effectively prevent multibilayer formation in the sonication preparation. This finding is also in line with the fact that synaptic vesicles only exhibit unilamellar structures in nature. The two SAXS curves almost overlap with each other except for the Bragg peak region, indicating a similar bilayer structure despite different stacking geometries.

**PC-PE-PIP$_2$ and its reaction to salt**

PIP$_2$ is a negatively charged lipid with a massive headgroup, one saturated and one unsaturated acyl chain. During synaptic vesicle fusion, it can bind to synaptotagmin and accelerate its response to Ca$^{2+}$ [43]. Here PIP$_2$ was incorporated into PC-PE 1:1 to facilitate unilamellar PC-PE-PIP$_2$ vesicles via sonication. Vesicles of pure PC-PE 1:1 were also prepared by sonication to serve as the control sample. Due to the fact that PC-PE 1:1 vesicles typically show multilamellar structures (see Fig. 4.9), subsequent extrusion [127] (50 nm pore size) was carried out to yield unilamellar PC-PE 1:1 vesicles for better comparison.

Their SAXS curves are plotted in Fig. 4.11 (colored). We first try to use the symmetric flat bilayer model to fit these curves. The fitting curves are shown by Fig. 4.11 (black), and the fitting results are summarized in Tab. 4.4. By comparing the SAXS and fitting curves, it is obvious that the symmetric flat bilayer model well fits the PC-PE 1:1 curve in the entire $q$ range and the PC-PE-PIP$_2$ curves in the high $q$ regime ($q > 0.09 \, \text{Å}^{-1}$), but not PC-PE-PIP$_2$ curves in the low $q$ regime ($q < 0.09 \, \text{Å}^{-1}$). Moreover, the bilayer thickness $d_{hh}$, the most important fitting parameter, seems to stay constant despite the increase of the PIP$_2$ concentration. However, our previous study [20] reveals that the addition of PIP$_2$ increases the $d_{hh}$ of DOPC bilayers continuously. Therefore, despite that all EDPs show the typical bilayer lineshape, the SAXS curves of PC-PE-PIP$_2$ can not be properly fitted by the symmetric flat bilayer model. We thus turn to the asymmetric flat bilayer model.

Fig. 4.12 shows the SAXS curves of PC-PE-PIP$_2$ (colored) and the fitting curves of the asymmetric flat bilayer model (black). Note that The PC-PE 1:1 curve is still fitted with the symmetric model because above we have already proven it to be suitable for this particular sample. The fitting parameters are summarized in Tab. 4.5. It is apparent that the asymmetric flat bilayer model fits the PC-PE-
4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

Figure 4.11: (left) SAXS curves (colored) and fitting curves (black) of PC-PE 1:1 vesicles doped with PIP$_2$ prepared by sonication. For all samples only pure H$_2$O is used (no buffer). The lipid concentration is 5 mg/ml and curves are vertically shifted for clarity. The symmetric flat bilayer model with a constant background $f$ is used to fit all curves. Only the data in the $q$ range of 0.050-0.495 Å$^{-1}$ is fitted, as indicated by the dashed line. (right) EDPs (arbitrary units) derived from the fitting results of the SAXS curves.

<table>
<thead>
<tr>
<th>Samples</th>
<th>$\varepsilon_1$[Å]</th>
<th>$\rho_1$[a.u.]</th>
<th>$\sigma_1$[Å]</th>
<th>$\sigma_2$[Å]</th>
<th>$d_{hh}$[Å]</th>
<th>$s$</th>
<th>$f$</th>
<th>$\chi^2_{\text{red}}$</th>
</tr>
</thead>
<tbody>
<tr>
<td>PC-PE 1:1</td>
<td>-18.18±0.39</td>
<td>1.24±0.12</td>
<td>3.48±0.04</td>
<td>7.91±0.33</td>
<td>36.36</td>
<td>0.08</td>
<td>0.51</td>
<td>3.90</td>
</tr>
<tr>
<td>PC-PE + 5% PIP$_2$</td>
<td>-18.10±0.39</td>
<td>1.17±0.11</td>
<td>4.27±0.05</td>
<td>8.88±0.35</td>
<td>36.20</td>
<td>0.05</td>
<td>0.42</td>
<td>0.95</td>
</tr>
<tr>
<td>PC-PE +10% PIP$_2$</td>
<td>-18.00±0.38</td>
<td>1.09±0.11</td>
<td>4.95±0.06</td>
<td>9.21±0.36</td>
<td>36.00</td>
<td>0.05</td>
<td>0.48</td>
<td>1.31</td>
</tr>
<tr>
<td>PC-PE +20% PIP$_2$</td>
<td>-18.11±0.39</td>
<td>1.20±0.12</td>
<td>6.38±0.09</td>
<td>12.41±0.39</td>
<td>36.22</td>
<td>0.05</td>
<td>0.62</td>
<td>1.90</td>
</tr>
</tbody>
</table>

Table 4.4: Fitting results of PC-PE 1:1 vesicles doped with PIP$_2$ prepared by sonication, using the symmetric flat bilayer model with a constant background $f$. The bilayer thickness $d_{hh}$ is calculated with the positions of the first and last Gaussian shell $\varepsilon_1$ and $\varepsilon_3$. The values after ± are the standard deviations.
SAXS studies of SNARE-reconstituted proteomicelles and proteoliposomes

Figure 4.12: (left) SAXS curves (colored) and fitting curves (black) of PC-PE 1:1 vesicles doped with PIP₂ prepared by sonication. For all samples only pure H₂O is used (no buffer). The lipid concentration is 5 mg/ml and curves are vertically shifted for clarity. The symmetric flat bilayer model is used for PC-PE 1:1 and the asymmetric flat bilayer model is used for the others, both with a constant background f. Only the data in the q range of 0.030-0.495 Å⁻¹ is fitted, as indicated by the dashed line. (right) EDPs (arbitrary units) derived from the fitting results of the SAXS curves.

Table 4.5: Fitting results of PC-PE 1:1 vesicles doped with PIP₂ prepared by sonication. The symmetric flat bilayer model is used for PC-PE 1:1 and the asymmetric flat bilayer model is used for the others, both with a constant background f. The bilayer thickness d_{hh} is calculated with the positions of the first and last Gaussian shell ε₁ and ε₃. The values after ± are the standard deviations.
4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

Figure 4.13: SAXS curves of PC-PE-PIP$_2$ vesicles in 2.5 mM CaCl$_2$ solution. The lipid concentration is 5 mg/ml. All curves show typical multilamellar lineshape with the bilayer periodicity $d \approx 59.28$ Å. Curves are vertically shifted for clarity.

PIP$_2$ curves much better than the symmetric model. Both in the low and high $q$ regime, the fitting curves highly match the experimental curves. Moreover, $d_{hh}$ exhibits a continuous increase with the PIP$_2$ concentration except for the PC-PE 1:1 vesicle, well in line with our previous observation [20]. We can therefore reasonably assume that the PC-PE-PIP$_2$ bilayers bear certain degrees of asymmetry. This assumption is confirmed by the weakening of the maxima and minima upon the addition of PIP$_2$, which has been reported to be possibly caused by membrane asymmetry [204]. Such an asymmetric distribution of PIP$_2$ also agrees with the fact that in $vivo$ PIP$_2$ largely exists in the cytoplasmic (inner) leaflet [211]. Such an asymmetry in $vitro$ in the absence of cations and proteins perhaps originate from its multivalence [212] (a net charge of -3 at neutral pH [213]).

For PC-PE-PIP$_2$ vesicles in ultrapure water, a unilamellar structure is always obtained due to the high number of charges in PIP$_2$. CaCl$_2$ was then added into the existing PC-PE-PIP$_2$ vesicle suspensions, arriving at a final CaCl$_2$ concentration of 2.5 mM. The suspensions were then immediately characterized by SAXS, whose results are shown in Fig. 4.13. For all PIP$_2$ concentrations, the unilamel-
lar structures transform into multilamellar as indicated by the characteristic Bragg peaks. It is indeed an interesting finding that the addition of CaCl$_2$ can eliminate PIP$_2$'s effect on the formation of unilamellar vesicles, which is in line with the fact that Ca$^{2+}$ can bind to negatively charged lipids and screen their electrostatic effects [214]. When more PIP$_2$ is present, this screening effect is less significant and the multilamellar order is lower, as indicated by the diminishing of the $2^{nd}$ Bragg peak. In the future this phenomena could be further investigated, possibly with respect to salt concentration and salt penetration into vesicle interiors.

### 4.4.5 SAXS fitting of proteoliposomes with the bilayer model

More importantly for the establishment of the novel sVS protocol, proteoliposomes composed of PC-PE-PS-Chol 5:2:2:1 or PC-PE 4:1 prepared via the co-micellization/size-exclusion routine (i.e. the column method) are also investigated by SAXS.

**PC-PE 4:1**

We have learned from the last section that PC-PE forms highly multilamellar vesicles in pure H$_2$O, especially when no sonication is performed. In this section, the PC-PE 4:1 vesicles were reconstituted with SNAREs and evaluated by SAXS.

Fig. 4.14 shows the SAXS curves of pure PC-PE 4:1 vesicle suspension (blue), (ii) PC-PE/$\Delta$N proteoliposome suspension (red), (iii) PC-PE/Syb proteoliposome suspension (green) and (iii) PC-PE/$\Delta$N+Syb proteoliposome suspension (purple), prepared by the column method. Bragg peaks are found in all SAXS curves indicating multibilayer structures, due to the lack of charged lipids. A noticeable feature of the SAXS curve of $\Delta$N containing vesicles is the strong intensity in the low $q$ region. This has occurred in the micelle SAXS section and can be attributed to the aggregation as we demonstrate below. Moreover, the SAXS curve of proteoliposome suspensions containing both $\Delta$N and Syb appears to be a simple average of the SAXS curves of unmixed $\Delta$N and Syb proteoliposome suspensions. This indicates that fusion events did not take place in large quantity during the short time (~ a few minutes) after mixing.

The bilayer periodicity $d$ of pure PC-PE (59.84 Å) is slightly smaller than the ones containing SNAREs, with $d = 63.53$ Å for $\Delta$N, 60.00 Å for Syb and 60.64 Å
4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

Figure 4.14: SAXS curves of SNARE-reconstituted PC-PE 4:1 vesicles prepared by the column method. Only pure H$_2$O is used (no buffer). The lipid concentration $\approx$ 7 mg/ml and the protein/lipid ratio $\approx$ 1:500. Some curves are vertically shifted for clarity. All curves show the typical multilamellar lineshape with the bilayer periodicity $d$ $\approx$ 59.84-63.53 Å. The position of the first Bragg peak is marked by the vertical line across all curves.

for the mixture of $\Delta$N and Syb. First of all, this result perfectly agrees with our observation in the micelle section that SNAREs slightly enlarge the micelles, with $\Delta$N brings about more profound modification than Syb. The $d$ of mixed suspensions falls in between the $d$ of unmixed suspensions, again indicating a lack of fusion events. We then performed 30 min incubation at room temperature on the mixed suspensions to inspect whether sufficient fusion events could occur to introduce significant structural alteration.

Fig. 4.15 shows the SAXS curves on the mixed proteoliposome suspensions before (0 min) and after incubation (30 min). It is obvious that two SAXS curves largely overlap with each other. Although currently no fitting has been performed due to the complexity of multilamellar vesicle fitting, we could still deduce from the lineshapes that 30 min of incubation at room temperature did not bring them into fusion on a large scale. One possible reason for this is the
Figure 4.15: SAXS curves of PC-PE 4:1 vesicles containing both $\Delta N$ and Syb before and after incubation. The first curve was obtained right after mixing the two proteoliposome suspensions (0 min) while the second curve was obtained 30 min after mixing. The two curves highly overlap with each other.

Table 4.6: Fitting results of the SAXS data of (i) pure PC-PE-PS-Chol 5:2:2:1 suspension prepared by sonication (Soni.), (ii) pure PC-PE-PS-Chol, (iii) PC-PE-PS-Chol/$\Delta N$, (iv) PC-PE-PS-Chol/Syb and (v) PC-PE-PS-Chol/$\Delta N$+Syb vesicle suspensions prepared by the column method. The values after $\pm$ are the standard deviations. The bilayer thickness $d_{hh}$ is calculated with $d_{hh} = 2|\varepsilon_1|$.

lack of salt in ultrapure water. In fusion assays, vesicle suspensions usually contain “fusion buffer” in order to promote rapid fusion [215].

**PC-PE-PS-Chol 5:2:2:1**

A lipid composition more suitable for unilamellar vesicle preparation, PC-PE-PS-Chol 5:2:2:1 is applied to the SNARE proteoliposomes as well. Besides the PC-PE-PS-Chol 5:2:2:1 vesicles prepared via the column method, pure PC-PE-PS-Chol vesicles were also prepared by sonication to serve as a detergent-free control sample.

Fig. 4.16a shows the SAXS curves (colored circles) and the fits (black lines) of (i)
4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

Figure 4.16: (a) SAXS curves (colored circles) and their fits (black lines) of (i) PC-PE-PS-Chol vesicles prepared by sonication, (ii) PC-PE-PS-Chol, (iii) PC-PE-PS-Chol/ΔN, (iv) PC-PE-PS-Chol/Syb and (v) PC-PE-PS-Chol/ΔN+Syb vesicles prepared by size-exclusion. Both are plotted on a logarithmic scale and shifted for clarity. The mass concentration of the lipid is ~ 7 mg/ml. Data in the q range of 0.075-0.495 Å⁻¹ is fitted, as indicated by the vertical dashed line. The intensities of q → 0 are again marked by arrows. The experimental errors of the first and last fitted data points are plotted in cyan. (b) Corresponding residuals of the fits to the symmetric flat-bilayer model. (c) Electron density profiles reconstructed with the obtained fitting parameters in Tab. 1b.

PC-PE-PS-Chol vesicles prepared by sonication, (ii) PC-PE-PS-Chol, (iii) PC-PE-PS-Chol/ΔN, (iv) PC-PE-PS-Chol/Syb and (v) PC-PE-PS-Chol/ΔN+Syb vesicles prepared by size-exclusion. Firstly all SAXS curves display the typical unilamellar lineshape. The third maxima appear in all SAXS curves due to the relatively high lipid concentration (5 mg/ml for (i) and 7 mg/ml for the others), while the previously measured 1 mg/ml vesicles suspensions of the same type provided only 2 maxima (data not shown). Unlike in Section 4.3.4, where the intensity of the ΔN-containing proteomicelles clearly indicates strong aggregation, here the scattering intensity of the ΔN-containing proteoliposomes does not stand out from the crowd. We will look further into this effect by dynamic light scattering in the coming section. Lastly, the SAXS curve of the mixed suspension of PC-PE-PS-Chol/ΔN and PC-PE-PS-Chol/Syb is also an average of the curves of
the unmixed ones, the same as the PC-PE 4-1 proteoliposomes. No other dis-
similarities are found between curves from visual comparison.

The fitting results are summarized in Tab. 4.6. They show that bilayer thick-
nesses $d_{hh}$ of the investigated vesicles vary considerably with the preparation
methods and the compositions. Firstly the bilayer of pure PC-PE-PS-Chol ves-
icle prepared by sonication ($d_{hh} = 37.52 \, \text{Å}$) is thicker than the one prepared
by size-exclusion ($d_{hh} = 36.08 \, \text{Å}$). As they have the same lipid composition,
the only appropriate explanation is that there was fairly abundant detergent
(mainly n-OG) left in the bilayers, which inserted into the lipid bilayers in a
wedge-like fashion [216] and lead to bilayer thinning [209]. Secondly for sVS
vesicles of PC-PE-PS-Chol/\(\Delta N\) ($d_{hh} = 38.28 \, \text{Å}$) and PC-PE-PS-Chol/Syb ($d_{hh} =
36.76 \, \text{Å}$), $d_{hh}$ is increased with respect to PC-PE-PS-Chol (protein-free control).
This is somewhat similar to the observed swelling of micelles discussed above.

In contrast to the micelles, however, the protein copy number of a vesicle is
much larger than one, in fact for 100% reconstitution efficiency we expect 44
proteins for a $R = 30 \, \text{nm}$ vesicle (see Appendix C.2). Given the still low protein-
to-lipid ratio $P/L = 0.002$, we cannot expect however to see a large contribution
of the “protein shell” around the bilayer. For this reason, it is plausible that the
electron densities reflect mainly the small changes which the protein reconsti-
tution brings to the lipid matrix, i.e. proteins are sensed only indirectly at this
$P/L$. For comparison, Fig. 4.16c shows the electron density profiles (EDPs) of all
5 types of vesicle bilayers reconstructed with the fitting parameters in Tab. 4.6.
They show that the bilayer structure is not significantly altered by SNARE recon-
stitution, apart from the minor membrane thickening. Lastly, almost all fitting
parameters of the mixed vesicles (PC-PE-PS-Chol/\(\Delta N+\text{Syb}\)) are approximately
the average of the non-mixed ones. It is likely that full fusion brings about no
observable changes to the SAXS results, as long as the flat bilayer model is used
to describe the data, i.e. as long as we are insensitive to the vesicle radius. How-
ever, we should be able to detect characteristic signals from docking and hemi-
fusion. Since the SAXS curve of the mixed SNARE vesicles (purple) is roughly
the average of the curves of single SNARE vesicles (red and green), we cannot
identify any such effect.

### 4.4.6 Dynamic light scattering investigation of PC-PE-PS-Chol/
SNARE proteoliposomes

From the micelle SAXS results we have deduced that the \(\Delta N\) proteomicelles
undergo strong aggregation. One could then reasonably suspect that the \(\Delta N-\)
4.4 SAXS modeling and fitting of pure lipid vesicles and SNARE-reconstituted proteoliposomes

Figure 4.17: (a) DLS correlation curves and (b) size distributions of proteoliposomes of (i) pure PC-PE-PS-Chol prepared by sonication, (ii) pure PC-PE-PS-Chol, (iii) PC-PE-PS-Chol/ΔN and (iv) PC-PE-PS-Chol/Syb prepared by the column method. Proteoliposome suspensions were diluted to 0.01 mg/ml and no buffer was added (pure H₂O only). Measurements were performed on ALV/CGS-3 laser light scattering goniometer system (ALG-GmbH, Langen, Germany), equipped with a 22 mW HeNe laser (λ = 632.8 nm) at 90° scattering angle. All vesicles share a radius $R_0 \approx 30$ nm, with ΔN showing a unique $R_1 \approx 150$ nm.

containing proteoliposomes might inherit this effect, which is not clearly shown by the vesicle SAXS data in Fig 4.16a. In this section, dynamic light scattering (DLS) is employed to further investigate the size distribution of these vesicles. Additionally, this technique can also quantitatively reveal vesicle populations when the proper weighting method is applied [217].

Fig. 4.17 shows the correlation curves and particle-size distributions of pure PC-PE-PS-Chol vesicles and PC-PE-PS-Chol/SNARE proteoliposomes, including (i) pure PC-PE-PS-Chol vesicles prepared by sonication, (ii) pure PC-PE-PS-Chol vesicles, (iii) PC-PE-PS-Chol/ΔN proteoliposomes and (iv) PC-PE-PS-Chol/Syb proteoliposomes prepared by the column (size-exclusion) method. The experimental auto-correlation functions (Fig. 4.17a) are fitted by logarithmic number-weighted algorithm to yield the size distribution functions (Fig. 4.17b). All vesicles share a mean radius $R_0 \approx 30$ nm with small peak width. It is rather surprising to find that the vesicles prepared by column and sonication exhibit similar size distributions. The shared mean radius $R_0$ indicates comparable vesicle sizes, and the small peak width indicates considerable monodispersity resulting from both methods. In addition, proteoliposomes prepared by the column method generally exhibit size distributions similar to pure lipid vesicles by the same method, confirming that SNARE reconstitution barely al-
ters vesicle structures. The only difference is the unique mean radius $R_0 \approx 150$ nm found in the size-distribution function of PC-PE-PS-Chol/ΔN. This result on the one hand verifies our suspect that the ΔN-containing proteoliposomes inherit the aggregation from the ΔN-containing proteomicelles on the other hand demonstrates that the majority of vesicles is however in an unaggregated fraction with radii in the expected size range around $R_0 \approx 30$ nm. In other words, despite a small degree of vesicle aggregation, most ΔN-containing proteomicelles remains mono-disperse. Therefore, we can nevertheless progress to Stage 3 of the sVS protocol (multibilayer) with the resulted proteoliposomes.

4.5 Summary and outlook

In this chapter, proteomicelles, pure lipid vesicles and proteoliposomes have been investigated by solution SAXS, with the data being fitted by appropriate models. We find out that (i) SNAREs are successfully reconstituted into both micelles and vesicles, leading to minor thickening effect without vastly changing their original structures; (ii) non-charged lipid mixtures exhibit multilamellar structures while charged ones formed unilamellar vesicles via co-micellization and size-exclusion; (iii) Chol, PIP$_2$ and SM (Nature's Own Lipid Mixture) are incorporated into PC-PE vesicles, resulting in an expected thickening effect on the bilayers; (iv) compared with the column method, sonication yields vesicles with lower multilamellar fraction, which could be further reduced by extrusion; (v) a small proportion of the ΔN-containing proteoliposomes aggregate, resulting in; while the majority of them remain mono-disperse; (vi) no coupling effect of ΔN and Syb can be detected even after 30 min of incubation.

SAXS results of SNARE-reconstituted micelles and vesicles together support a simple picture of protein reconstitution. The SNAREs anchor themselves into the host aggregates via the TMDs, leading to minor structural modifications in the detergent and lipid assembly. These findings provide adequate information both for the current protocol and for future refinement. More importantly, they validate the sVS preparation in Stage 1 and 2, which is a prerequisite for the following deposition of multibilayers (Stage 3).
5 X-ray characterizations of SNARE-reconstituted multibilayers

Part of this chapter is based on the manuscript: Y. Xu, J. Kuhlmann, M. Brennich, K. Komorowski, R. Jahn, C. Steinem and T. Salditt. Reconstitution of SNARE proteins into solid-supported lipid bilayer stacks and x-ray structure analysis. BBA-Biomembranes (submitted)

Having determined structures of the proteomicelles and proteoliposomes (Stage 1 and 2 of the sVS protocol, Fig. 3.6), we now proceed to the characterization of sVS multibilayers (Stage 3 of the sVS protocol), with the ultimate goal of 3d EDP reconstitution of the stalk structure in the presence of SNARE complexes ahead. In this chapter, multibilayers containing SNAREs are studied by x-ray reflectivity and grazing-incidence small-angle x-ray scattering (GISAXS). This chapter starts with the preliminary results of the GISAXS investigation on SNARE-containing multibilayers at ID01, ESRF. It is followed by the results of systematic in-house investigation of x-ray reflectivity and GISAXS. PC-PE mixtures are selected as the main lipid composition for multibilayer preparation in this work based on our previous finding that it is able to form highly aligned bilayer stack with rhombohedral phases forming at relatively high RHs (low osmotic pressure) [21,25].

5.1 GISAXS characterizations of SNARE-reconstituted multibilayers at ID01

In the early stage of the development of the sVS method, SNAREs were reconstituted into both PC-PE and PC-PE-PS-Chol multibilayers always in an mixed fashion, aiming at stalk formation in the presence of coupled SNARE complexes.

5.1.1 Beamline setup

The ID01 undulator beamline has already been introduced in Chap. 1 and 2. Briefly, multibilayers were mounted in the software-controlled humidity cham-
ber, positioned on the sample tower of the 6-axis goniometer. The 17.91 keV monochromatic beam was focused by a set of beamline optics to $160 \times 20 \, \mu\text{m}^2$ on the sample and detected by a Medipix TAA22PC pixel detector mounted 178.59 mm away from the sample. Each exposure was recorded for 10 s using a 200 $\mu$m thick Mo attenuator. The incident angle $\theta$ was carefully chosen so that the specular beam resided between the primary beam and the first Bragg peak. A rectangular beamstop was mounted right in front of the detector to further attenuate the primary beam and specular beam. For chain-correlation characterization, the detector was moved 12 mm and 6 mm in the y and z directions off the central position to capture the chain-correlation peaks. No Mo attenuator was used due to the low intensity of the chain-correlation peaks.

5.1.2 PC-PE-PS-Chol 5:2:2:1

Fig. 5.1 shows the GISAXS patterns of PC-PE-PS-Chol 5:2:2:1 multibilayers recorded at ID01 at RH 90% and 50%. (left) Pure PC-PE-PS-Chol prepared by sOS, (center) pure PC-PE-PS-Chol prepared by sVS, and (right) PC-PE-PS-Chol/$\Delta$N+Syb prepared by sVS. Images were recorded at a number of hydration conditions. Fig. 5.1 shows the ones recorded at RH 90% and 50%. At RH 90%, all multibilayers exhibit typical diffraction patterns of oriented lamellar phases, with more Bragg orders observed from the sOS multibilayer than from the sVS multibilayers ($6 \text{ vs } 4$). First of all at higher hydration condition the multibilayers prepared by sVS also show high lamellar ordering, as indicated by the Bragg peaks. This property may yield high-resolution data for structural determination, phase identification, and eventually 2d or even 3d EDP reconstruction. Secondly, the sVS multibilayers show lower lamellar ordering compared with the sOS method at the same lipid composition. In the sOS preparation, lipid molecules move freely in organic solutions so that bilayers could find lower energy mesoscopic states more easily, hence higher lamellar ordering. Contrarily, in the sVS method lipid bilayers are deposited onto the wafers via vesicle adsorption and rupture. Inevitably, there can be a certain number of incomplete ruptures and more bilayer defects [179], hence lower lamellar ordering.

At RH 50%, the sOS multibilayer transformed to the rhombohedral ($R$) phase, which have been observed in many other sOS multibilayers [19, 25, 33]. Additionally, a new lamellar ($L$) phase appears perhaps due to the complex lipid composition. For sVS multibilayer however, the new $L$ phase is found to be in coexistence with an inverted hexagonal ($H_{II}$) phase, instead of the expected $R$ phase. It seems that under low hydration conditions, the sVS multibilayers
Figure 5.1: GISAXS patterns of multibilayers of (left) pure PC-PE-PS-Chol 5:2:2:1 prepared by sOS, (center) pure PC-PE-PS-Chol 5:2:2:1 prepared by sVS, and (right) PC-PE-PS-Chol 5:2:2:1 reconstituted with ΔN and Syb by sVS, measured at RH 90% and 50%. The dark blue bar is the shadow of the rectangular beamstop. All images were recorded with 10 s exposure time with the specular beam lying between the primary beam and 1st Bragg peak behind the beamstop. The intensity profiles along the $q_\parallel = 0$ direction are plotted in red. The $d$ values in the images represent the bilayer periodicities, and the white scale bar in the lower left corner indicates 50 pixels on the detector. The false color scale corresponds to the logarithmic scattering intensity.
of PC-PE-PS-Chol do not form stalk structures. It is of course not a desired result, which shall be further verified on other lipid compositions such as PC-PE (see the next section). Concerning the sVS multibilayers with/without SNAREs, no significant differences can be seen. This result is in good agreement with our observations from proteomicelles and proteoliposomes in the last chapter that SNAREs only slightly modified the host aggregates. Another interestingly outcome is that the bilayer periodicity \( d \) of sVS is always larger than \( d \) of sOS, whereas SNARE reconstitution slightly reduces it. However, these \( d \) values may contain high experimental errors due to large peak width in GISAXS studies. For more precise \( d \) results reflectivity investigation with sharp specular peaks shall be performed.

Alkyl chain correlation (CC) measurement is a powerful tool to reveal the lateral order of lipids within membranes \([18,64,139]\). Fig. 5.2 shows the CC results and the fitting of the three PC-PE-PS-Chol multibilayers. Fig. 5.2a displays the diffraction patterns of the same PC-PE-PS-Chol multibilayers as above but measured in the \( q \) regime of CC peaks. A strong CC peak appears in the diffraction pattern of sOS multibilayer of pure PC-PE-PS-Chol, showing a typical peak shape of multibilayers with high chain-ordering \([64,139]\). In contrast, the multibilayers of sVS with and without SNAREs both exhibit non-typical CC peaks, which are much weaker and almost angular independent compared to the peak of the sOS multibilayer. The intensity profiles at various angles \( \phi \) (as shown in Fig. 5.2a, left) are extracted from the diffraction maps. These profiles are then fitted in the same way as in Chap. 2 by

\[
f(q) = I_0 \frac{\omega^2}{(q - q_0)^2 + \omega^2} + mq + b, \tag{5.1}
\]

where \( \omega \) is the half width maximum, \( q_0 \) is the peak center, \( I_0 \) is the maximum of the Lorentzian which is normalized to 1 at \( \phi = 10^\circ \), \( m \) the slope of the linear background, and \( b \) the constant offset \([64,139]\). The average chain-chain distance \( a \) is then derived from \( a = \frac{9\pi}{4q_0} - \frac{3\omega}{2q_0} \) and the correlation length \( \xi \) of the acyl chains from \( \xi = \frac{1}{\omega} \). The intensity profiles between 10° and 50° are available in this experiment. Every 5° an intensity profile is extracted and fitted by Eq. 5.1. Fig. 5.2b shows the intensity profiles and fitting curves of the sOS multibilayer to offer an example of the fitting process.

Fig. 5.2c plots resulting fitting parameters \( I_0 \), \( a \) and \( \xi \) with respect to \( \phi \). Firstly the main chain-tilting angle can then be deduced from the maxima of \( I_0 \) \([64,139]\). The maxima of all \( I_0 \) do not appear in the fitted \( \phi \) range, meaning that all main chain-tilting angles are smaller than 10°. In other words the ma-
5.1 GISAXS characterizations of
SNARE-reconstituted multibilayers at ID01

Figure 5.2: (a) GISAXS patterns of pure PC-PE-PS-Chol 5:2:2:1 multibilayers plotted measured in the chain-correlation q regime. (Left) pure PC-PE-PS-Chol prepared by sOS, (center) pure PC-PE-PS-Chol prepared by sVS and (right) PC-PE-PS-Chol reconstituted with ΔN and Syb by sVS. The dashed lines denote \( I_0 \). In the left image, each colored line represents the intensity profile at each \( \phi \) angle. All images were recorded with 10 s exposure time. The false color scale corresponds to the logarithmic scattering intensity and the dark blue bar results from the beamstop.

(b) Experimental data (stars) and fits (solid lines) of the pure PC-PE-PS-Chol by sVS, shown as an example of the fitting process.

(c) Lateral ordering parameters of the multibilayers derived from the fitting. The maximum of the Lorentzian \( I_0 \) (log scale), chain-chain distance \( a \), correlation length \( \xi \) and their standard deviations are plotted as a function of \( \phi \).
majority of the lipids do not tilt strongly, indicating high membrane orientation for all three samples. However the sVS multibilayers have a more isotropic $l_0$ distribution, i.e. lower orientation, which decreases slightly further when $\Delta N$ and Syb are incorporated. These effects possibly result from incomplete vesicle rupture [179] and the coupling of $\Delta N$ and Syb. Secondly the average chain-chain distance $a$ varies only slightly at different $\phi$ for all multibilayers. $a$ of pure lipid multibilayers prepared by sOS and sVS are almost the same ($\sim 4.5 \text{ Å}$), while $a$ increases significantly in the presence of SNAREs ($\sim 5 \text{ Å}$). It seems that the incorporation of SNAREs increases the area per lipid of the host bilayers. Lastly, chain-chain correlation length $\xi$ of the sOS multibilayer is significantly higher than the sVS multibilayers, demonstrating that sVS method results in bilayers with lower lateral chain correlation. $\xi$ of the two sVS multibilayers are nearly the same, indicating that SNARE reconstruction does not affect the lateral chain correlation of sVS bilayers. Moreover $\xi$ decreases with $\phi$ for all samples, indicating that untilted lipids ($\phi < 10^\circ$) have stronger chain-chain correction than tilted ones ($\phi > 10^\circ$) [64].

5.1.3 PC-PE 4:1

Fig. 5.3 shows the GISAXS patterns of sVS PC-PE-PS-Chol 4:1 multibilayers recorded at ID01 at RH 95% and 50%. (left) Pure PC-PE (center) PC-PE reconstituted with SNAREs via the normal sVS routine, and (right) PC-PE reconstituted with premixed SNAREs (mixed before preparation). Images were taken at a number of hydration conditions including RH 95% and 50%, as shown in Fig. 5.3. In line with the PC-PE-PS-Chol multibilayers, at RH 95% both the sVS PC-PE multibilayers with/without SNAREs exhibit clean single lamellar phase. Moreover, 5 Bragg orders can be observed for both samples, also indicating that the sVS preparation results in multibilayers with high lamellar ordering comparable with the sOS preparation. The premixed SNAREs however give raise to less Bragg orders and two coexisting $L$ phases, evidencing clear phase separation. In this special preparation, we assume that the full SNARE complex has been formed from the beginning and then been reconstituted via the micelle-vesicle-multibilayer pathway. Hence, the four-helix bundle is likely to anchor into the same bilayer via the two TMDs. Since this presumably extends the inter-bilayer distance to an unfavorable value, the system seems to react by phase separation. Such “kinetically or thermodynamically improbable conformation” [162] is one of the central concerns in the reconstitution of surface-associated proteins.
5.1 GISAXS characterizations of SNARE-reconstituted multibilayers at ID01

Figure 5.3: GISAXS patterns of sVS multibilayers of (left) pure PC-PE 4:1, (center) PC-PE 4:1 reconstituted with SNAREs via the normal sVS routine, and (right) PC-PE 4:1 reconstituted with premixed SNAREs (mixed before preparation), measured at RH 95% and 50%. The dark blue bar is the shadow of the rectangular beamstop. All images were recorded with 10 s exposure time with the specular beam lying between the primary beam and 1st Bragg peak behind the beamstop. The intensity profiles along the \( q_{\parallel} = 0 \) direction are plotted in red. The \( d \) values in the images denote the bilayer periodicities, and the white scale bar in the lowerleft corner indicates 50 pixels on the detector. The false color scale corresponds to the logarithmic scattering intensity.
At RH 50%, all measured PC-PE multibilayers show a phase coexistence of an $H_{II}$ and an $L$ phase. The same as PC-PE-PS-Chol multibilayers prepared by sVS, $H_{II}$ phases appear instead of the expected $R$ phase (i.e. stalk structures). Based on such observation on the two different lipid compositions at various hydration conditions, we now can conclude that the current sVS preparation yields multibilayers with different phase behaviors despite the same lipid composition. We assume that it mainly results from the unremoved n-OG, in agreement with the SAXS results of proteoliposomes in Section 4.4.5. It has been reported that n-OG is able to suppress the formation of non-lamellar phases [209]. However it is yet not clear whether n-OG alters multibilayers in the same way as in the literature. Due to the limitation in time of synchrotron measurements, we are unable to evaluate their phase behaviors in great detail.

5.2 In-house x-ray reflectivity studies of SNARE-reconstituted multibilayers

At ID01 we have already preliminarily investigated the sVS multibilayers of PC-PE-PS-Chol and PC-PE at several hydration conditions. Many aspects remain unclear due to the limited amount of time at synchrotron. Back home we systematically studied the PC-PE 4:1 sample family with more control samples and more hydration conditions, by making use of the in-house instrumentation. Pure PC-PE multilayer prepared by sOS, pure PC-PE multilayer, PC-PE/ΔN multilayer and PC-PE/ΔN+Syb multilayer prepared by sVS were investigate by both x-ray reflectivity and GISAXS.

5.2.1 Instrumentation

X-ray reflectivity experiments in this section were performed with the same home-built laboratory diffractometer Wendi as in Chap. 1 and 2. Briefly, the samples were mounted in the software-controlled humidity chamber, positioned in a $\theta/2\theta$ two-circle goniometer. A $1 \times 6 \text{ mm}^2$ Cu $K_\alpha$ beam ($\lambda = 1.54 \text{ nm}$, $E = 8.048 \text{ keV}$) hit the multilayer at an incident angle $\theta$. The intensity of the exit beam at exit angle $2\theta$ was measured by a fast scintillation counter (Cyberstar, Oxford-Danfysik). Reflectivity curves at various hydration conditions were obtained by scanning $\theta$ from 0 to $10^\circ$ for 2 s at each angle under controlled RH.
5.2 In-house x-ray reflectivity studies of SNARE-reconstituted multibilayers

5.2.2 The effect of TR on PC-PE multibilayers

Before starting the systematic investigation of PC-PE multibilayers, a comparative assay was carried out to inspect the effect of Texas Red on multilayer orientation. Texas Red (TR) is grafted onto dihexadecanoyl phosphoethanolamine (DHPE) and serves as a lipid dye in the sVS protocol to provide a better visual management of the elution process. However, it is worth noting that TR-DHPE may change the phase behavior of the host membranes [218]. To this end, we prepared two PC-PE multibilayers by sVS, one containing 0.67 wt% TR-DHPE and the other TR-DHPE free, which were both characterized by x-ray reflectivity at various hydration conditions.

![X-ray reflectivity curves of PC-PE 4:1 multibilayers with/without TR-DHPE prepared by sVS measured at RH 90% (left) and 50% (right). Scans were recorded at θ intervals of 0.01° and 2 s per step. The TR-free curves are shifted for clarity.](image)

Fig. 5.4 shows reflectivity curves of both multibilayers at two hydration conditions, RH 90% for the lamellar phase and 50% for non-lamellar phases. At RH 90%, both curves exhibit single phase, with the Bragg peaks shifting to higher $q$ in the presence of 0.67 wt% TR. On the one hand at higher hydration conditions, TR-DHPE does not affect the lamellar ordering at RH 90% so that the same number of Bragg orders appear. It seems that the TR groups or TR-DHPE as a whole can properly adapt themselves to the lamellar lattice, leading to undistorted bilayers. Furthermore, the bilayers become slightly thinner due to TR-DHPE. It has been reported by computational study that the hydrophobic TR groups tend to reside in the chain region [219], and thus increases the average area per lipid and reduces bilayer thickness. At RH 50%, significant difference between the two curves appear. In the presence of TR-DHPE, less Bragg orders can be observed and the Bragg peaks become broader. This result implies that under lower hydration conditions, TR drastically reduces the lamellar ordering...
and the mosaic spread of the multibilayer [220]. The giant TR groups seem to be unable to properly adopt themselves to non-lamellar lattice in the way they have done in the lamellar phase above. Knowing that even small amount of TR might largely change the bilayer properties in our system, we hence completely abandoned the use of TR in the following sVS preparations, at the cost of more difficult elution management.

5.2.3 Systematic x-ray reflectivity studies of PC-PE 4:1 multibilayers

Rocking scan

Prior to the reflectivity scans, rocking scans were performed in the positions of the 1st Bragg peaks to achieve proper experimental alignments and to determine membrane mosaicity. The detector angle was fixed in the first Bragg position $2\theta$ with $2\theta \equiv \alpha_i + \alpha_f$, where $\alpha_i$ and $\alpha_f$ denote the incident angle and exit angle. Rocking curves were obtained by scanning $\alpha_i$ around the equilibrium position $\theta$ at intervals of 0.002° with 2 s scanning time. Before fitting, all $I_{max}$ are normalized to 1. Each rocking curve is then fitted by a single Gaussian:

$$I(\omega) = e^{-\frac{4 \ln 2 \omega^2}{W^2}}, \quad (5.2)$$

where $\omega = \alpha_i - \theta$ and $W$ denotes the peak width (full width at half maximum, FWHM).

Fig. 5.5 shows both the rocking scans and the fits of different PC-PE 4:1 multibilayers at RH 90%, including pure PC-PE 4:1 multibilayer prepared by sOS, pure PC-PE 4:1, PC-PE 4:1/ΔN and PC-PE 4:1/ΔN+Syb multibilayers prepared by sVS. The peak width $W$ obtained from fitting is listed in the legend: The $W$ of the sOS multibilayer (0.043°) is smaller than all others, the $W$ of sVS multibilayers of pure PC-PE 4:1 (0.050°) and PC-PE 4:1/ΔN (0.049°) are slightly larger, and the $W$ of the sVS multibilayer of PC-PE 4:1/ΔN+Syb (0.070°) is the largest among all samples. These results suggest that (i) the sVS method leads to a lower membrane orientation compared with the sOS method, (ii) reconstruction of ΔN alone does not reduces membrane orientation and (iii) reconstruction of both ΔN and Syb significantly reduces the orientation. Despite the decrease of membrane orientation, all $W$ here are comparable to literature values [15, 221]. Hence the sVS preparation yields sufficiently oriented multibilayers, even in the presence of both ΔN and Syb. All these findings are well in line with the GISAXS results above.
5.2 In-house x-ray reflectivity studies of SNARE-reconstituted multibilayers

Raw reflectivity curves

Fig. 5.6 shows the reflectivity curves of PC-PE 4:1 multibilayers at various hydration conditions (RH 90-50% at 2 % intervals). (i) Pure PC-PE multibilayer prepared by sOS (black) results in typical relativity curves of sVS multibilayers in response to the RH: a series of sharp Bragg peaks appear at all measured RHs and shift to the high $q$ region at lower RHs. (ii) PC-PE multibilayer prepared by sVS also give rise to a number of strong Bragg peaks, but less Bragg orders are visible especially at higher RHs. Such a decrease in Bragg orders has already been observed with GISAXS at ID01 beamline (Section 5.1.3), indicating a lower lamellar ordering and more static defects of the sVS method compared with the sOS method. Moreover, a new series of Bragg peaks show up at lower RHs (RH 60-70%, highlighted by the green arrows in Fig. 5.6), indicating a phase separation due to preparation method. On the positive side however, 5-8 Bragg orders is already a sign of high lamellar ordering. With them we can carry out EDP reconstitution by means of Fourier synthesis [222] (results shown in Fig. 5.7).
Figure 5.6: X-ray reflectivity curves of PC-PE 4:1 multibilayers measured at RHs 90-50% at 2% intervals. From top to bottom: (i) Pure PC-PE 4:1 multibilayer prepared by sOS, (ii) pure PC-PE 4:1 multibilayer prepared by sVS, (iii) PC-PE 4:1/ΔN multibilayer prepared by sVS and (iv) PC-PE 4:1/ΔN+Syb multibilayer prepared by sVS. Curves of lower RHs are shifted for clarity. The green arrows point to the new series of Bragg peaks.
Next we compare the reflectivity curves of the different samples prepared by the sVS method. The curves of sVS multibilayer with $\Delta N$ (red) are similar to the ones of the pure lipid sVS multibilayer, except that the secondary phase does not appear. Hence single SNARE, $\Delta N$ in this case does not largely modify the host structures either. The reflectivity curves of the multibilayer with mixed $\Delta N$ and Syb (purple) on the other hand shows a completely different lineshape with the other two sVS multibilayers, with Bragg peaks becoming weaker and less sharp, and shifting to smaller $q_z$. We have learned from the SAXS results that the incubation of $\Delta N$ and Syb vesicles does not alter the vesicle structure and size distribution. Thus such profound structural modification could only have taken place on the substrates where strong evacuation was applied to form a dry multibilayer. This way, bilayers were forced into close contact [162] and hence the fusion events were initiated. In the presence of both $\Delta N$ and Syb, the bilayer could dock, hemifuse or fuse, yielding a large variety of vesicle geometries and sizes [172]. As a result, PC-PE/$\Delta N+$Syb multibilayer exhibit lower lamellar ordering compared to the other sVS multibilayers.

**EDP reconstruction**

![EDP reconstruction graph](image)

Figure 5.7: EDPs of the PC-PE 4:1 multibilayers at RH 90% reconstructed from the reflectivity curves in Fig. 5.6. The phase combination of $-1, -1, +1, -1, +1$ is used. The electron densities are in arbitrary units and are normalized by the electron density of the methyl dip.
As we can see in the reflectivity curves, although the sVS preparation and SNARE coupling reduces the lamellar ordering, there are still enough Bragg orders for EDP reconstitution analysis, at least at higher hydration conditions. Here the swelling method as introduced in Chap. 1 can not be performed due to the lack of experimental conditions. Instead, the phase combination $-1, -1, +1, -1, +1$ is directly used based on previous results [25,65], yielding reasonable EDPs at higher hydration conditions (e.g. RH 90%) by means of Fourier synthesis. However, it is rather difficult to perform the same reconstruction at lower RHs especially for the multibilayer with both $\Delta N$ and Syb due to the lack of Bragg orders and unclear separation between peaks.

Fig. 5.7 shows the EDPs of all 4 multibilayers at RH 90%. Assuming that the electron density of the methyl group at the end of the acyl chain stays constant, EDPs of different multibilayers are normalized by the intensities of the methyl dip. On the one hand, the EDP of the pure PC-PE multibilayer by sOS shows the typical bilayer EDP distribution of single lamellar multibilayers [223]: the headgroup separates clearly with the water region and the carbon chains. On the other hand, for the EDPs of the sVS multibilayers (blue, red and purple) the contrast between different lipid segments are no longer significant. This could be explained by the fact that there are more defects in the sVS multibilayers, resulting in lower lateral order (as shown by the chain-correlation results) and less distinguishable segment separation. The highly overlapping EDPs of PC-PE and PC-PE/$\Delta N$ sVS multibilayers demonstrate that the reconstruction of single SNARE barely changes the membrane structure. However, the EDP becomes much wider when the two SNARE are mixed indicating higher level of swelling. It could possibly originate from the coupling effect between $\Delta N$ and Syb. In this case the fully assembled SNARE complex with the 4-helix bundle has to be accommodated into the multilamellar structure, leading to significant structural change in the host membrane. Nonetheless, at this point we cannot come to any 3d structures to properly address our observation. Interestingly, the EDPs of the sVS multibilayers overlap with each other in the acyl region. It seems that in multibilayers of PC-PE 4:1 their TMDs can match the lipid carbon chains well without drastic structural distortion.

**Bilayer periodicity $d$**

Due to the lack of Bragg orders and poor peak sharpness, we are unable to perform EDP reconstitution for all RHs. The bilayer periodicity $d$ offers an estimation of the bilayer structures assuming that $d_{hh}$ is proportional to $d$. Fig. 5.8 plots the bilayer periodicities $d$ of PC-PE multibilayers with respect to RH. We
5.2 In-house x-ray reflectivity studies of SNARE-reconstituted multibilayers

Figure 5.8: Plots of bilayer periodicity $d$ of the PC-PE 4:1 multibilayers as a function of the RH, derived from the x-ray reflectivity curves in Fig. 5.6. Only the orders between the first and the last orders are used in the calculation. The standard deviations are smaller than the size of the markers and thus not plotted. Each circle marker represents a performed measurement. The two vertical pink lines denote possible phase transition at the RH*.

can find that (i) the $d$ of pure PC-PE prepared by sVS is larger than pure PC-PE prepared by sOS, (ii) the $d$ plots of pure PC-PE and PC-PE/$\Delta N$ almost overlap, and (iii) $d$ increases significantly in the presence of both $\Delta N$ and Syb. These results are in line with the observations in the EDP section that sVS preparation swells the bilayers, $\Delta N$ reconstitution causes no observable structural modification and $\Delta N$ and Syb coupling swells the bilayers even further. Secondly, we could deduce the phase transition from the changes in curve slopes [21], but only as an indirect evidence. As expected, the pure PC-PE multibilayer prepared by sOS transform into a non-lamellar phase at RH 68% as indicated by the sudden slope change of its $d$ plot (black). In contrast, neither the reflection curve of pure PC-PE multibilayer prepared by sVS (blue) nor the reflection curve of PC-PE multibilayer containing $\Delta N$ (red) shows such a transition. Interestingly, when both $\Delta N$ and Syb are present (purple), a possible phase transition occurs at RH 58%. Notwithstanding we can not confidently determine phase transitions merely from $d$, unless more convincing proofs are found. In order to provide further support to the findings in this section, careful in-house GISAXS experiments were then performed on the same multibilayers and at the same RHs.
5.3 In-house GISAXS investigations of SNARE-reconstituted multibilayers

5.3.1 Instrumentation

The in-house GISAXS experiment was performed on the self-built laboratory diffractometer Rosi, which is sketched in Fig. 5.9. The Cu Kα (λ = 1.54 nm, E = 8.048 keV) beam was produced by a rotating anode generator (MicroMax-007 HF, Rigaku) operating at U = 40 kV and I = 30 mA. The effective size of the focal spot was a 0.07 mm circle at 6° take-off angle, yielding a total flux of 6.13 × 10^8 cps. A pair of Kirkpatrick-Baez mirrors (Confocal Max-Flux Optics, Osmic) was used to collimate and monochromatize the divergent beam. Afterwards the beam was attenuated by combining 4 Cu foils with different thickness (see Appendix D.1), and then defined to 1 × 1 mm^2 size by the entrance slits. A monitor (Simens) and a fast shutter were mounted between the slits and the sample to inspect the intensity before the sample and to protect the detector. The samples were placed in the same vapor chamber as used for Wendi, which was mounted on a 6-axis goniometer stage (Huber). The beam entered the multibilayer at an incidence angle θ ≈ 0.6° and the exit beam was captured by a Pilatus 100K pixel detector (DECTRIS) with 487 × 195 pixels and 172 × 172 µm^2 pixel size, mounted 20 cm behind the sample. A square Si (2.34 × 2.34 × 1.00 mm^3) beamstop was glued onto the Kapton window direct in front of the detector to attenuate the bright primary beam. Each image was recorded with 1000 s exposure time.
5.3 In-house GISAXS investigations of 
SNARE-reconstituted multibilayers

5.3.2 Systematic GISAXS characterizations of PC-PE 4:1 at various RHs

Fig. 5.10 shows the in-house GISAXS patterns of PC-PE 4:1 multibilayers measured at various hydration conditions (RH 88-50% at 2% intervals). (Row 1) pure PC-PE prepared by sOS, (Row 2) pure PC-PE prepared by sVS, (Row 3) PC-PE with ∆N prepared by sVS, and (Row 4) PC-PE with both ∆N and Syb prepared by sVS. The first row shows the familiar phase transition from the L phase to the rhombohedral (R) phase [21, 25]. The hallmark of the R phase is the two off-axis peaks on each side of the in-plane peaks, which are most clearly visible in the GISAXS pattern at RH 50%. For PC-PE 4:1, the phase transition happens around 60%, comparable to 68% that Fig. 5.6 has predicted. With this information at hand, we turn to the sVS samples. In the ideal case, the measured phase diagram should be an intrinsic property of the lipid mixture, not of the preparation. However, this turns out not to be the case. In contrast to the sOS sample, where single phase behavior is always observed, we obtain a pronounced phase-coexistence regime at lower RHs from sVS multibilayers. Furthermore, neither of the two phases transform into the R phase when the RH further decreases, even in the presence of both ∆N and Syb. The first L phase persists while the second L phase transforms into the H_{II}. One may speculate whether the difference in the phase diagram, in particular the appearance of the H_{II} phase instead of the R phase, can be attributed to the higher defect level in the sVS preparation. While the influence of defects on the phase diagram in soft condensed matter [224] is not completely implausible, we rather believe that this unexpected and complex phase behavior originates from remaining detergent (mainly n-OG) introduced by the preparation. Comparison of pure vesicles prepared by sonication and size-exclusion above have already proved the existence of abundant n-OG in vesicles prepared by the new protocol. In the multibilayers it further inhibits the transitions to non-lamellar phase [209], and also gives rise to a new phase which could transform from L to H_{II} phase at lower RHs [225]. Moreover, the structure of the new phase appears to be rather irregular if we compare the three sVS samples, perhaps due to the random concentration of remaining n-OG.

5.3.3 The effect of extra purification on PC-PE 1:1

In the last few sections, it was found that large amount of n-OG remains after two runs of G-25 column dilution and affects the phase behaviors of resulting
Figure 5.10: In-house GISAXS patterns of PC-PE 4:1 multibilayers recorded at various hydration conditions (RH 88-50% at 2% intervals). From left to right: (Row 1) Pure PC-PE multibilayer prepared by sOS, (Row 2) pure PC-PE multibilayer prepared by sVS, (Row 3) PC-PE/ΔN multibilayer prepared by sVS and (Row 4) PC-PE/ΔN+Syb multibilayer prepared by sVS. Each exposure was recorded for 1000 s. The dark shadow in the center of all images results from the beamstop which attenuates the primary beam. In the upper right corner, the false color scale corresponds to the logarithmic scattering intensity and the white scale bar denotes 20 pixels on the detector.
Figure 5.11: In-house GISAXS patterns of PC-PE 1:1 multibilayers prepared by sVS recorded at various hydration conditions (RH 90-60% at 2% intervals).
(a): (Left) normal purification routine, i.e. 2 times through the columns and (right) extra purification routine, i.e. 4 times through the columns. The dark shadow in the center of each exposure results from the beamstop which attenuates the primary beam.
(b): Zoom of the two diffraction patterns at RH 60%. For both samples, the primary beam (PB) and specular beam (SB) are denoted in white, the lamellar indices in black and hexagonal indices in red, with vertical dash lines connect common phases. The pink dash circle/arc in the upper image denotes the additional phase which does not appear in the lower one. The false color scale corresponds to the logarithmic scattering intensity and the white scale bar denotes 20 pixels on the detector.
multibilayers. Many approaches can be taken to fully remove n-OG, including extra column runs, dialysis and hydrophobic adsorption [226]. Here we preliminarily attempt to apply 2 extra column runs to the proteoliposome suspensions. The multibilayers via normal purification routine (2 column runs) and extra purification routine (4 column runs) were investigated with in-house GISAXS.

Fig. 5.11 shows the GISAXS patterns of PC-PE 1:1 multibilayers prepared via 2 and 4 column runs. Fig. 5.11a presents the two sets of exposures at various hydration conditions (RH 90-60% at 2% intervals). An extremely complicated phase behavior is observed on the first set for which only 2 column runs were performed. Generally up to 3 phases appear at all RHs. In contrast, the second set exhibits a much cleaner phase behavior with only 2 phases coexisting in the diffraction patterns. The extra purification runs seem to work by delivering cleaner diffraction patterns containing less phases. We then take a look at the diffraction patterns at RH 60% more carefully (Fig.5.11b). The common phase in both samples is indexed as one L phase (black) and one HII phase (red). The additional phase of the sample with standard purification is possibly 12-fold symmetric quasi-crystal [227, 228] or a gyroid cubic phase [229], which can not be undoubtedly indexed due to week peak intensity. Either way, such a phase is rather uncommon for pure lipid systems in this hydration condition range. It is therefore assumed to be a result of n-OG partitioning into the lipid bilayers. This difference clearly demonstrates that the standard purification procedure does not sufficiently remove the detergents for meaningful phase diagram studies. To this end the purification procedures of the sVS preparation has to be improved, maybe at the expense of yield and efficiency. This preliminarily attempt with extra column runs only offers a possible approach of further purification, but is not necessarily more efficient compared with dialysis and hydrophobic adsorption.

5.4 Summary and outlook

In this chapter the effects of sVS preparation as well as SNARE reconstitution on multibilayer structures are evaluated by x-ray reflectivity and GISAXS. Results show: (i) the sVS preparation results in thicker bilayers compared to sOS, probably due to n-OG and incomplete vesicle rupture. (ii) ΔN alone does not dramatically alter the bilayer structures. (iii) the coupling of ΔN and Syb can bring about drastic membrane misorientation and swelling but no stalk structures, possibly due to the remaining n-OG in the multibilayers and (iv) extra
purification is able to reduce n-OG remaining, hence simpler phase behavior. In the future further efforts shall be made to thoroughly remove the remaining n-OG with more effective detergent removal techniques, in order to observe SNARE-mediated stalk formation in the multibilayer system, and eventually re-construct 3d stalk structures in the presence of SNAREs.
6 Conclusion and outlook

The aim of this thesis is to extend previously established x-ray studies of stalk formation in pure lipid multibilayers to more complex systems closer to actual physiological conditions of fusion events in 

\textit{vivo}. To this end, efforts on three levels have been devoted, namely the lipid level, the peptide level and the protein level.

On the lipid level, we found a “magic lipid mixture” for which the minimal osmotic pressure is required to promote fusion, i.e. the highest RH\textasciicircum*\textasciicircum, so that pure lipid stalk formation can take place in the aqueous environment where merely mild osmotic pressure can be induced by solutes like PEG. After a series of attempts with binary, ternary and quaternary lipid mixtures, we found that the PC-PE-Chol 45:45:10 mixture forms a single stalk (R) phase at RH \leq 87\%, which is already achievable by PEG aqueous solutions. First GISAXS results showed that indeed this mixture can form stalks in PEG-400 aqueous solutions which offer equivalent osmotic pressure (PEG mass fraction \geq 65\%), but in the presence of a unexpected $H_{II}$ phase which might disturb the structural characterizations in more complex lipid systems. Consequently, prior to the introduction of physiological conditions like pH level and ion strength, progress has to be made to eliminate the additional $H_{II}$ phase.

On the peptide level, we investigated two families of transmembrane $\beta$-peptides, one with one without additional tryptophan anchors, aiming at structurally stable and tailorable $\beta$-helical TMDs. By introducing I-labels into either the tail region or the center region of the peptides, we were able to determine the relative positions of these moieties with respect to the lipid bilayers. CD spectra and x-ray scattering results demonstrate that $\beta$-peptides with desired helical structures are successfully integrated into DOPC bilayers in a transmembrane fashion. Moreover, $\beta$-peptides adopt a slightly tilted conformation to compensate for the peptide-lipid hydrophobic mismatch, which can be diminished by additional tryptophan anchors. Based on this approach, in the future we could design and synthesize complete SNARE analogs containing $\beta$-helical TMDs, in association with various fusion recognition motifs and linkers [230].

On the protein level, a novel vesicle-based protein-compatible preparation protocol for supported multibilayers has been developed, so that stalk formation can be studied in the presence of SNAREs in the multibilayer system. This new protocol consists of three stages as shown in Fig. 3.6: (i) SNAREs
are co-micellized together with n-OG and lipids, yielding n-OG/lipid/SNARE proteomicelles; (ii) n-OG is then removed by size-exclusion, resulting in lipid/SNARE proteoliposomes; (iii) SNARE-reconstituted multibilayers are obtained by spreading vesicle suspensions (the sVS method) onto the substracts. Both the proteomicelles and proteoliposomes have been characterized by SAXS with the data being fitted by parameterized models. Results show that SNAREs are successfully incorporated into micelles and vesicles via co-micellization and size-exclusion, and that SNARE reconstitution induces a minor bilayer thickening effect. Mixing the two proteoliposome suspensions yields multibilayers containing both SNAREs (ΔN as the t-SNARE and Syb as the V-SNARE). Subsequent x-ray reflectivity and GISAXS characterizations reveal that the coupling effect of the two SNAREs under partial dehydration significantly thickens the bilayers and reduces their lamellar ordering, and that an $H_{II}$ phase instead of an anticipated $R$ phase is observed probably due to incomplete removal of n-OG. At present we have successfully reconstituted SNAREs into supported multibilayers via the novel sVS protocol, but failed to observe stalk structures in sVS multibilayers containing SNAREs. To this end in the future we shall seek more effective purification procedures and preparation conditions to fabricate multibilayers with higher orientation and less impurity, and eventually achieve our long term goal: 3d EDP reconstruction of stalk structures in the presence of SNAREs.
## Appendix

### A.1 Major x-ray reflectivity measurements in Chap. 1

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## A.2 Filter parameters of the in-house reflectometer

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*Made of aluminum.*

*Taken from http://henke.lbl.gov/optical_constants/filter2.html.*
A.3 Reflectivity curves of PC-PE-DOG 45:45:10

Figure A.1: Reflectivity curves of PC-PE-DOG 45:45:10 at RH 94-70%. Data plotted in logarithmic scale and scaled for clarity. Inset: Zoom of the 2\textsuperscript{nd} Bragg peak at RH 90%.
A.4 Reflectivity curves of PC-PE-Chol 40:40:20

Figure A.2: Reflectivity curves of PC-PE-Chol 40:40:20 at RH 90-80%. Data plotted in logarithmic scale and scaled for clarity. Inset: Zoom of the 2nd Bragg peak at RH 86%.
A.5 Reflectivity curves of PC-PE-PIP$_2$ 35:35:30

Figure A.3: Reflectivity curves of PC-PE-PIP$_2$ 35:35:30 at RH 90-78%. Data plotted in logarithmic scale and scaled for clarity. Inset: Zoom of the 3$^{rd}$ Bragg peak at RH 87%.
**B.1 Preparation and fitting conditions of vesicles investigated in this work**

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<td>ΔN/Syb</td>
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</tr>
</tbody>
</table>

<sup>a</sup> Protein/lipid ratio 1:500
function I = I_micelle(P, scan_suspension, range)
q = scan_suspension(range,1) * 0.1; % scattering vector in Angstrom

% read all fitting parameters
a = P(1); % minor semi-axis length in Angstrom
b = P(2); % major semi-axis length in Angstrom
rho1 = P(3); % inner rho (carbon chain) in e/A^3
rho2 = P(4); % outer rho (headgroup) in e/A^3
ta = P(5); % bilayer thickness in a direction in Angstrom
tb = P(6); % bilayer thickness in b direction in Angstrom
s = P(7); % scaling factor
f = P(8); % offset

V1 = 4*pi*a*b^2/3; % core volume
Vt = 4*pi*(a+ta)*(b+tb)^2/3; % total volume

% replace qR with u
% replace cos(th) with x
u1 = @(x)q*sqrt(a^2*x.^2 + b^2*(1-x.^2));
u2 = @(x)q*sqrt((a+ta)^2*x.^2+(b+tb)^2*(1-x.^2));

% I as a function of x
% adapted bessel function: besselj(n+1/2,x)*sqrt(pi/(2*x))
I_x = @(x) ((3*V1*(rho1-rho2) * besselj(1+1/2,u1(x)).*sqrt(pi./(2*u1(x))))./u1(x))...
     + 3*Vt*(rho2-0.334)* besselj(1+1/2,u2(x)).*sqrt(pi./(2*u2(x))))./u2(x).^2;

% integrate x from 0 to 1
I = integral(I_x,0,1,'ArrayValued',true);
% add s and f to match the calculated I with the experimental I
I = I*s + f;
end
% symetric planar bilayer model
% model taken from P. Szekely et al., Langmuir, 2010
% by Karlo Komorowski and Yihui Xu, Feb 2016

function I = I_Vesicle_Sym(P, Scan_vesicle, ran)

q = Scan_vesicle(ran,1); % q-range (nm)

% Setup parameters for the symetric planar bilayer model
% Peak position z / Angstrom
z(1) = P(1); % headgroup 1 in Angstrom
z(2) = 0; % chain region in Angstrom
z(3) = -P(1); % headgroup 2 in Angstrom

% Amplitude of rho
r(1) = P(2); % headgroup 1 in a.u.
r(2) = -1; % chain region in a.u.
r(3) = P(2); % headgroup 2 in a.u.

% FWHM tau of the Gassian shells, sigma = tau/2.35
r(1) = P(3); % headgroup 1 in Angstrom
r(2) = P(4); % chain region in Angstrom
r(3) = P(3); % headgroup 2 in Angstrom

% Scaling factor and offset
s = P(5);
f = P(6);

% Form factor (FF) calculation
I = zeros(1,length(q))';
for i=1:3
    for j=1:3
        I = I + ...
            (2*pi^3./((q.^2)*log(2))^2...)
            r(i)*r(j)*t(i)*t(j).*...
            exp(-(q.^2.*(t(i).^2 + t(j).^2))/(16.*log(2))).*...
            cos(q.*(z(i)-z(j)))
    end
end

% add s and f to match the calculated I with the experimental I
I = I*s + f;
end
C.1 Estimation of $N_{SNARE}$ per Micelle

To better interpret the presence or absence of changes in the SAXS measurements with SNARE reconstitution, it is essential to first estimate the average SNARE number per micelle, since the SAXS measurements correspond to an ensemble average (see the discussion in the main text). Below we present the parameters used in the corresponding calculation, i.e. SAXS results in Tab. 1a for the micelle geometry, literature values for lipid and surfactants and the stoichiometry parameters of our preparation. We conclude that only 9% of all micelles have a reconstituted SNARE protein.

List of constants

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Value</th>
<th>Units</th>
</tr>
</thead>
<tbody>
<tr>
<td>$V_{nOG}$ [Å$^3$]</td>
<td>243</td>
<td></td>
</tr>
<tr>
<td>$V_{lipid}$ [Å$^3$]</td>
<td>1620</td>
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</tr>
<tr>
<td>$M_{nOG}$ [g/mol]</td>
<td>282</td>
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</tr>
<tr>
<td>$M_{lipid}$ [g/mol]</td>
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<tr>
<td>CMC [mg/ml]</td>
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</tr>
<tr>
<td>$m_{nOG}$ [g]</td>
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<td>$m_{lipid}$ [g]</td>
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<tr>
<td>$V_{solution}$ [µl]</td>
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<tr>
<td>a [Å]</td>
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</tr>
<tr>
<td>b [Å]</td>
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</tr>
<tr>
<td>$t_a$ [Å]</td>
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<td></td>
</tr>
<tr>
<td>$t_b$ [Å]</td>
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</tr>
<tr>
<td>$R_{protein/lipid}$</td>
<td>1:500</td>
<td></td>
</tr>
</tbody>
</table>

Calculation

$$V_{micelle} = \frac{4}{3} \pi (a + t_a)(b + t_b)^2 \approx 119209 \quad \text{(C.1)}$$

$$R_{lipid/nOG} = \frac{m_{lipid}/M_{lipid}}{(m_{nOG} - V_{solution} \cdot CMC)/M_{nOG}} \approx 0.27 \quad \text{(C.2)}$$

$$N_{nOG} = \frac{V_{micelle}}{V_{nOG} + V_{lipid}R_{lipid/nOG}} \approx 175 \quad \text{(C.3)}$$

$$N_{SNARE} = N_{nOG}R_{lipid/nOG}R_{protein/lipid} \approx 0.09 \quad \text{(C.4)}$$

---

1 Almog et al. (1990) and Wenk et al. (1997).
2 Parameters of DOPC rather than the lipid mixtures are used.
C.2 Estimation of $N_{\text{SNARE}}$ per Vesicle

Similar to the estimation in Appendix A, we have performed a calculation of the copy number $N_{\text{SNARE}}$ per vesicle. Below we present the calculation using parameters obtained from literature\(^3\), SAXS results in Tab. 1b and DLS results in Appendix B.

**List of constants\(^4\)**

<table>
<thead>
<tr>
<th>Constant</th>
<th>Value</th>
<th>Description</th>
</tr>
</thead>
<tbody>
<tr>
<td>$V_{\text{lipid}} ,[\text{Å}^3]$</td>
<td>1620</td>
<td>volume per lipid molecule</td>
</tr>
<tr>
<td>$R_0 ,[\text{Å}]$</td>
<td>300</td>
<td>mean vesicle radius from DLS</td>
</tr>
<tr>
<td>$D_b ,[\text{Å}]$</td>
<td>36.76</td>
<td>bilayer thickness from SAXS fitting</td>
</tr>
<tr>
<td>$R_{\text{protein/lipid}}$</td>
<td>1:500</td>
<td>protein/lipid molar ratio</td>
</tr>
</tbody>
</table>

**Calculation**

\[
V_{\text{out}} = \frac{4}{3} \pi R_0^3 \approx 1.13 \times 10^8 \text{ Å}^3 \tag{C.5}
\]

\[
V_{\text{in}} = \frac{4}{3} \pi (R_0 - D_b)^3 \approx 7.64 \times 10^7 \text{ Å}^3 \tag{C.6}
\]

\[
N_{\text{SNARE}} = \frac{V_{\text{out}} - V_{\text{in}}}{V_{\text{lipid}}} R_{\text{protein/lipid}} \approx 43.61 \tag{C.7}
\]

\(^3\) Almog et al. (1990).

\(^4\) Parameters of DOPC rather than the lipid mixtures are used.
### D.1 Attenuator parameters of the in-house diffractometer Rosi

#### Index

<table>
<thead>
<tr>
<th>Index</th>
<th>Attenuator status$^a$</th>
<th>Thickness [µm]</th>
<th>Transmission (theoretical)$^b$</th>
<th>Transmission (experimental)</th>
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<td>0</td>
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<td>1.00</td>
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</table>

$^a$ 16 different transmission rates are achieved by combining 4 Cu foils with the thicknesses of 24, 48, 96 and 192 µm. 0 denotes the foil is out of position whereas 1 denotes the foil is in position.

$^b$ Taken from http://henke.lbl.gov/optical_constants/filter2.html.
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Own publications


\(^1\) These authors contributed equally
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Curriculum vitae

Personal information

Name: Yihui Xu
Date of birth: 18. Oct. 1987
Place of birth: Yancheng, China
Citizenship: Chinese

Education

10/2012-present: PhD student and scientific employee in the Group of Tim Salditt, Institute for X-ray Physics, Universität Göttingen, Göttingen, Germany; Member of the “International Max Planck Research School for Physics of Biological and Complex Systems” (IMPRS-PBCS) under “Göttingen Graduate School for Neuroscience, Biophysics and Molecular Biosciences” (GGNB); Funded by German Science Foundation DFG (SFB 803)

09/2009-06/2012: Master student in the Group of Tao Zhang, Department of Materials Science & Engineering, Nanjing University, Nanjing, China

09/2005-06/2009: Bachelor student, Department of Materials Science & Engineering, Nanjing University, Nanjing, China

09/2002-06/2005: Yancheng Middle School, Yancheng, China
Previously, our group successfully characterized the effect of various lipids on the stalk formation in pure lipid multilayers by means of x-ray scattering. In this model system, the energy required for stalk formation was supplied by the osmotic pressure of the aqueous vapor. Despite its remarkable simplicity and efficiency, the sample environment of this method was distinct from the fusion sites in vivo. This work aims to extend the x-ray study of stalk formation to more physiological conditions. To this end, efforts on three levels have been devoted, namely the lipid level, the peptide level and the protein level. On the lipid level, PEG solutions rather than aqueous vapor were used as the stressor to promote stalk formation in pure lipid bilayers. On the peptide level, D-β-peptides were incorporated into model lipid multilayers to investigate its transmembrane behaviors. Lastly, on the protein level, a novel solvent-free protocol was developed, and SNAREs, a family of proteins which mediate vesicle fusion, were reconstituted into the multilayers via the micelle-vesicle-multilayer pathway.